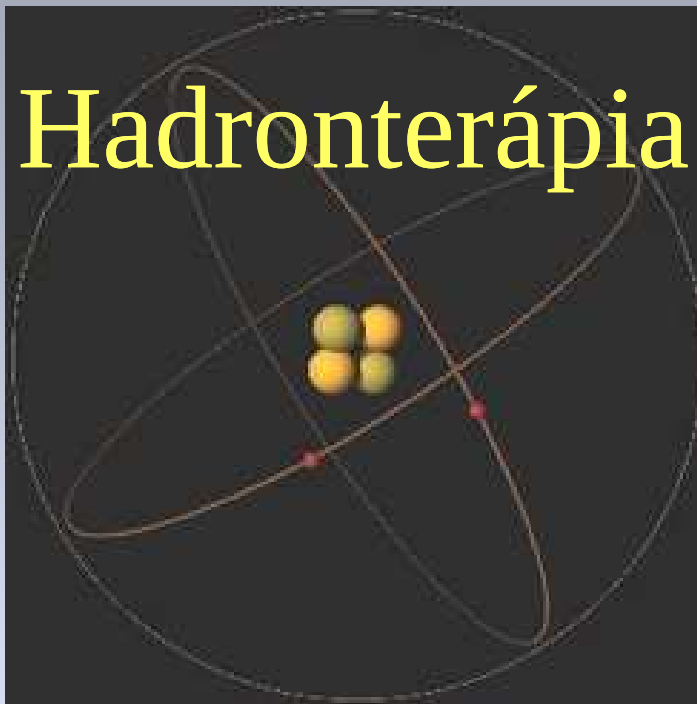


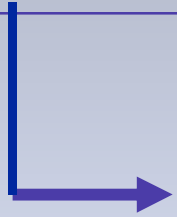
Hadronterápia



Hideghéty Katalin

Komplex tumorkezelés

Fejlett
diagnosztika
interdisciplináris
döntés



Műtét

Sugárterápia

Kemoterápia

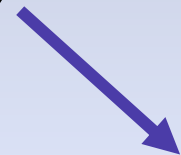
Célzott specifikus terápia

Monoclonalis antigén

Génterápia

Redifferentáció

Vaccinálás



Minőségi élettartam
meghosszabbítás
Szerv/működés
megtartás

Sugárzás hatása különböző szinteken

Atomi

Energia
Ionizáció

Molekuláris

Szabad oxigén
gyökök

Makromolekuláris

Fehérje
DNS károsodás

Szubcelluláris

Anyagcsere
Szabályozás
Membrán,DNS

Celluláris

Sejthalál
Sejtkárosodás

Szövetek

Citokinek
érfal
működés

Makroszkópikus

Sugárreakciók
Nekrózis
Szerv-funkciózavar

Nagy LET

Alacsony LET (indirekt)

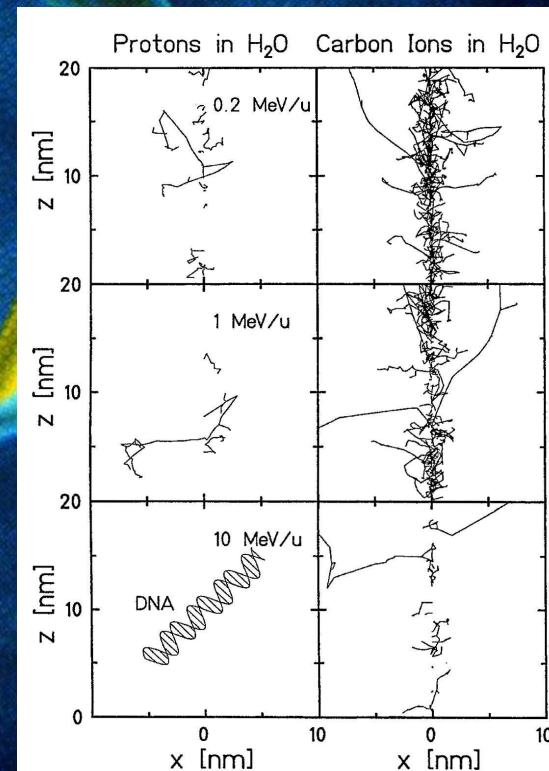
Sűrű ionizáció

Ionizáció ROS

Halmazott hibák

Magas RBE
Alacsony OER

Izolált károsodás



A sugárkezelés hatása, célja

A daganat (el)pusztítása

Gyógyítás (**Kuratív** kezelés)

Tumor volumen csökkentés

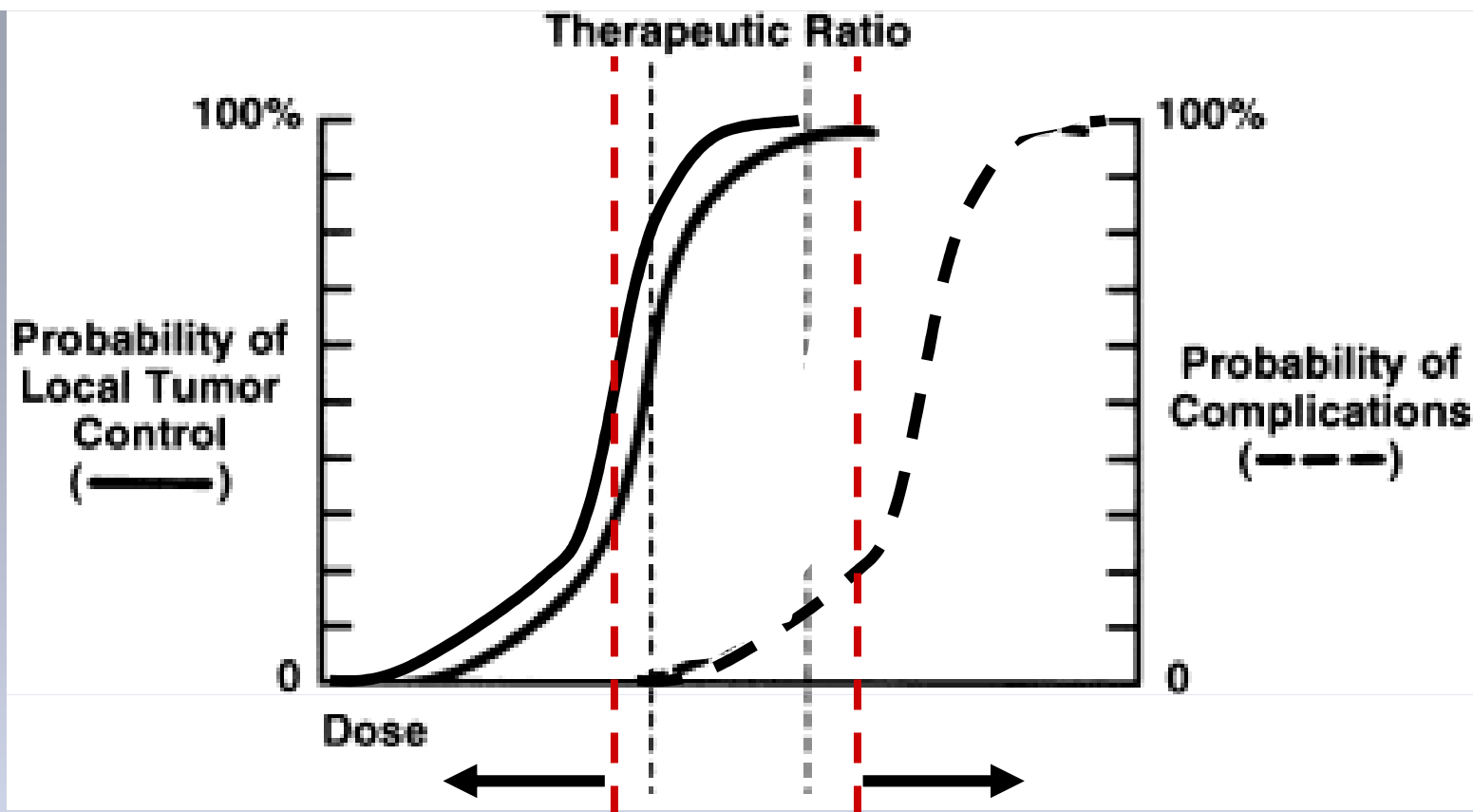
A műtétek kiterjedésének csökkentése (Szerv-/működés-megtartás)

Devitalizálás

Apoptosis indukció

Panaszok csökkentése
(**Palliatív** kezelés)

Proliferáció-gátlás



Frakcionálás

Hypofrakc.

Hyperfrack.

Accelerált hyperfr.
(CHART)

CHARTWELL

Sugárérzékenyítés

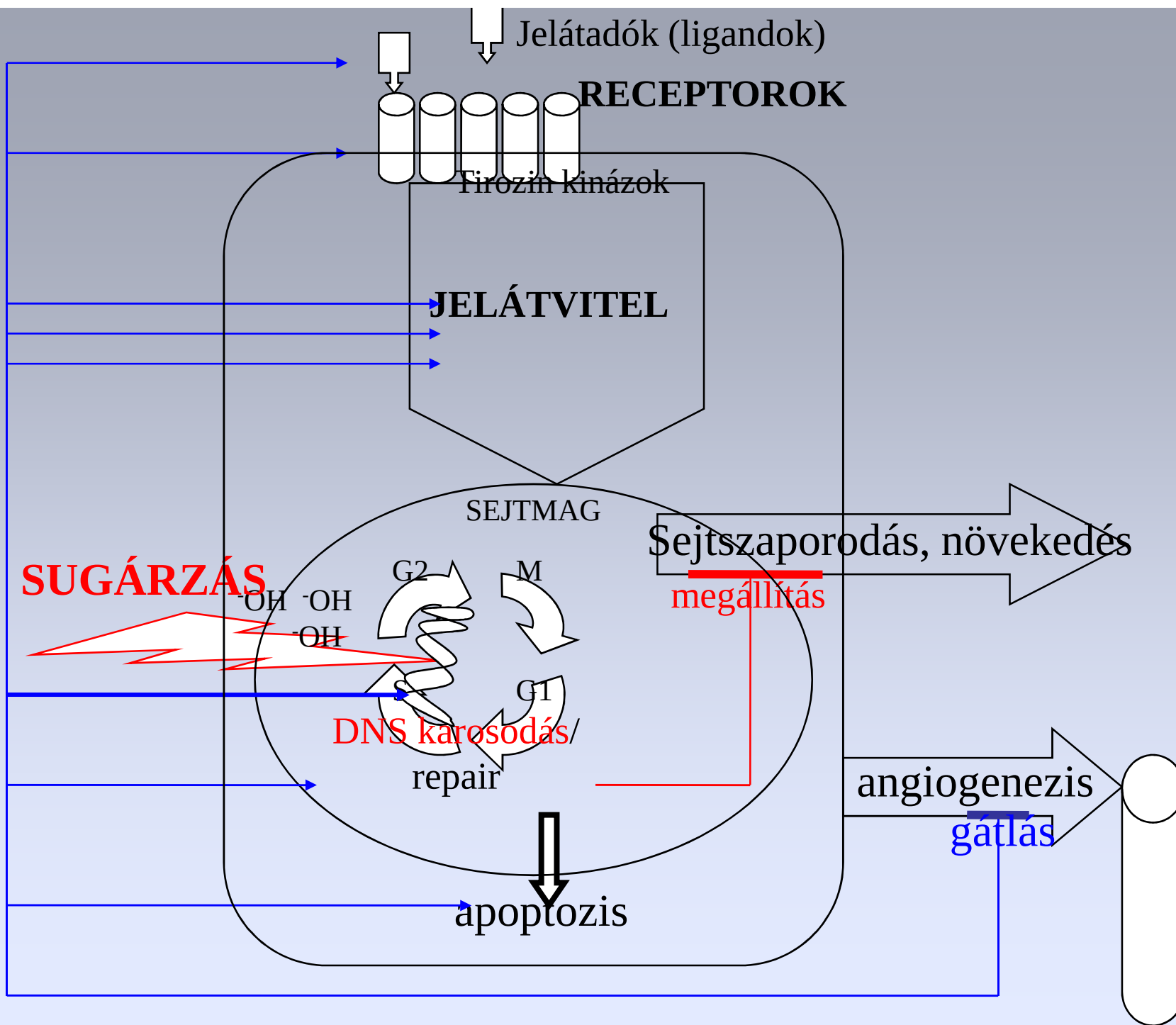
Chemo-, hormon, biol.m.

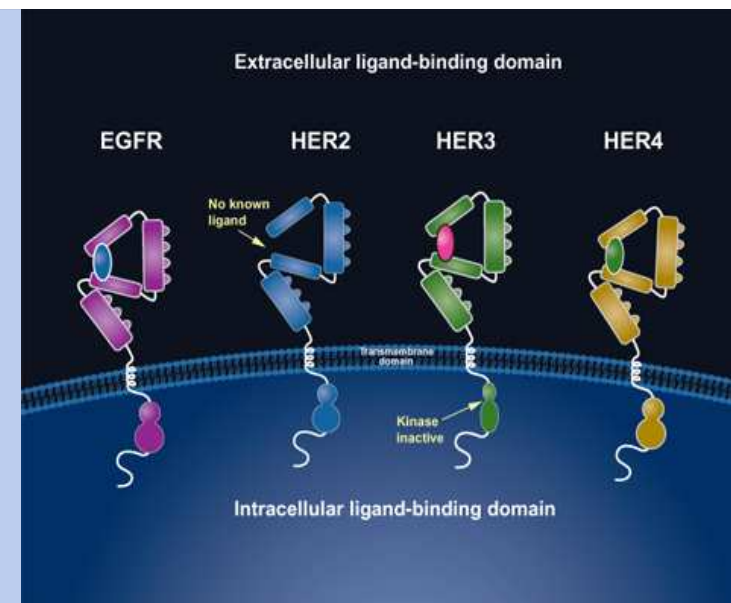
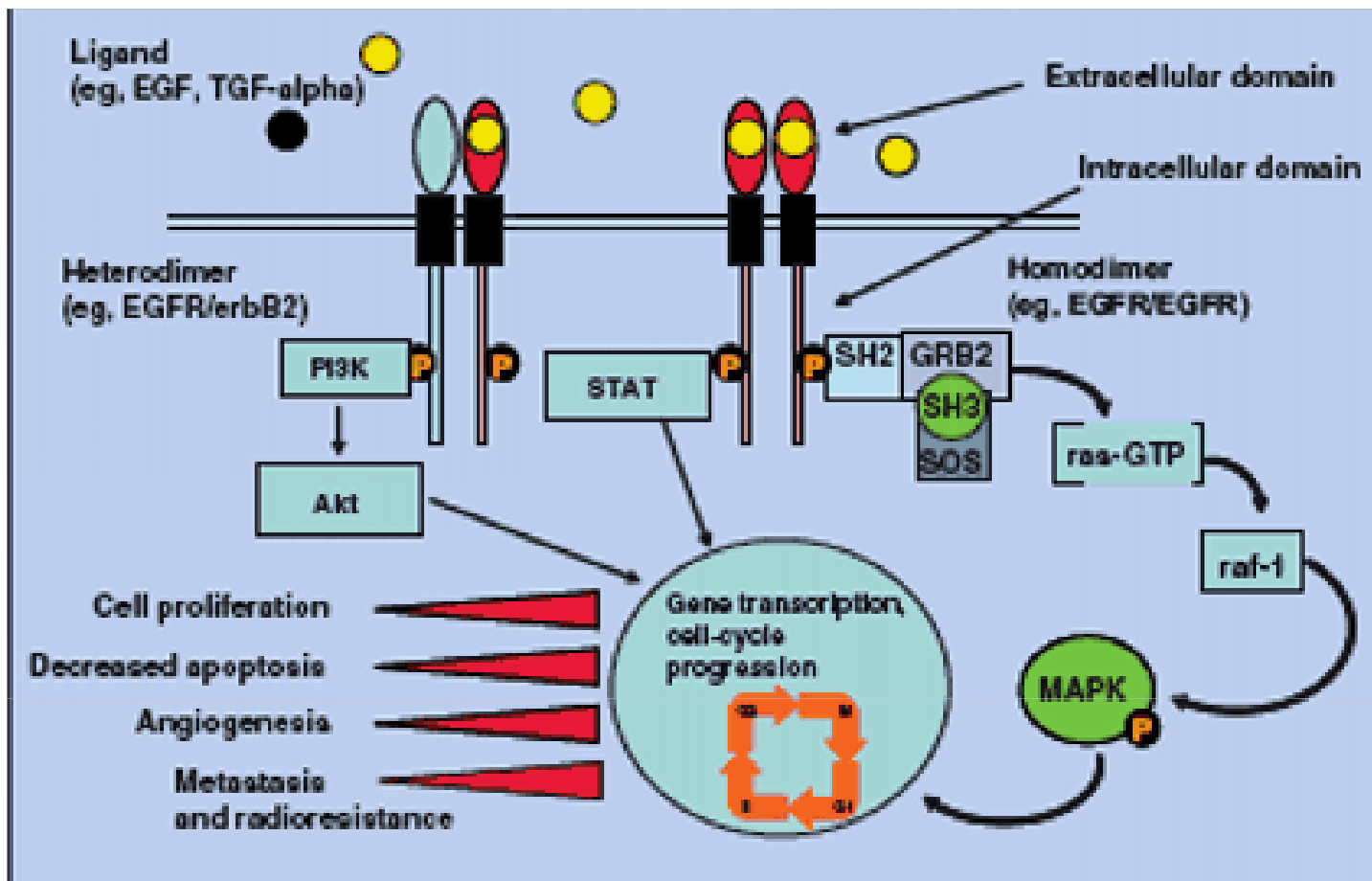
Hypoxiás szenzitizálók

Technikai fejlődés

Fokozott szelektivitás

Biológiai válasz módosító és kemoterápia





Anti-EGFr

TKI

Lapatinib

Erlotinib

Topov

PF-00299804

Multi-I

c-Raf, b-Raf VEGFR-1/2/3, PDGFR- β

Sorafenib

Proteosoma-I

Bortezomib

Cetuximab

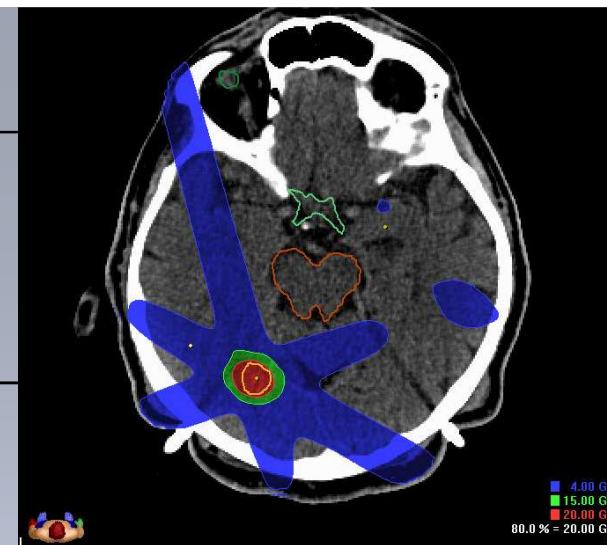
Zalutumumab

Panitumumab

Nimotuzumab



A fizikai specificitás növekedés



Céltérfogat

Szelektív, homogén, ill.
tervezett inhomogén
besugárzás

TCP ↑

Ép szövetek

Besugárzott térfogat és
normál szöveti dózisterhelés
csökkenése

NTCP ↓

Terápiás index növekszik

Szelektív sugárterápia

3D/IG brachyterápia

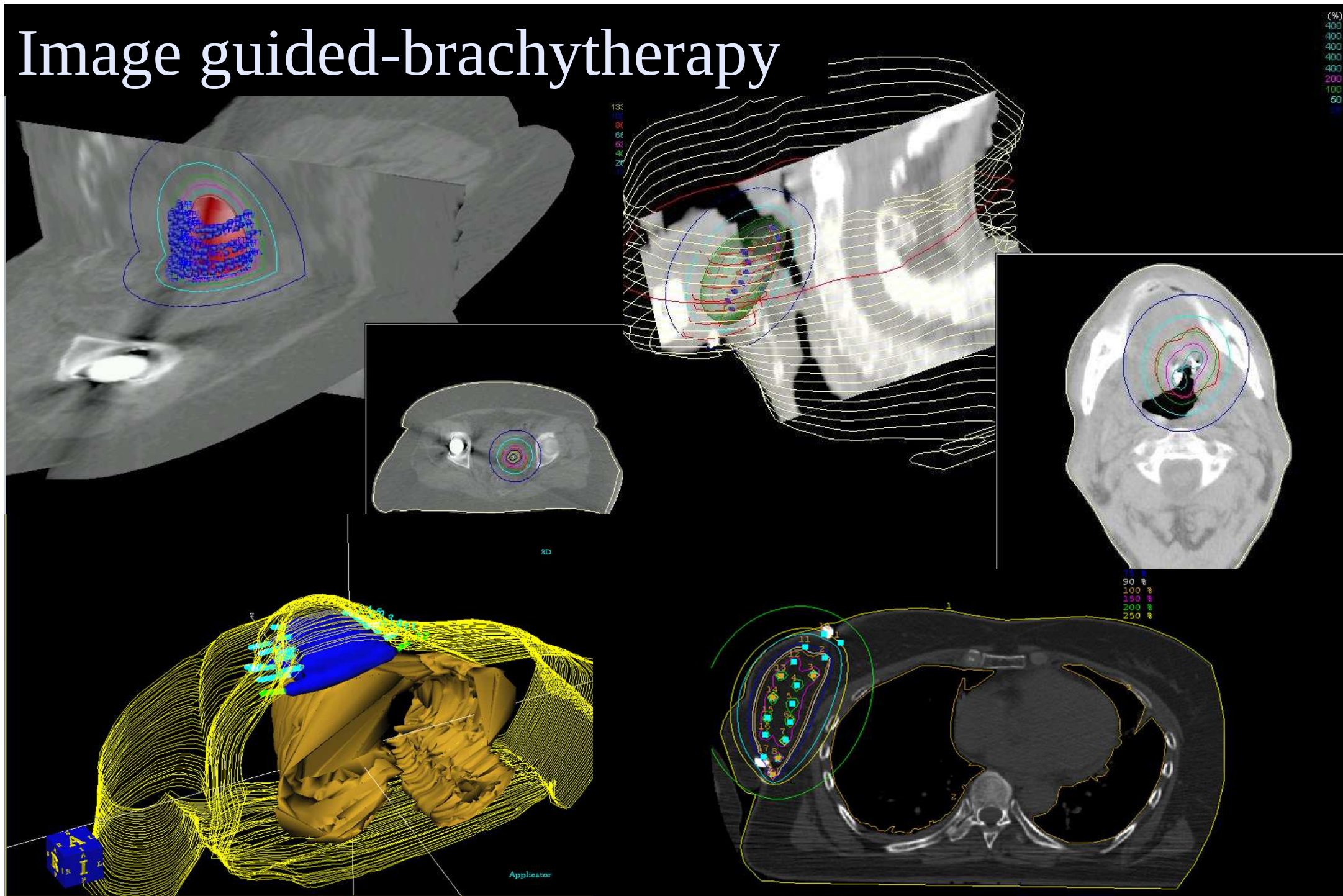
3DCRT/sztereotaxia

IMRT/HT/VMAT

HADRON TERÁPIA

IGRT

Image guided-brachytherapy



Sugárforrások

X-ray tube, Orthovolt (250KV)

Cobalt beam 1,26 MeV

Linearis gyorsító/ VMAT

Helical-/Robot-forrás

Synchrocyclotron/reaktor

**Laser indukált hadron
forrás**



Céltérfogat meghatározás

2D becslés, Anatomia, Szimulátor

CT, PET-CT/MRI

Tervezés

Manuális, 2D

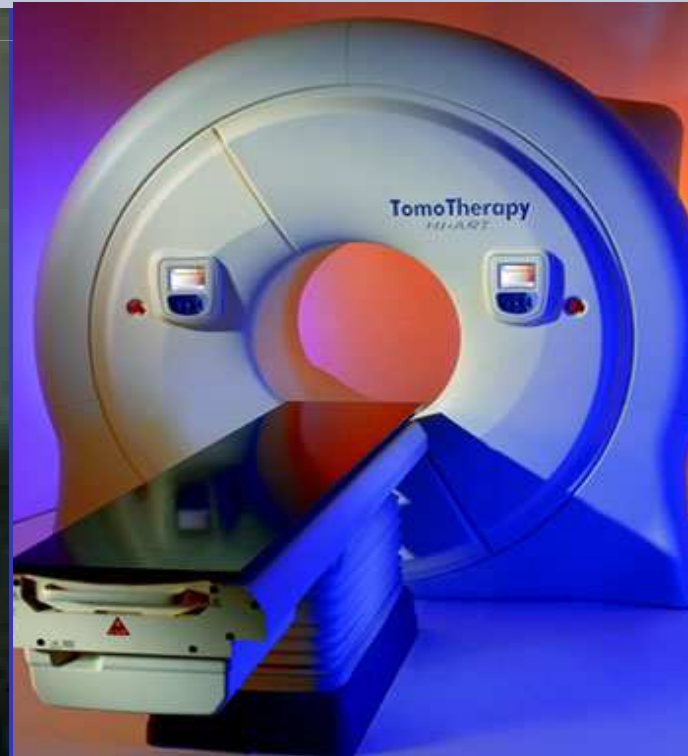
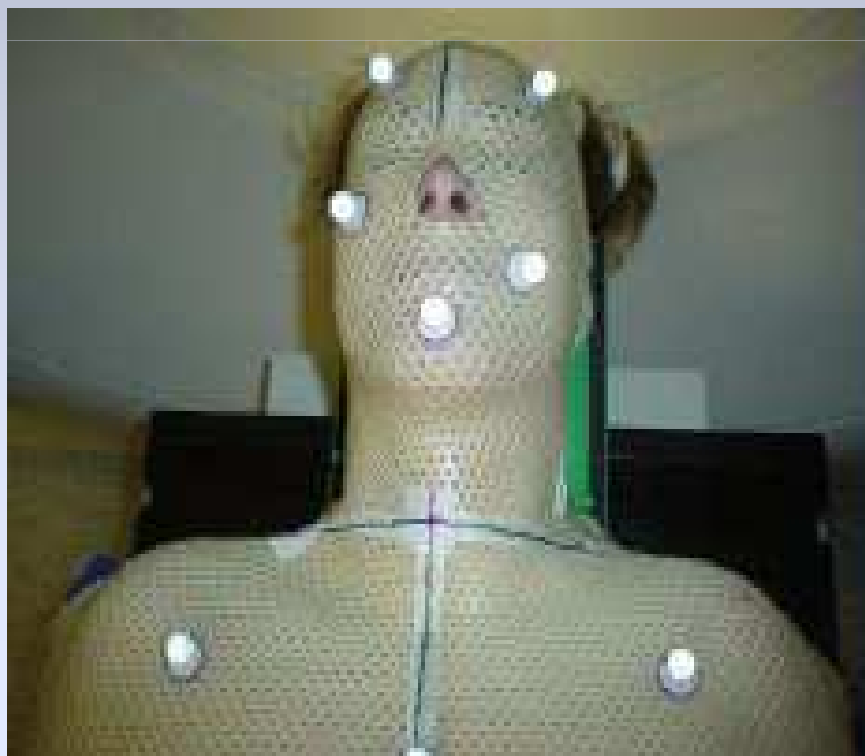
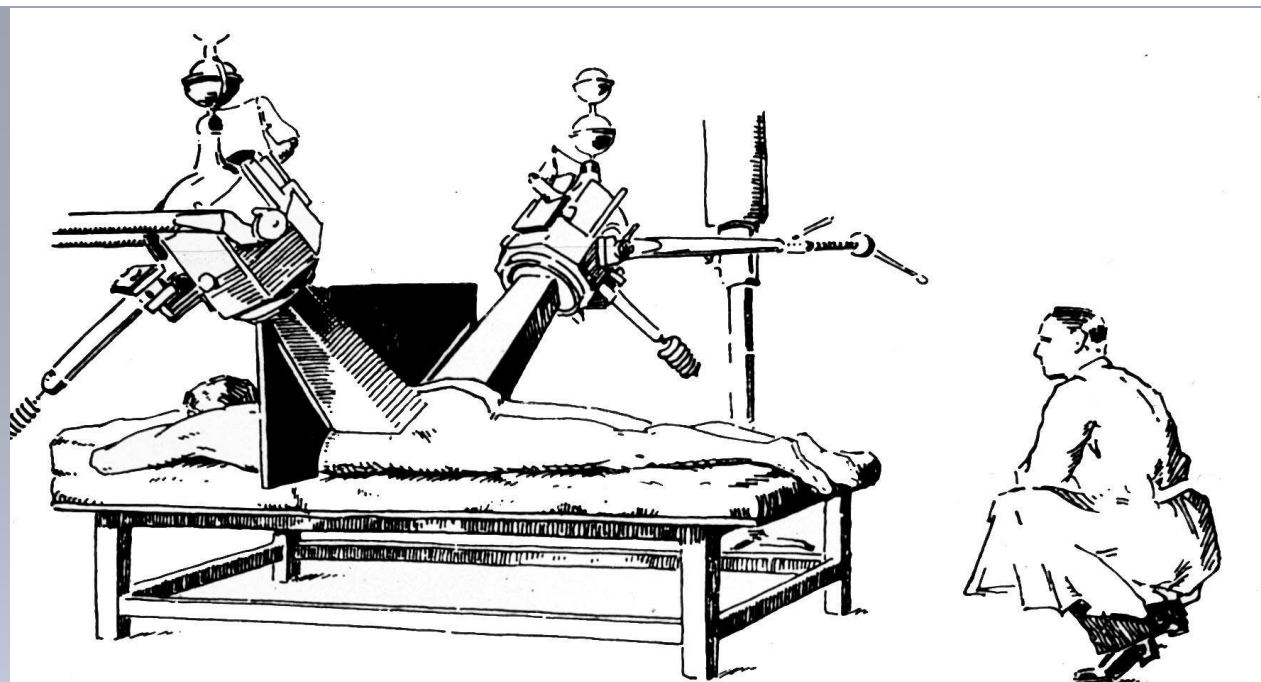
3D forward, inverz

Kivitelezés

Pozícionálás/ beállítás

Kezelés verifikáció

Film, EPID, IGRT



Folyamat-rendszer

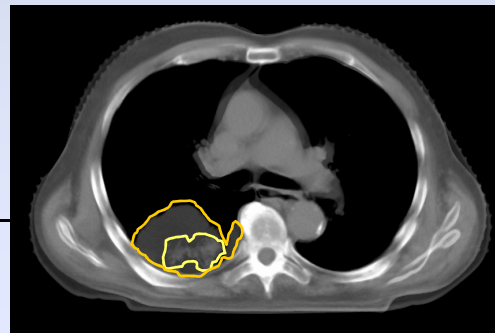
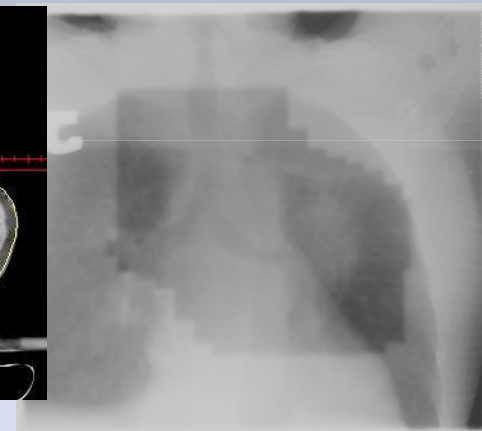
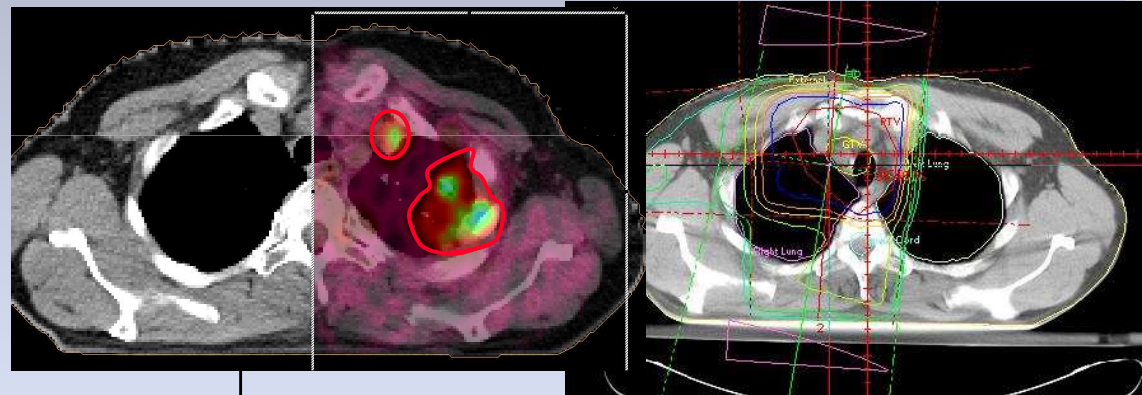
Beteg fektetés
immobilizáció

Tervezési
képalkotás(CT)

3D
tervezés

Beállítás, me-
zőellenőrzés

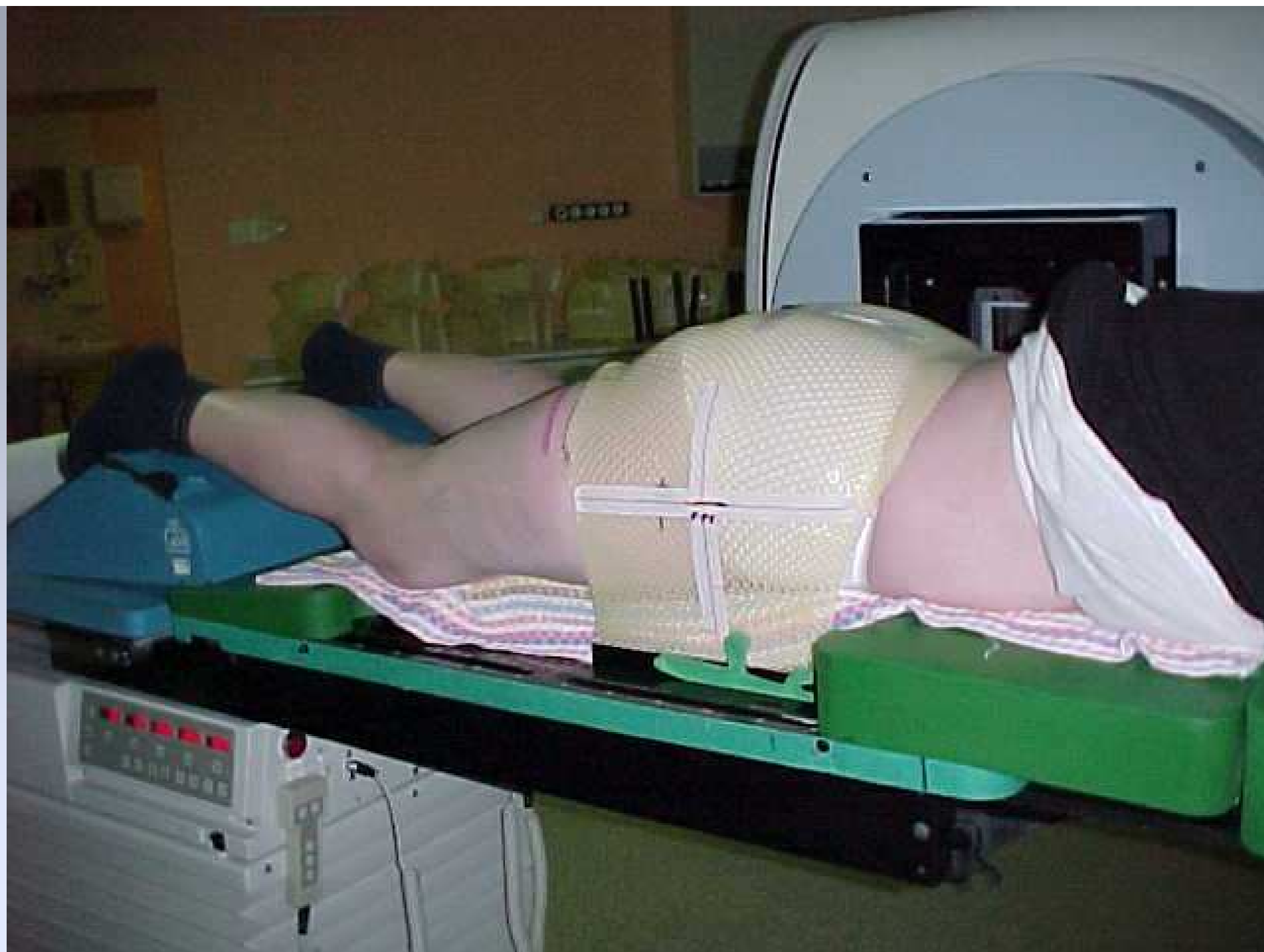
PET-CT/MRI



Re-CT- kép fúzió



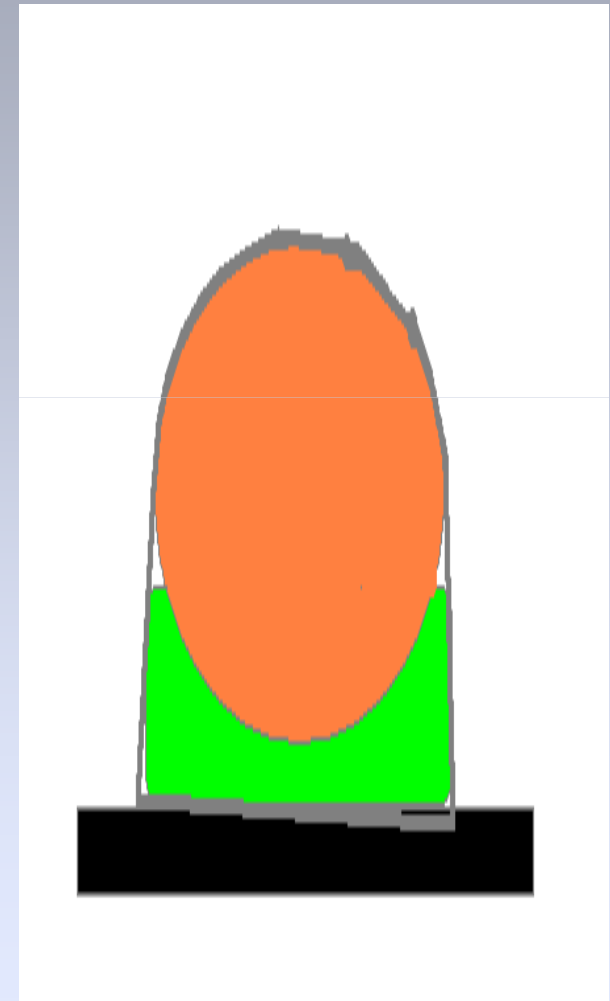
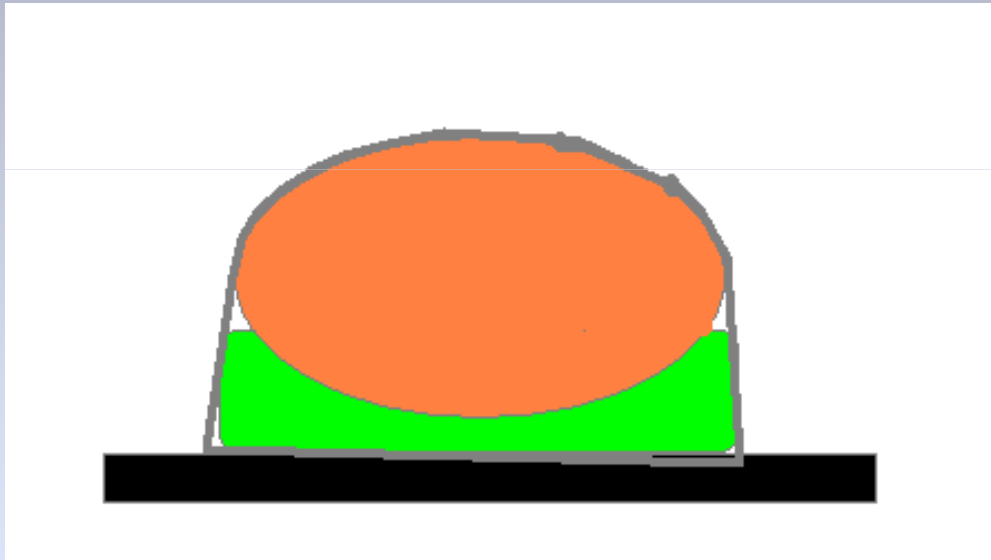








Combination of vacuum cushion and thermoplastic mask







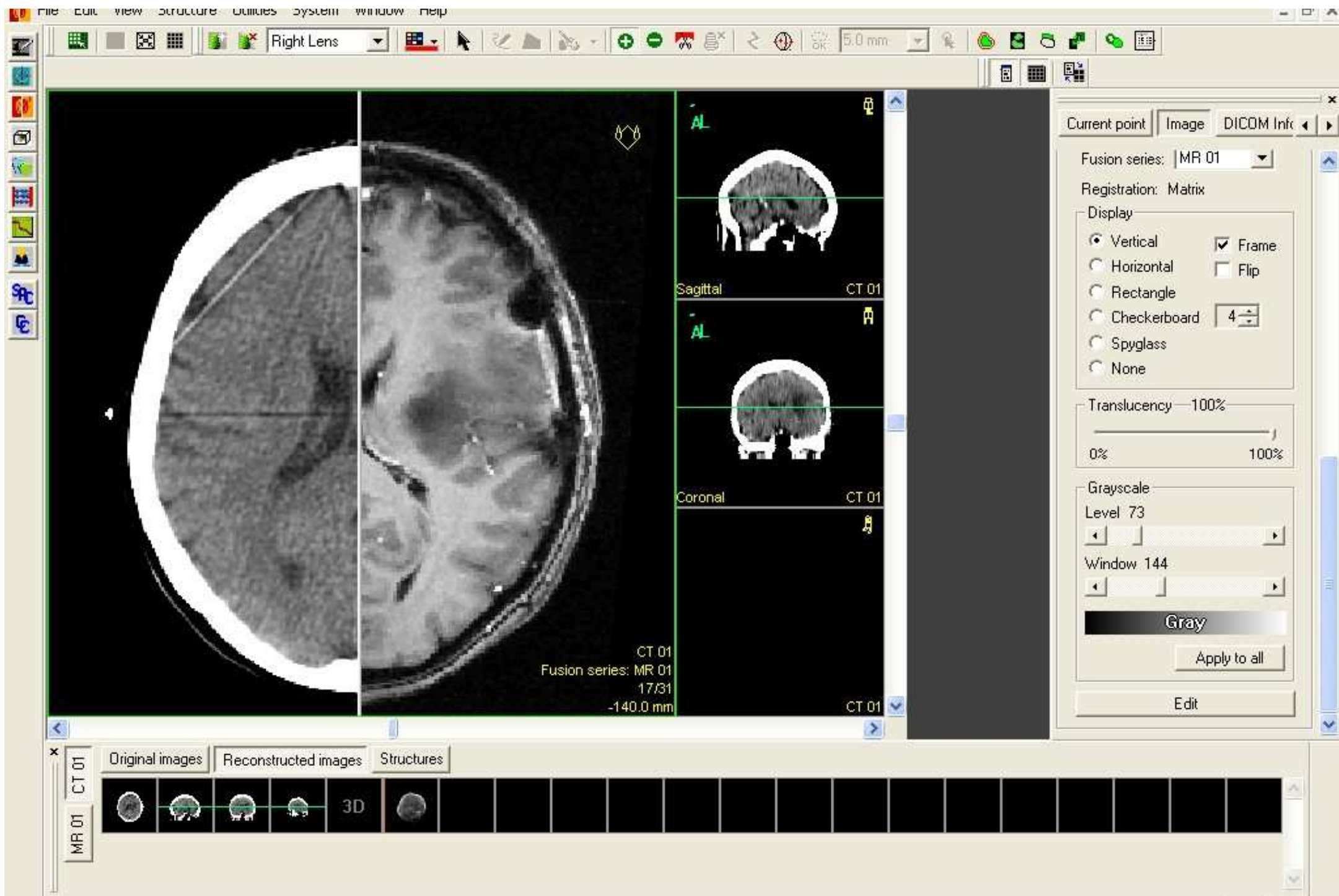




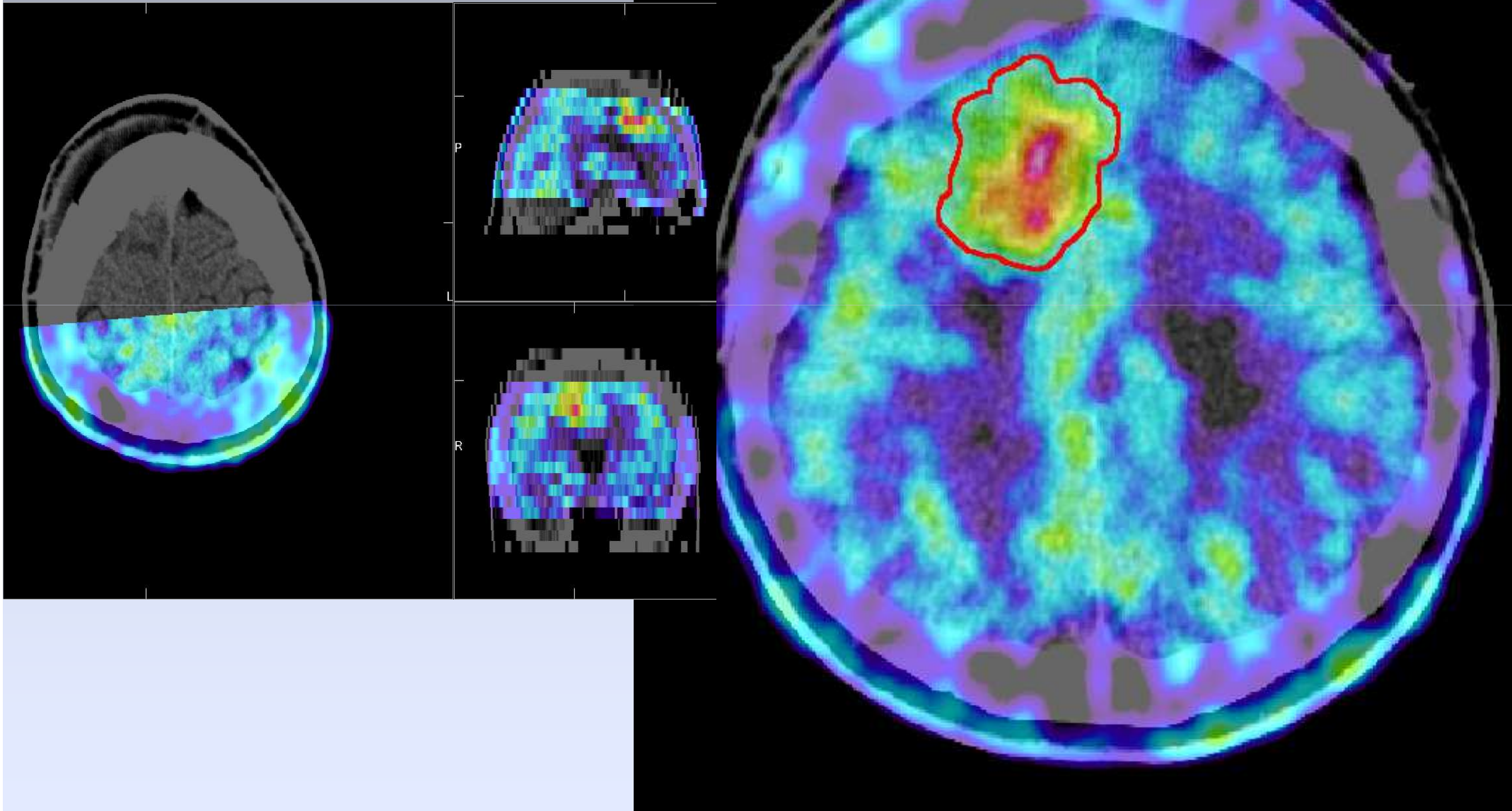


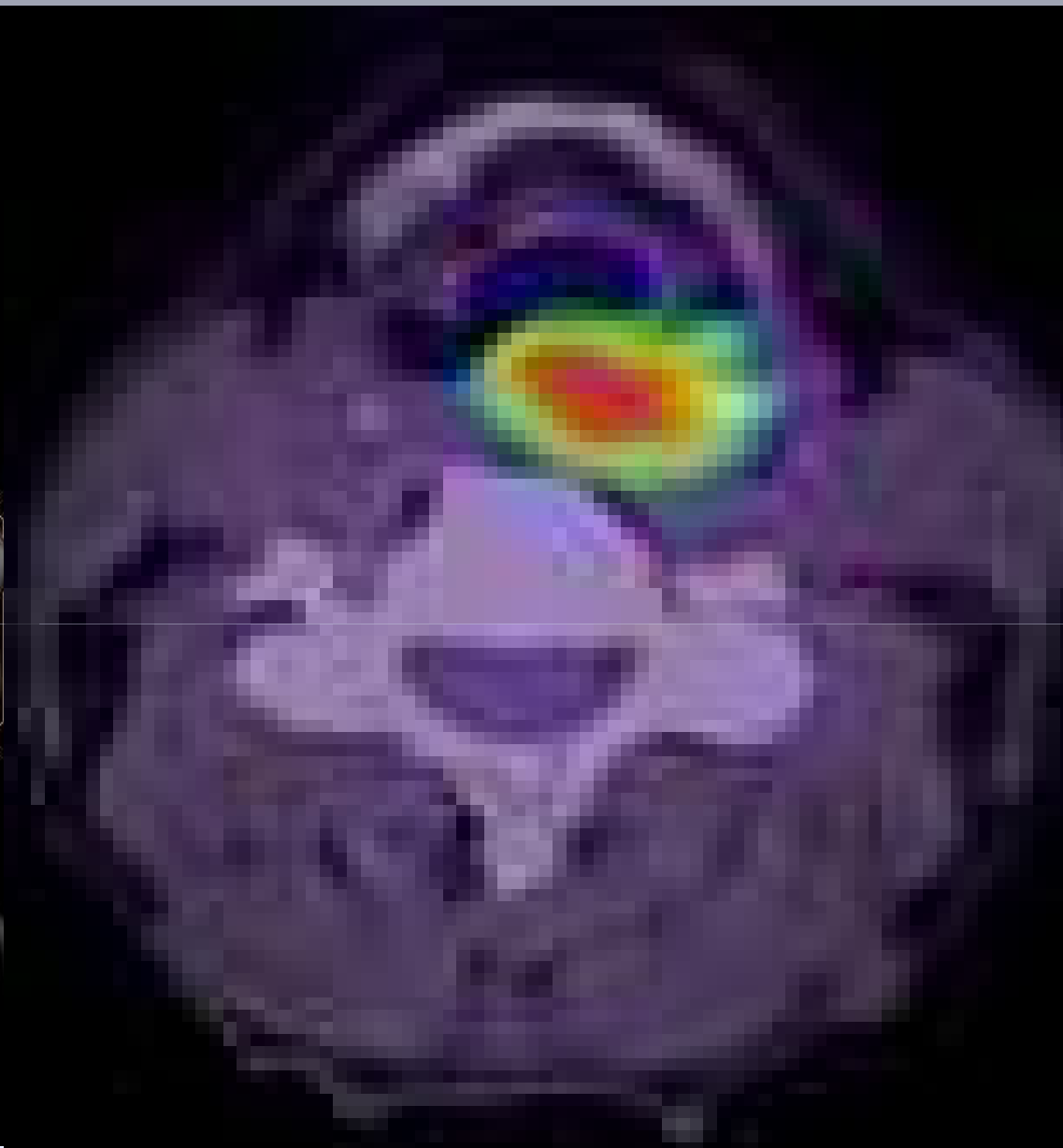
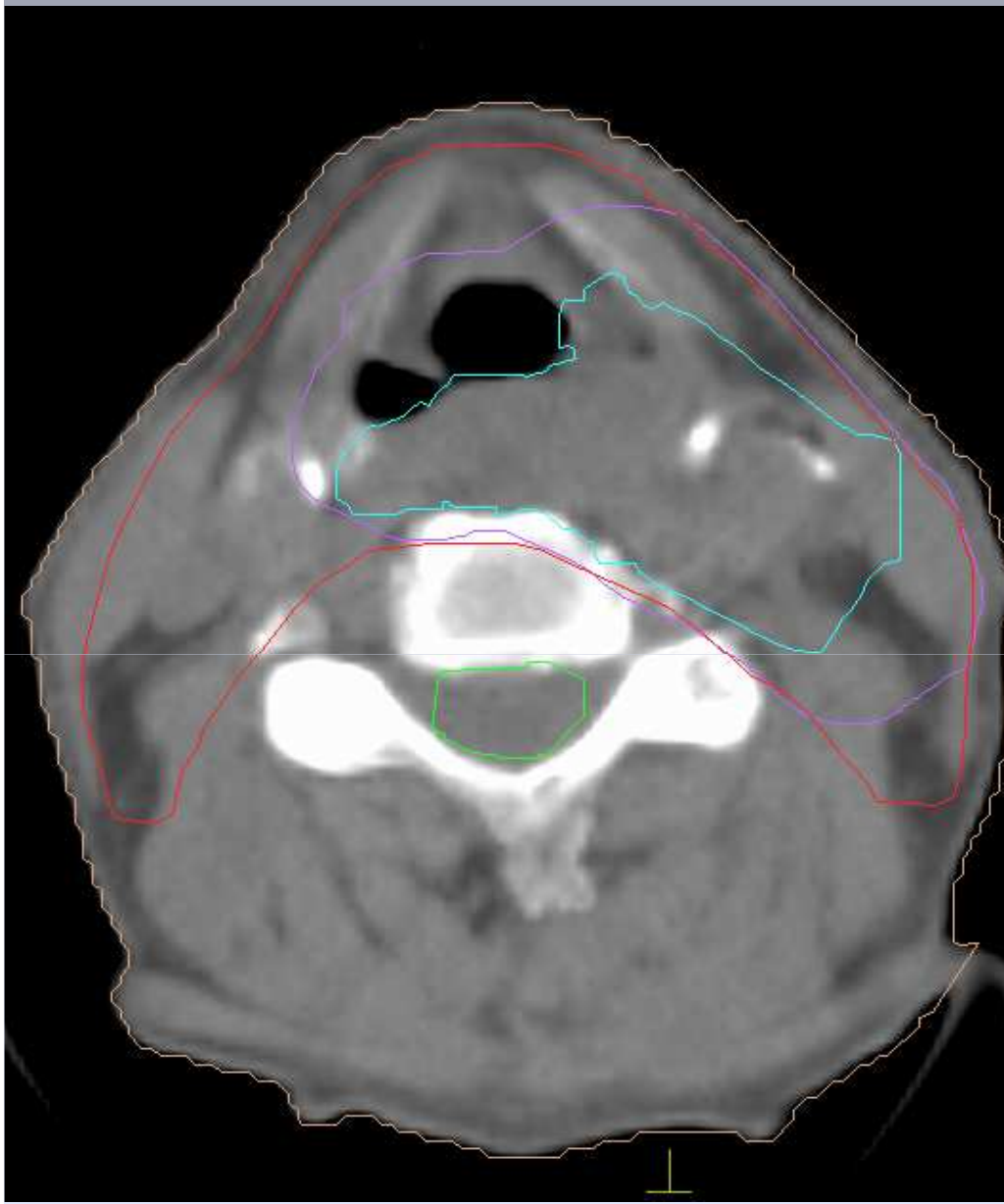
PET/CT





Indication of target volume on the basis of PET-CT image fusion

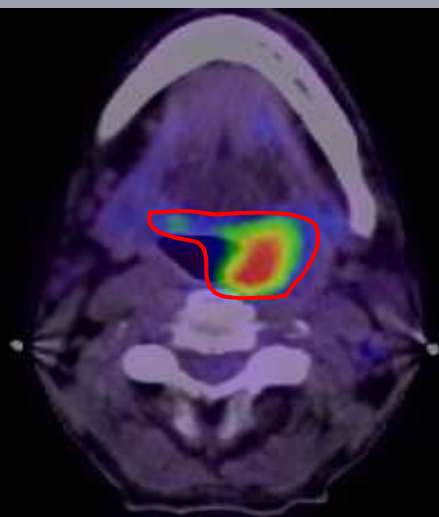




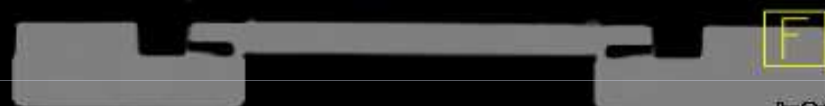
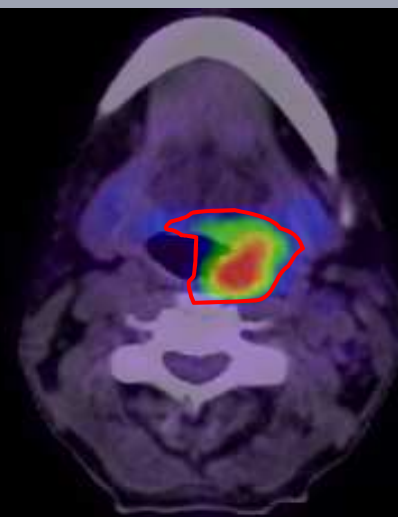
FD0802



Time:17:06:32
No.:54
x 0.9

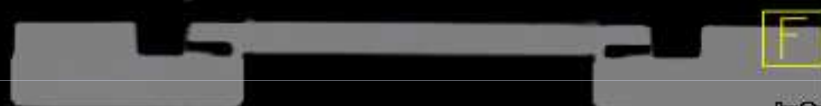


L R



AcqNo:2
SL:
ST:
CM: CS:
GT: TI:

ImC:SUG.TERV. MAR kV:
W : 00255 mA:
C : 00127 Feed:



ImC:SUG

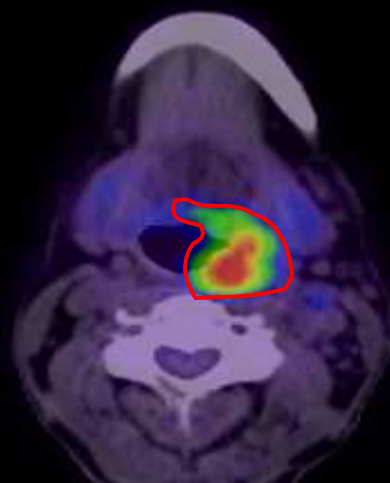
ENYHE JANOS****
15110
01/1951
08/2007
06:32

P
A

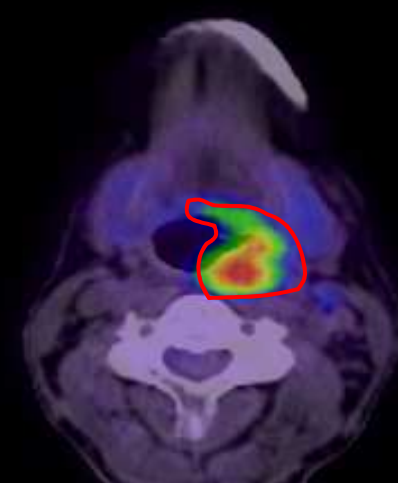
Inst:Pozitron-Diagnosztika Kft. Name:BENYHE JANOS****
Model:Sensation 16 ID:016115110



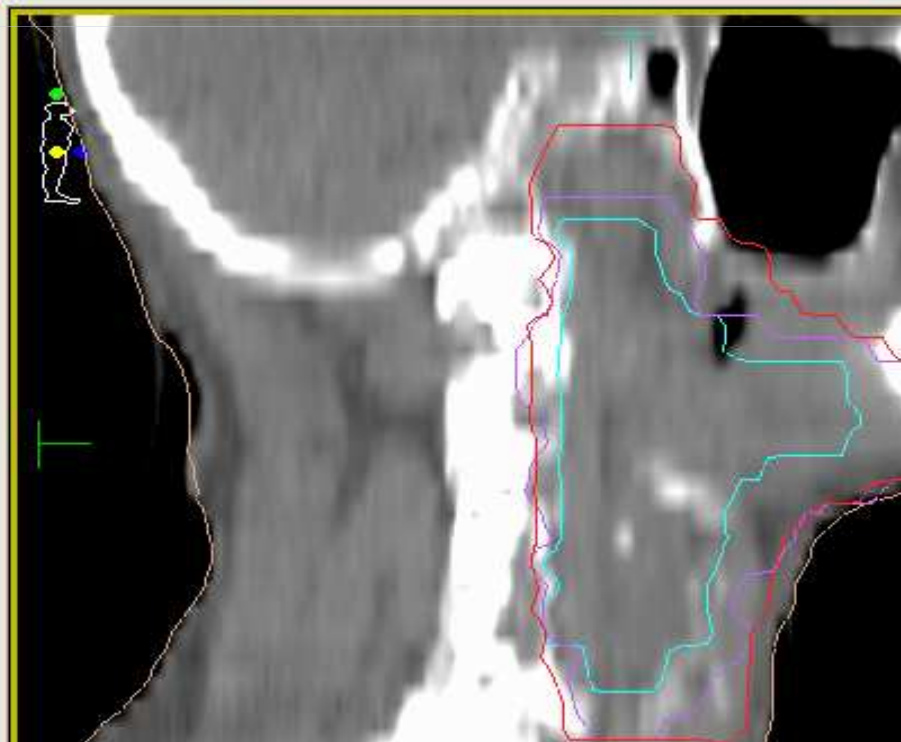
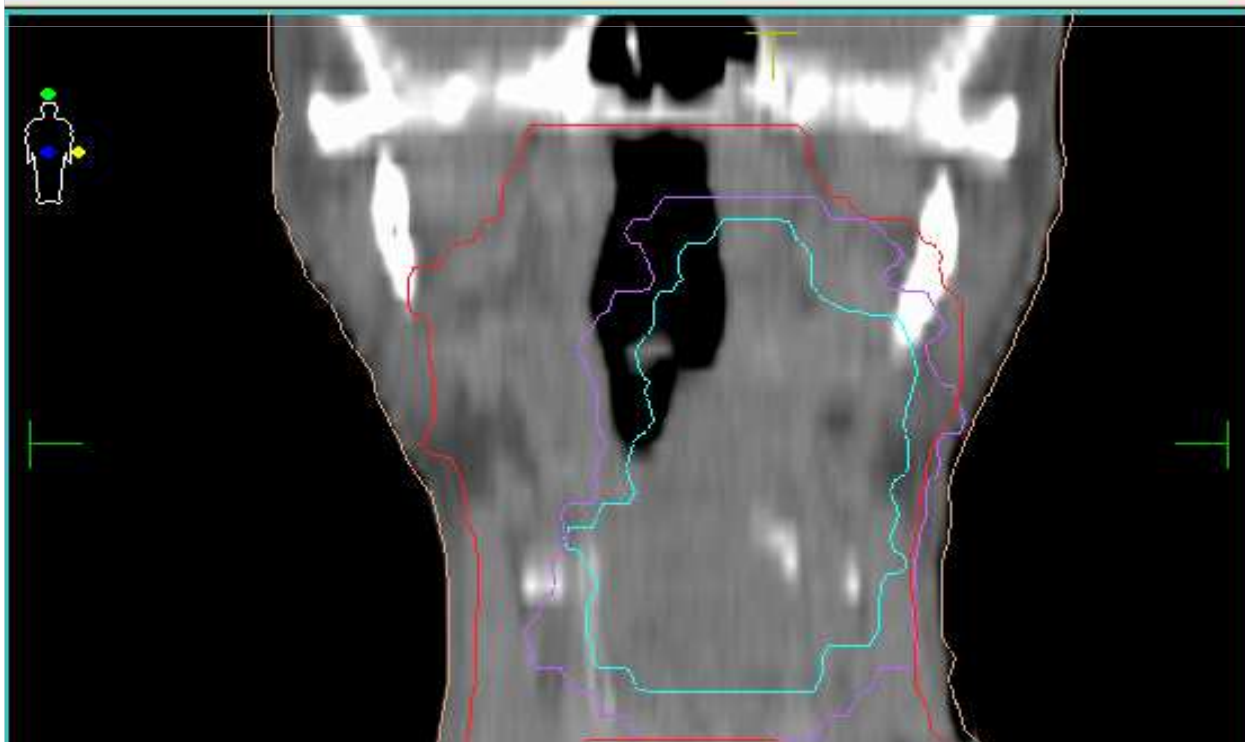
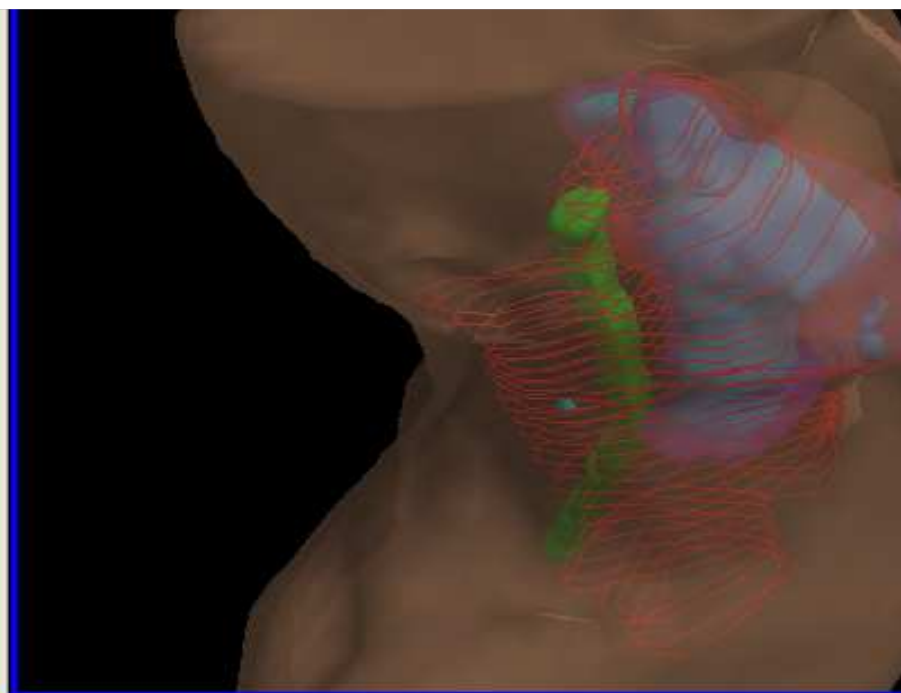
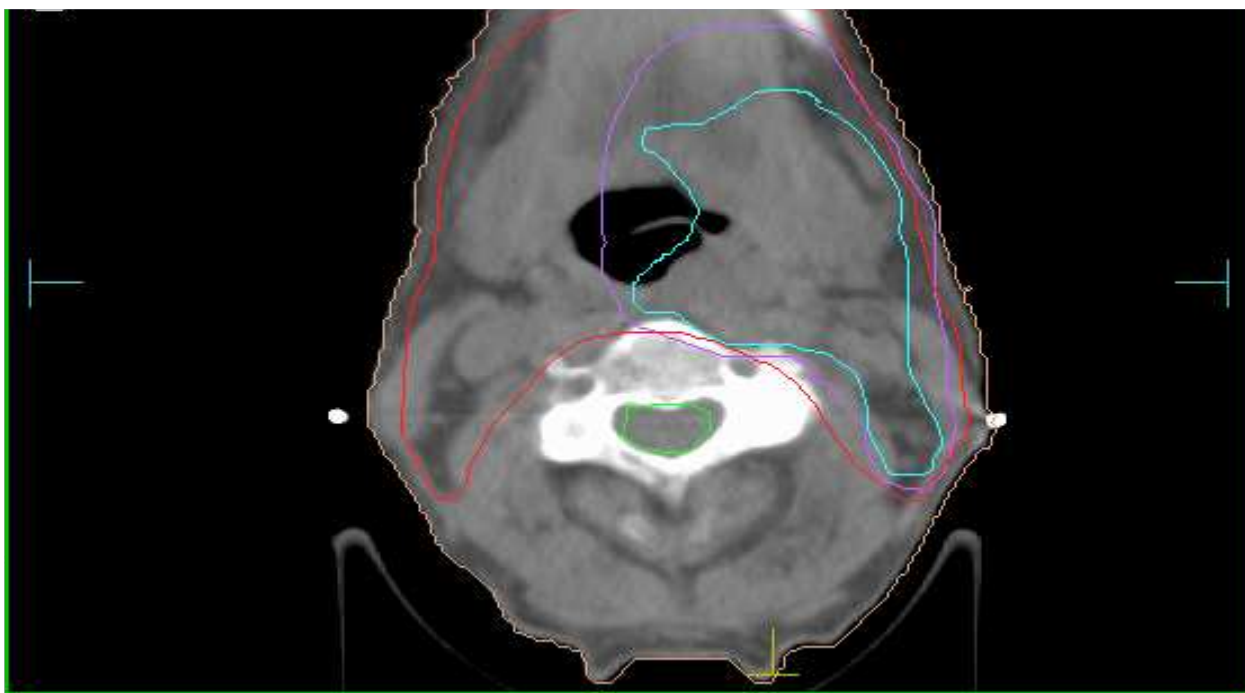
55 DoB:13/01/1951
Date:06/08/2007
Time:17:06:32
No.:56
x 0.9

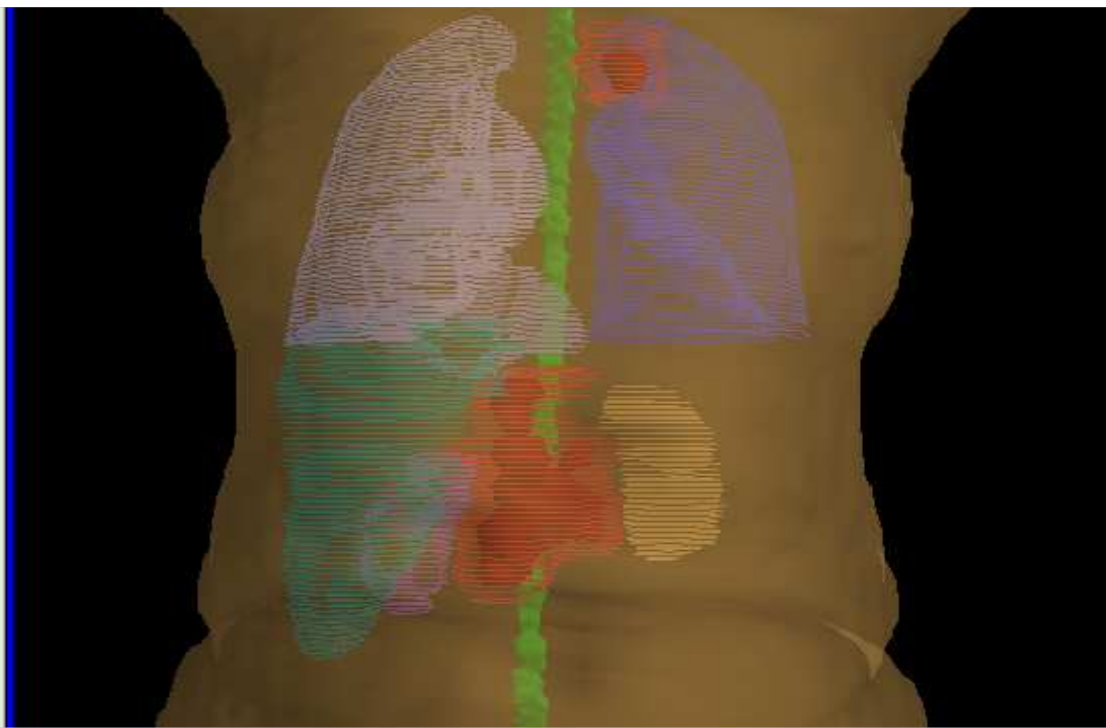
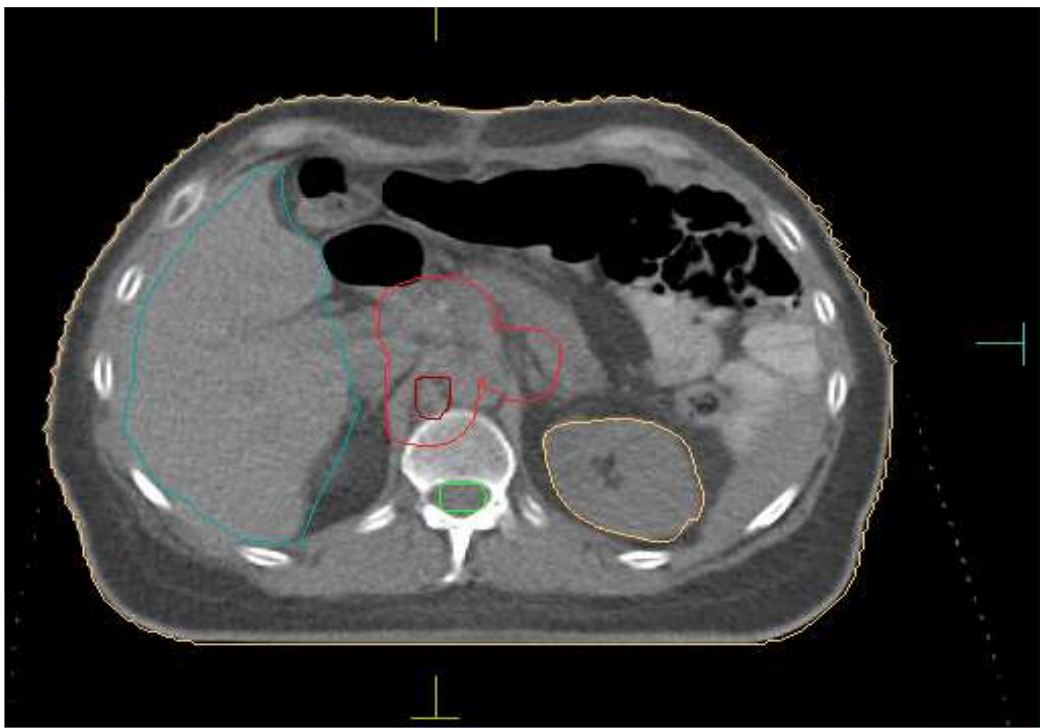


L R



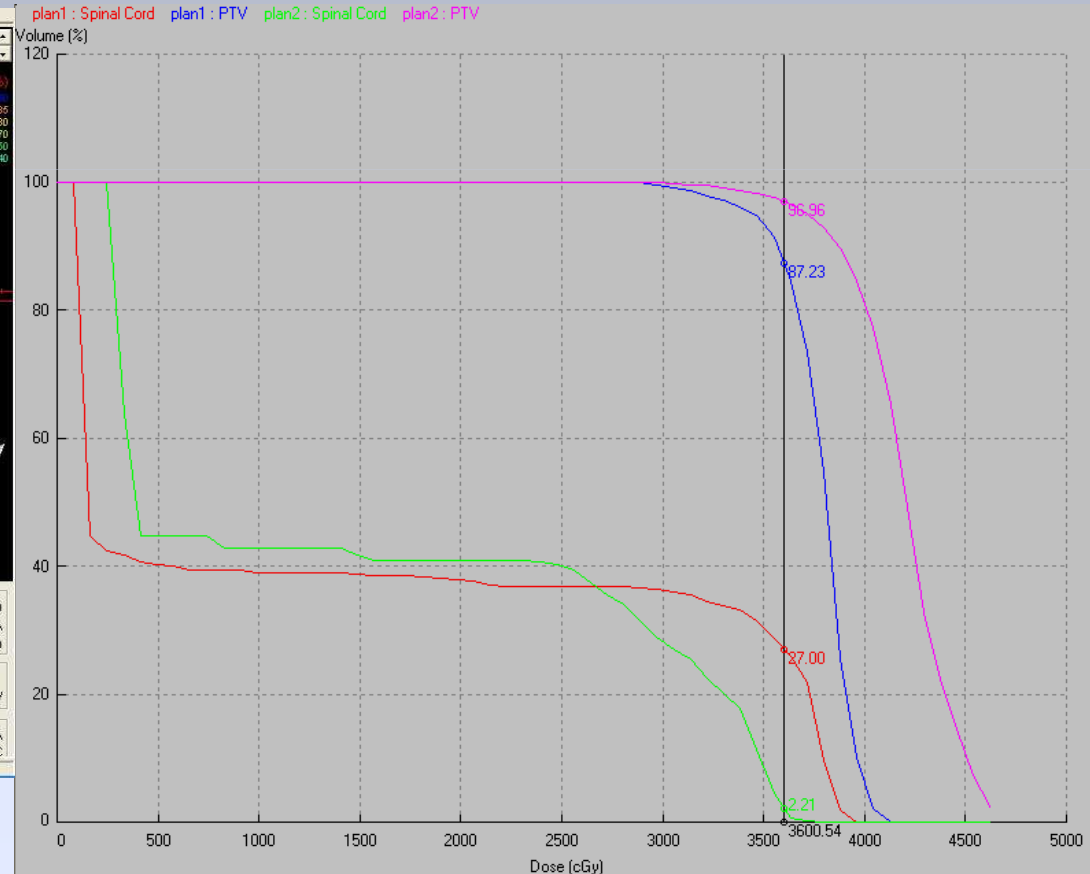
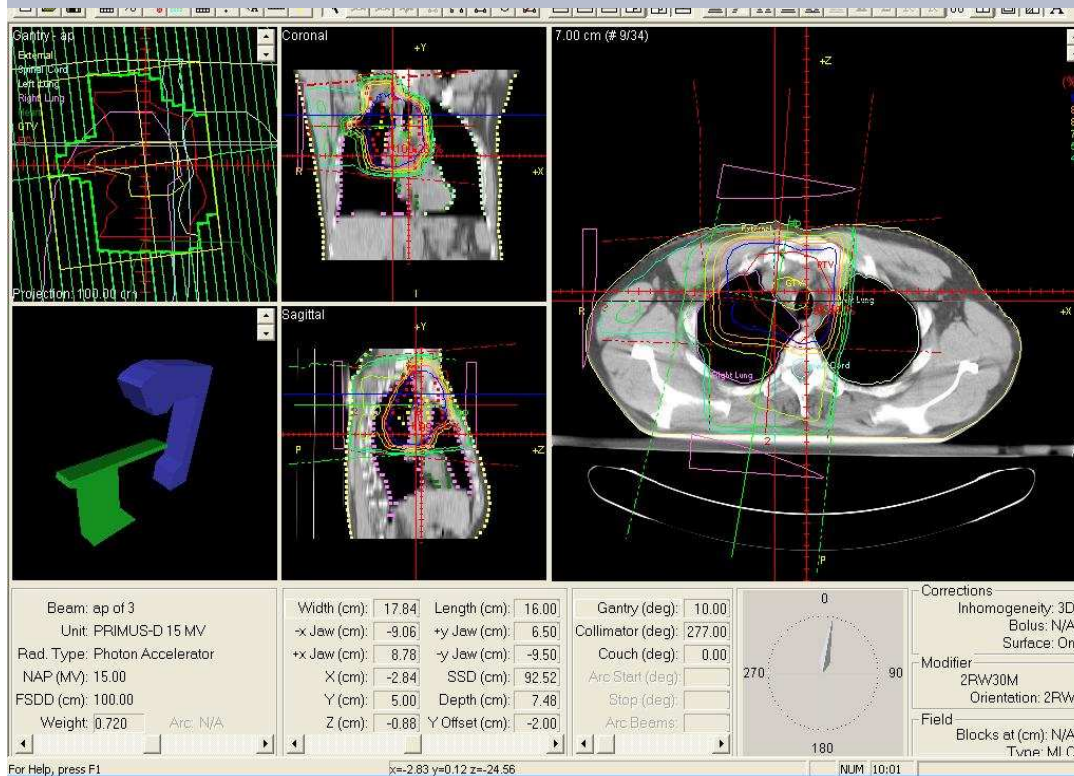
P
A
Inst:Pozitron-Diag
Model:





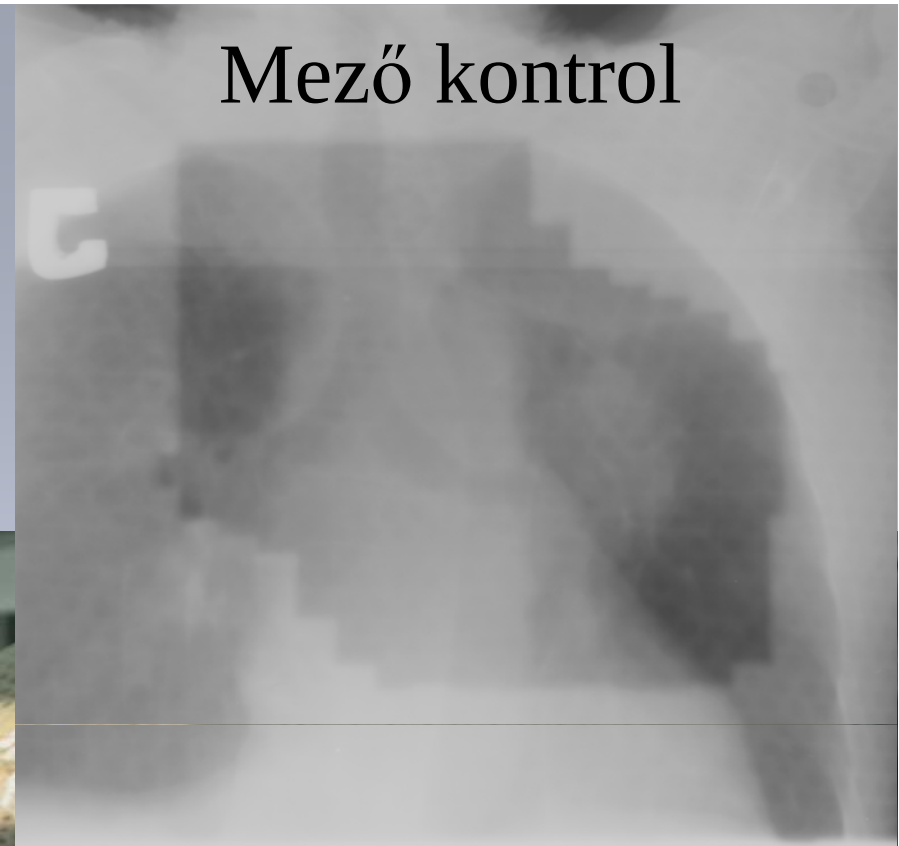
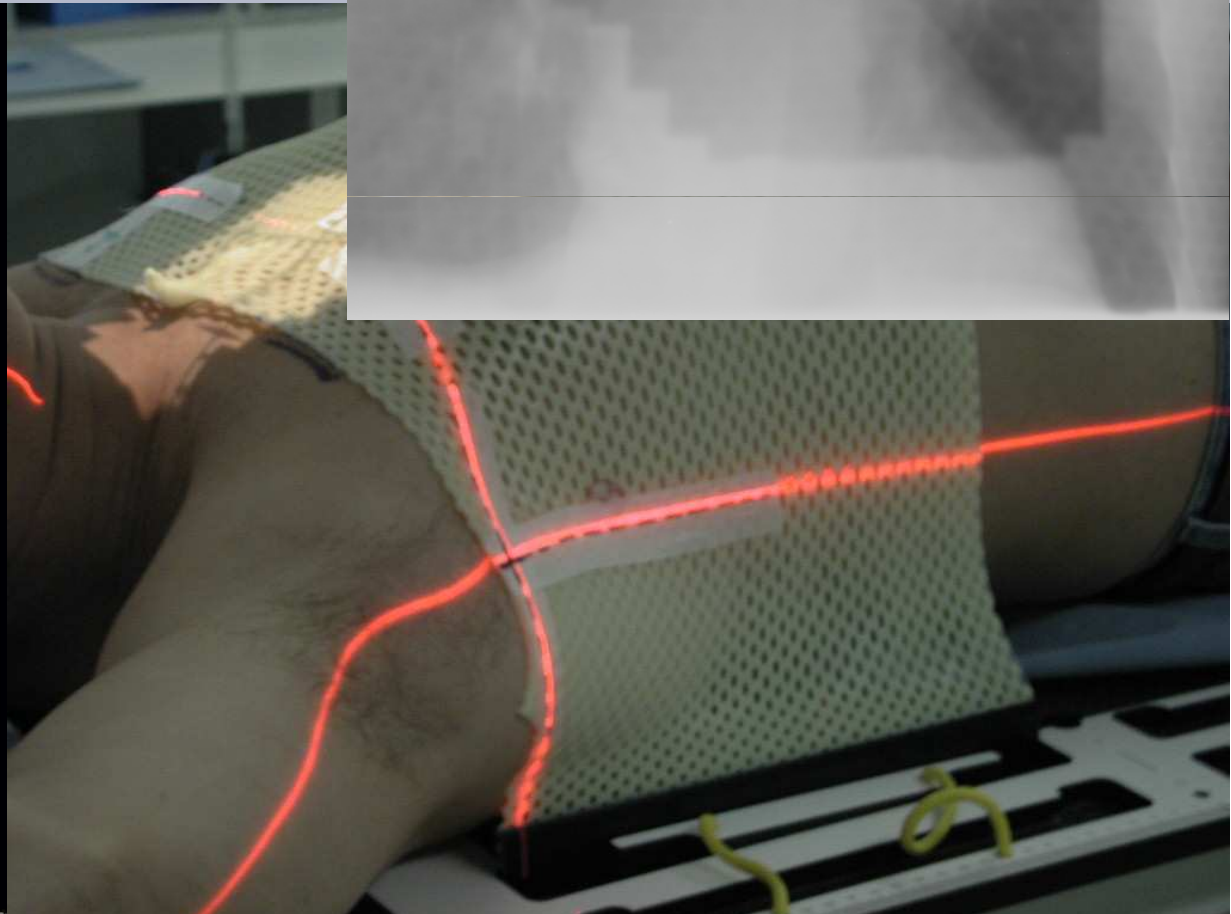
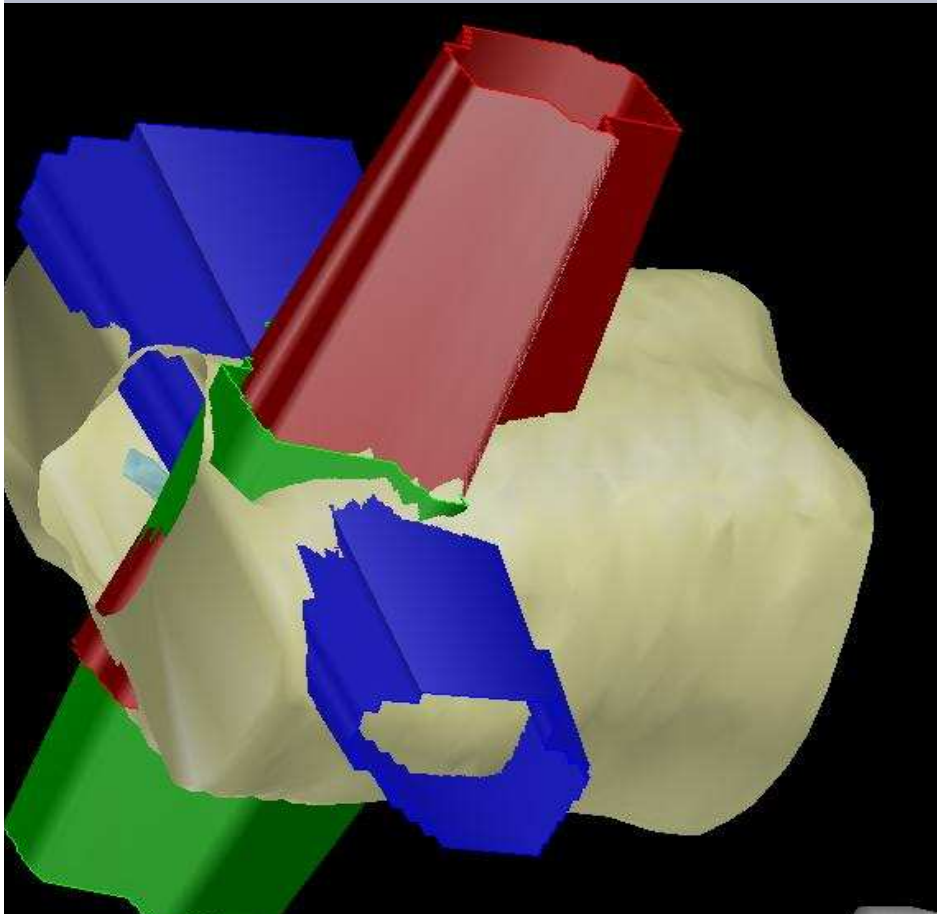
Besugárzás-tervezés- terv értékelés

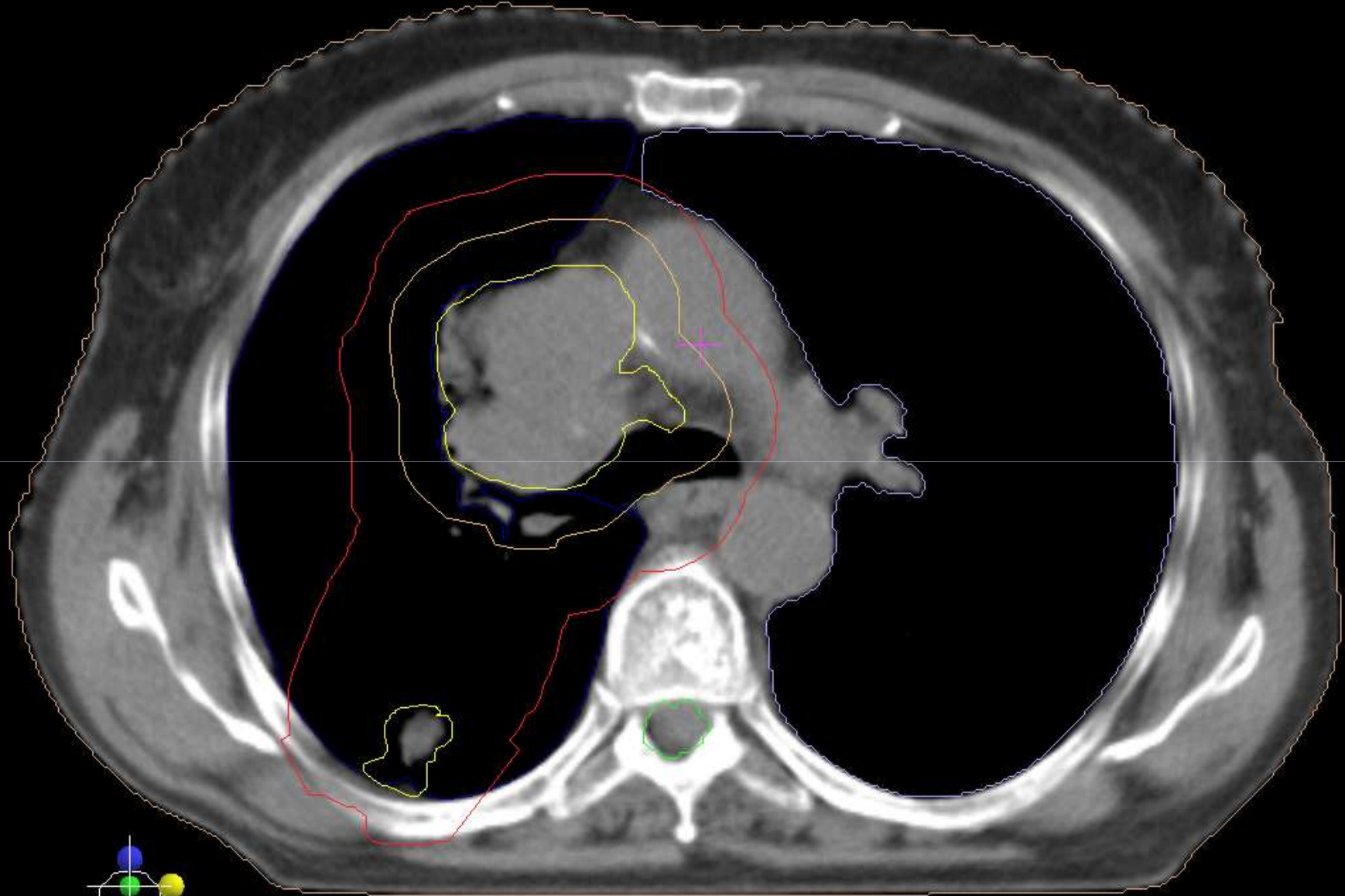
dóziseloszlás – numerikus, anat., DVH



Besugárzás

Mező kontrol



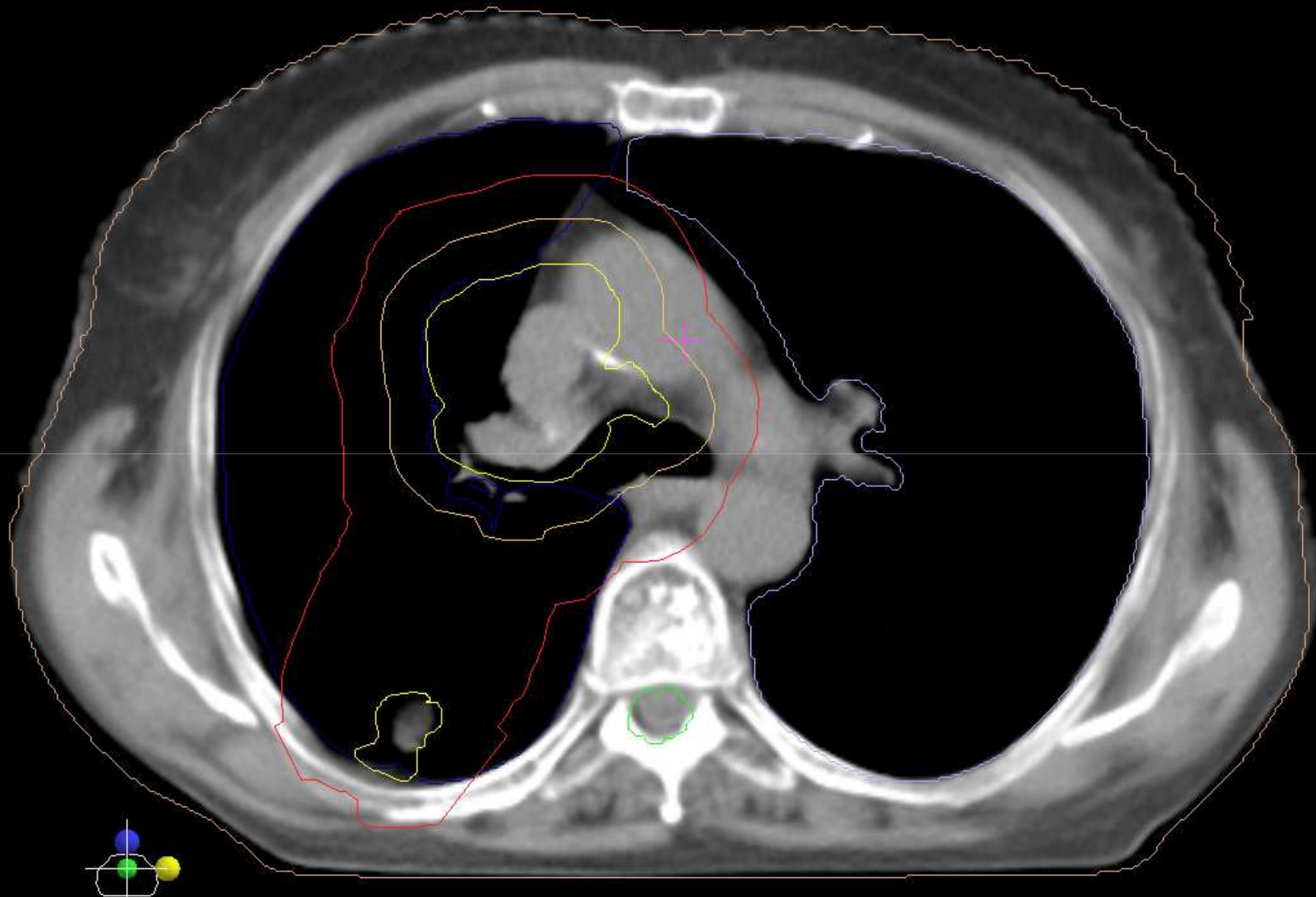


Maximized

T: 1.90 (cm)

Scale=1: 1.11

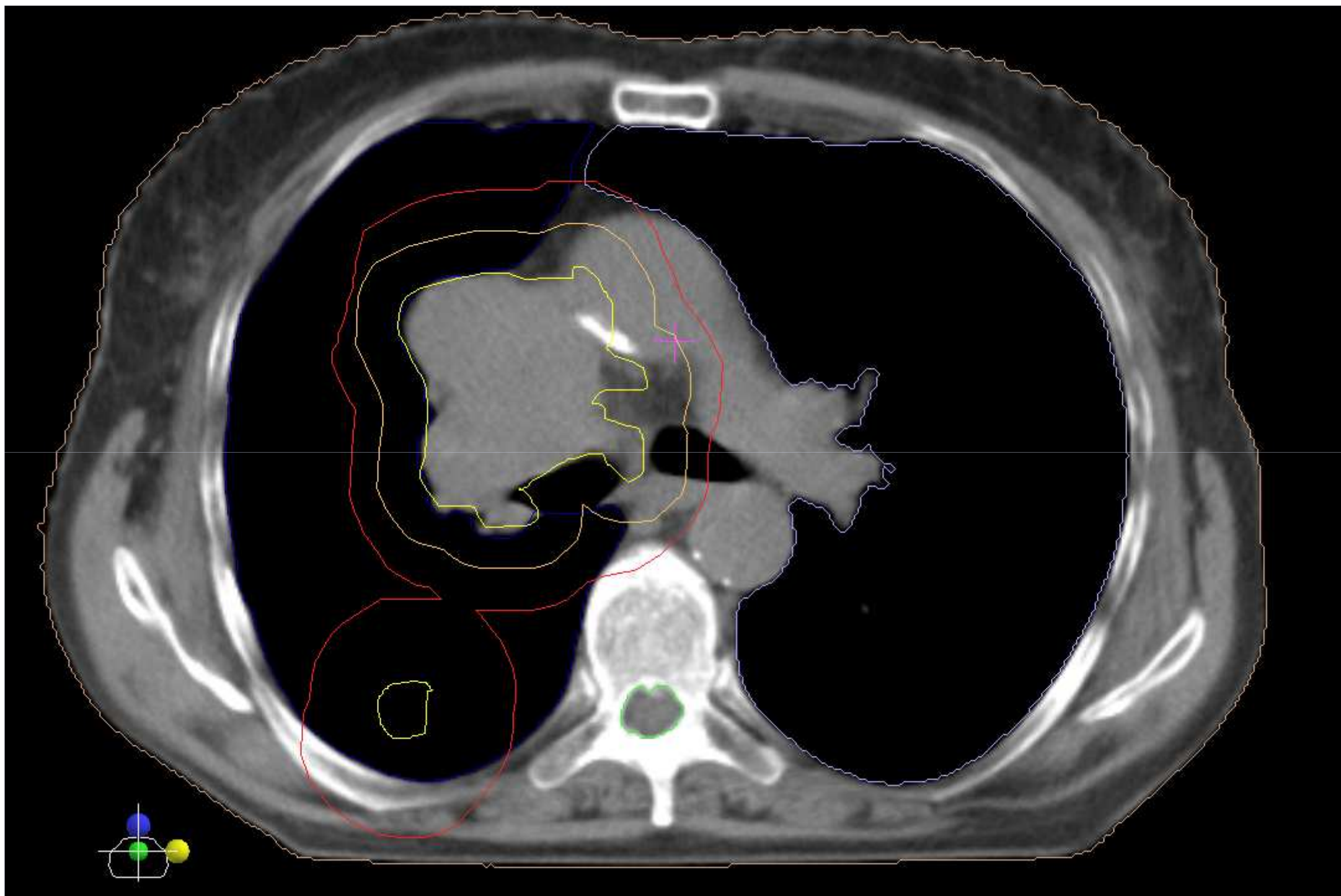
Re-CT 45Gy-nél

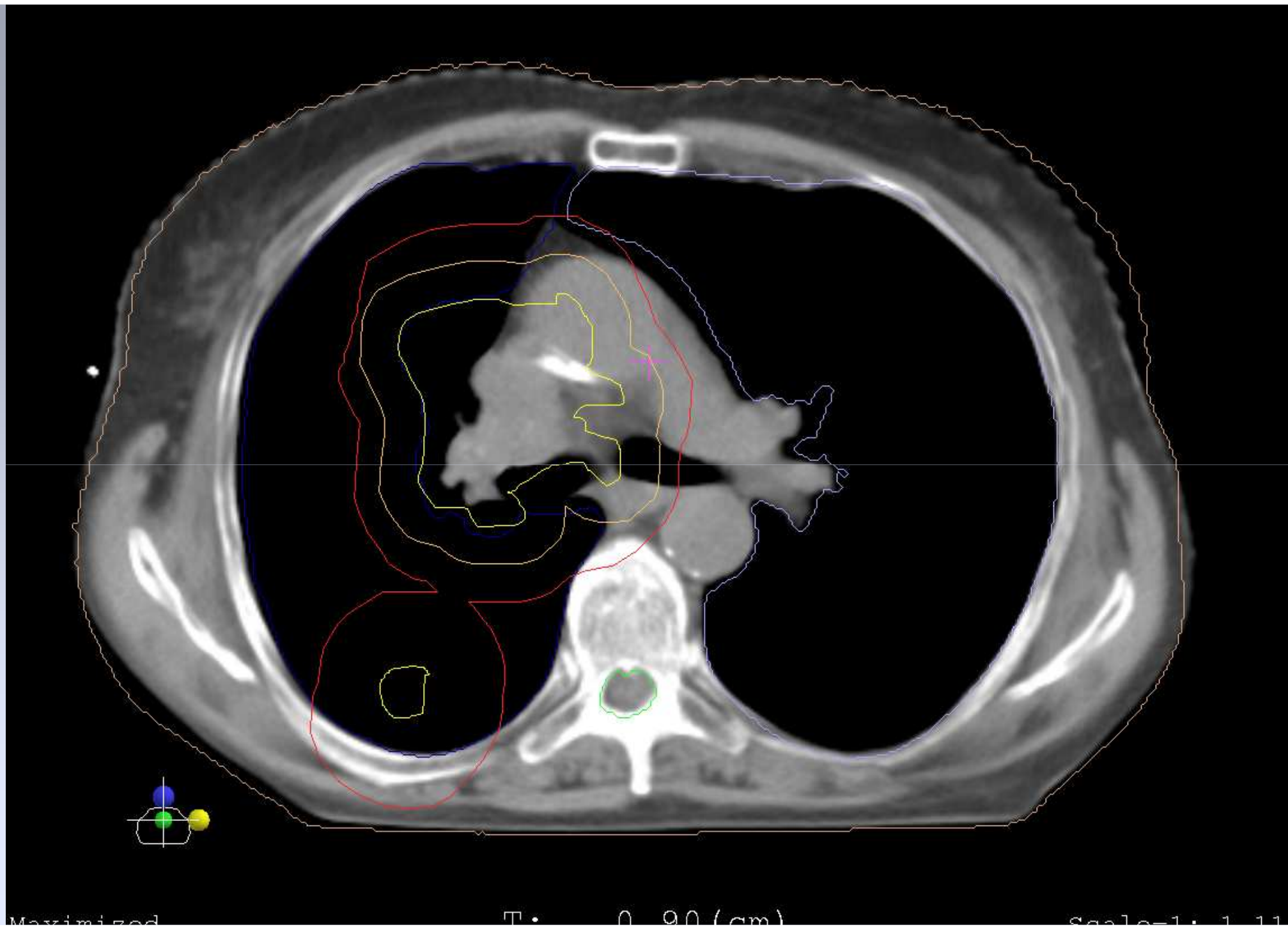


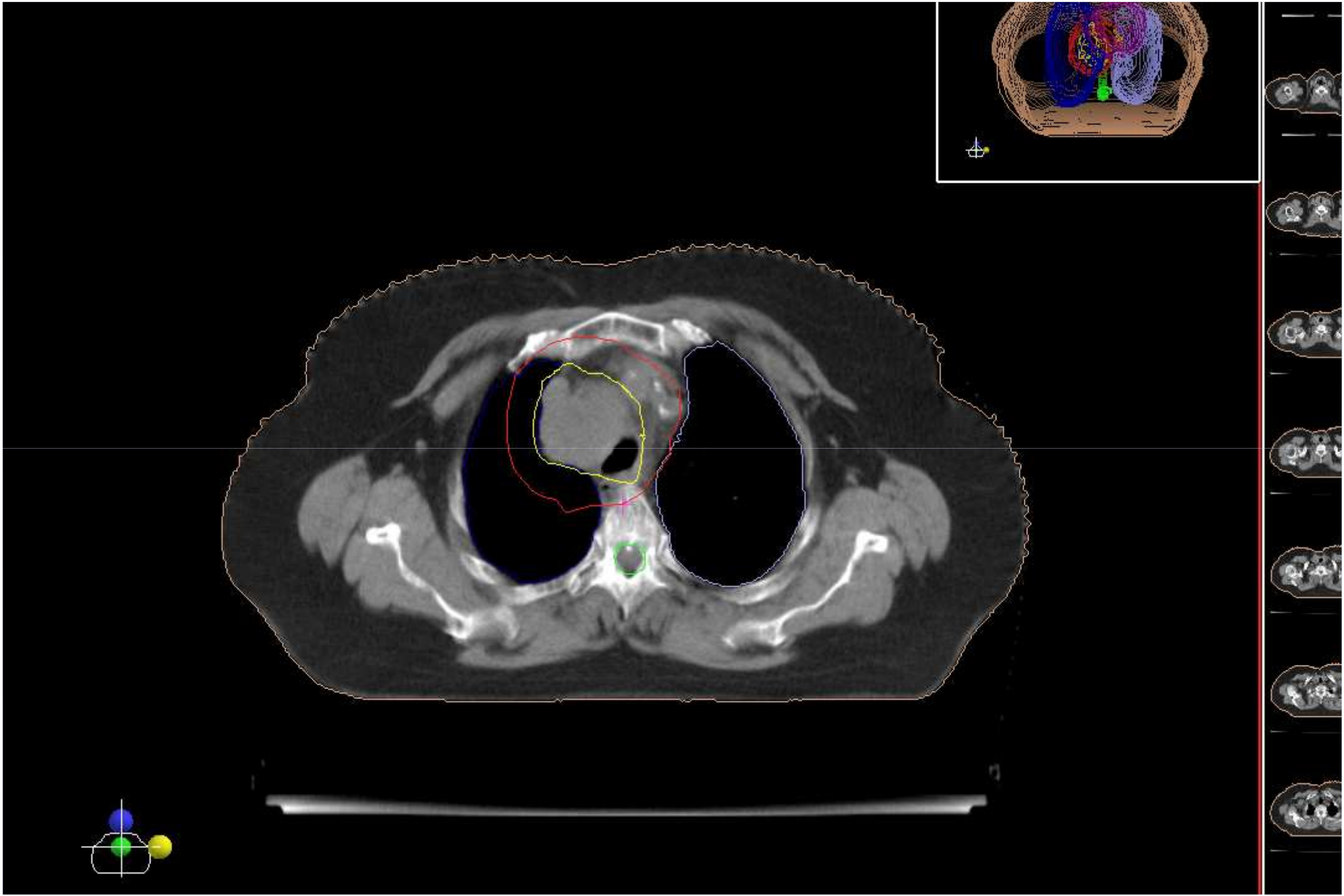
Maximized

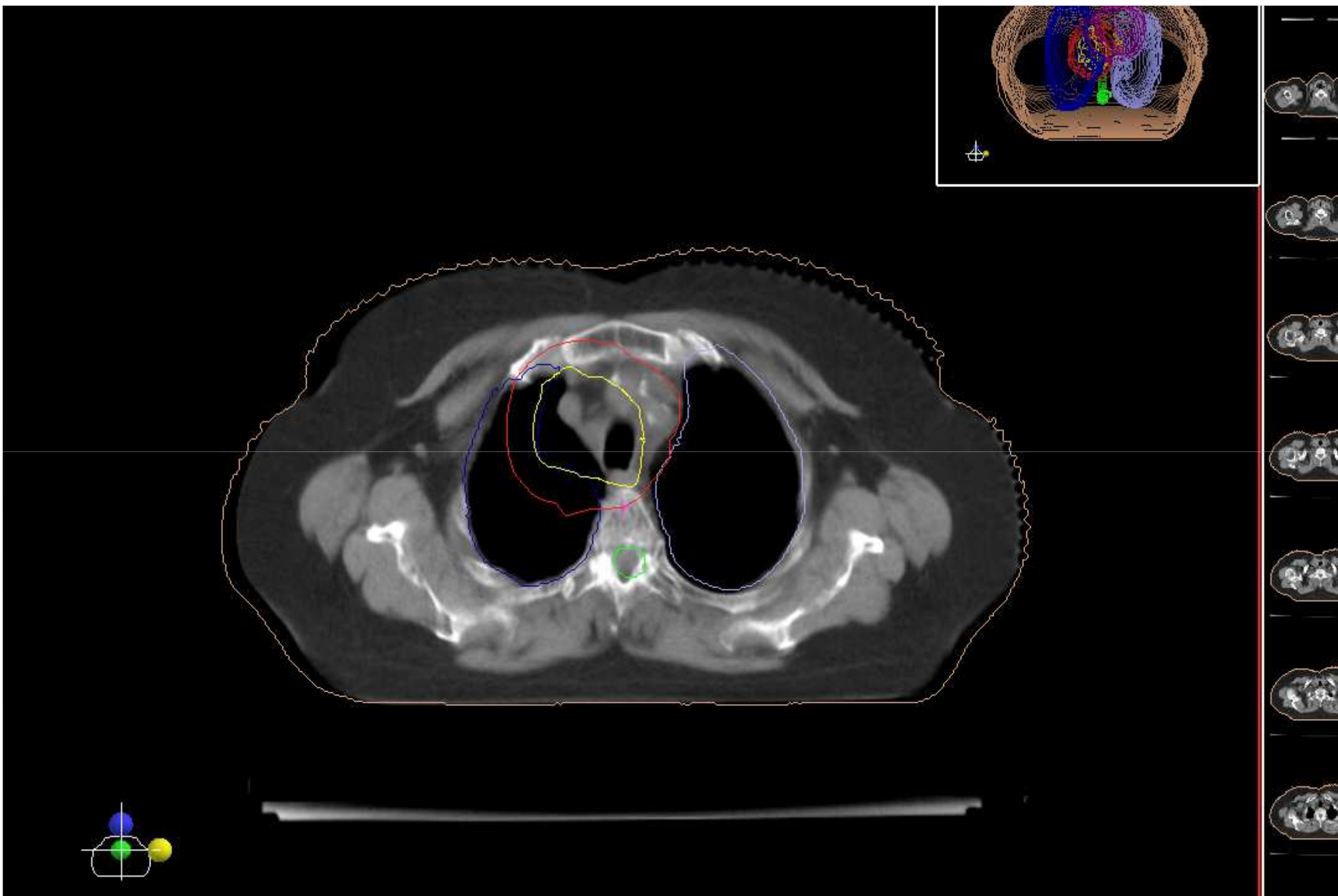
T: 1.90 (cm)

Scale=1: 1.11









Atommag részecskék

Nagy fizikai
szelektivitás

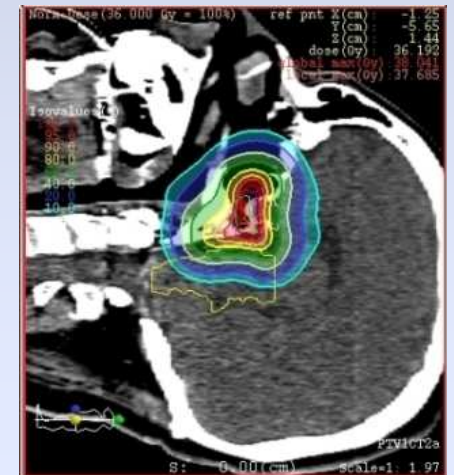
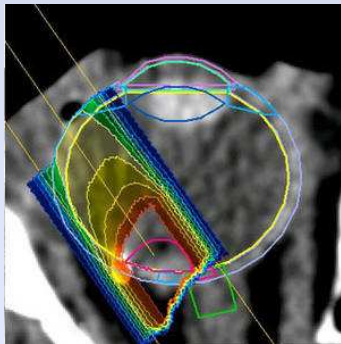
Proton

Magas LET,
nagy RBE

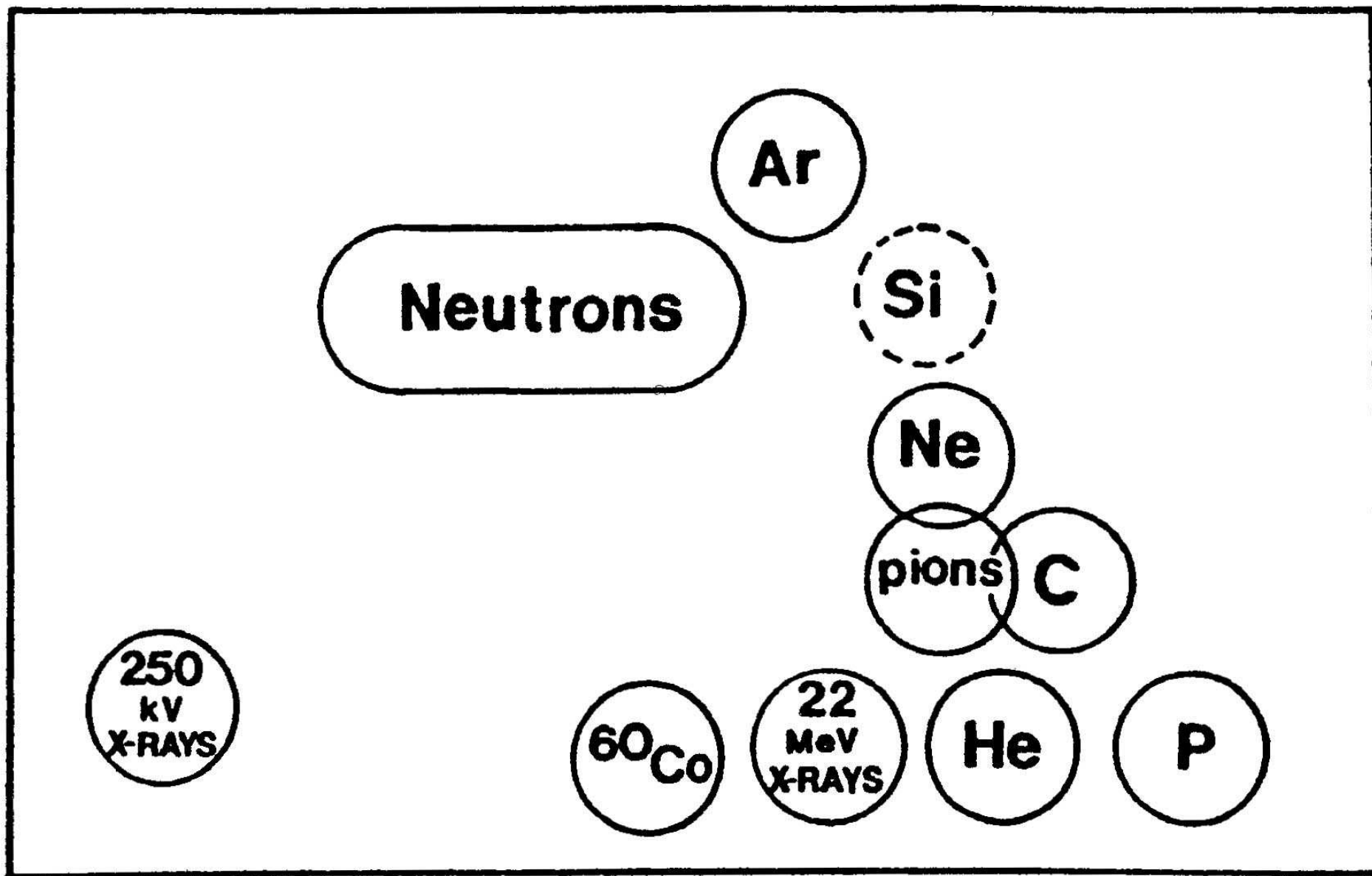
Neutron

Nehéz ionok:
Szén, Oxigén, Neon

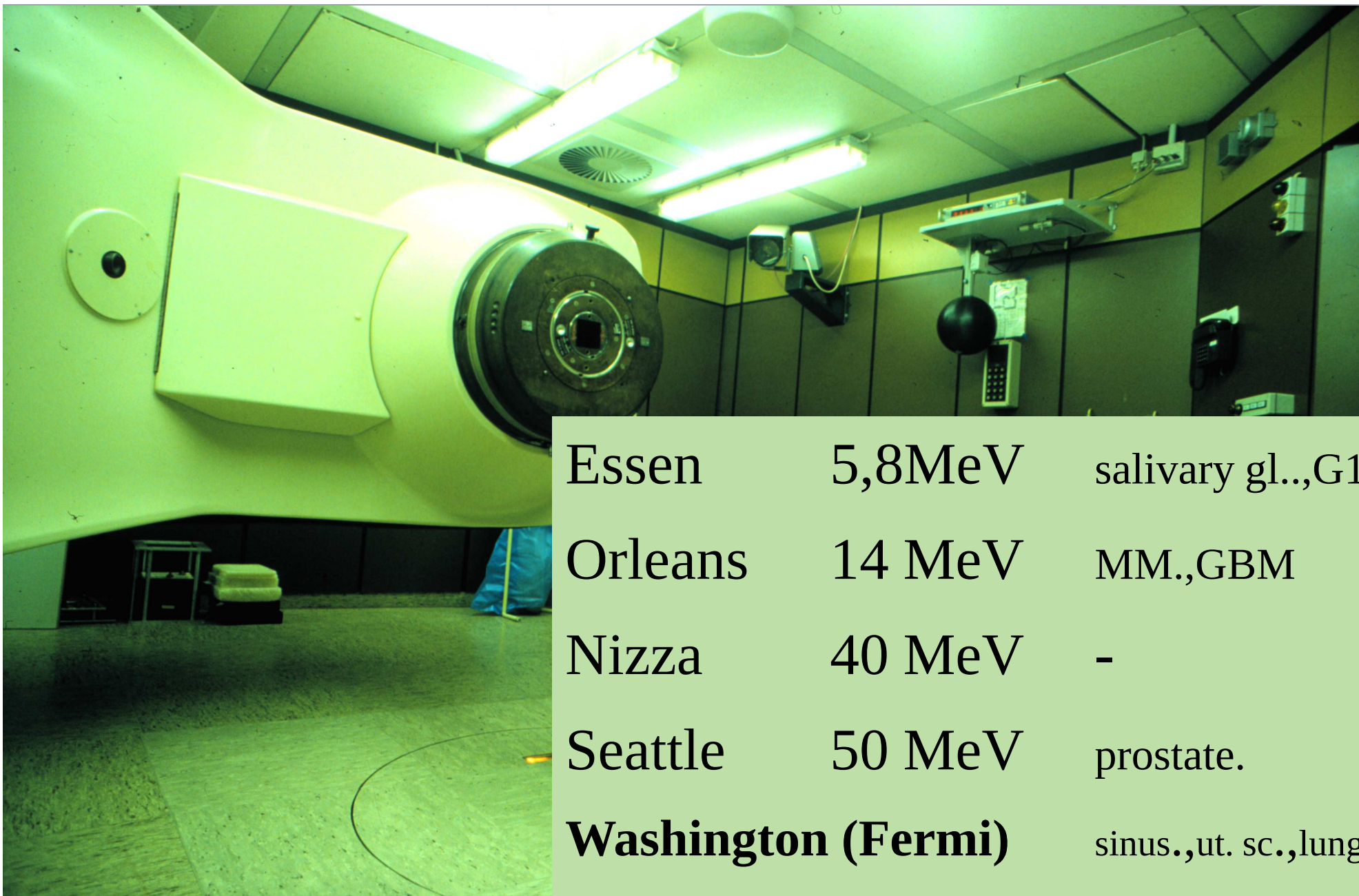
2010-ig >80.000 beteg



↑
LET

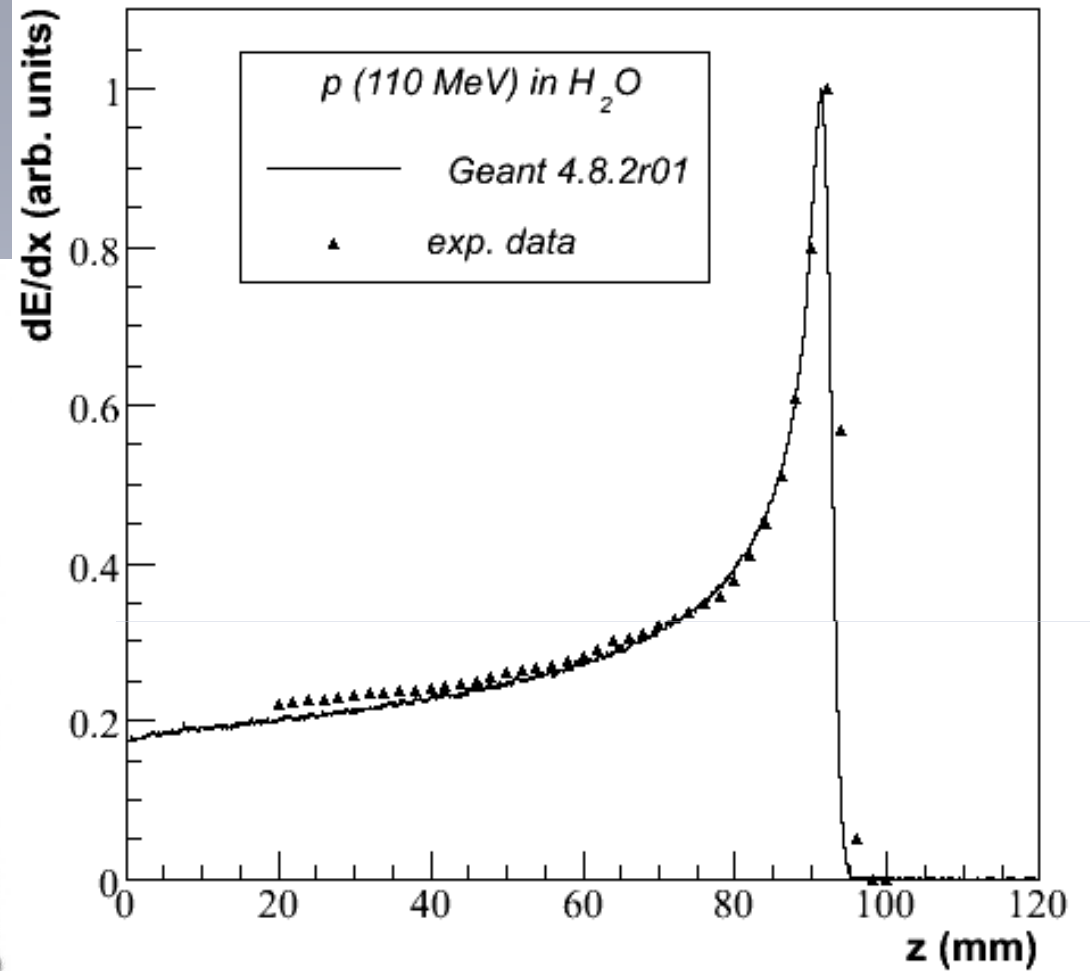
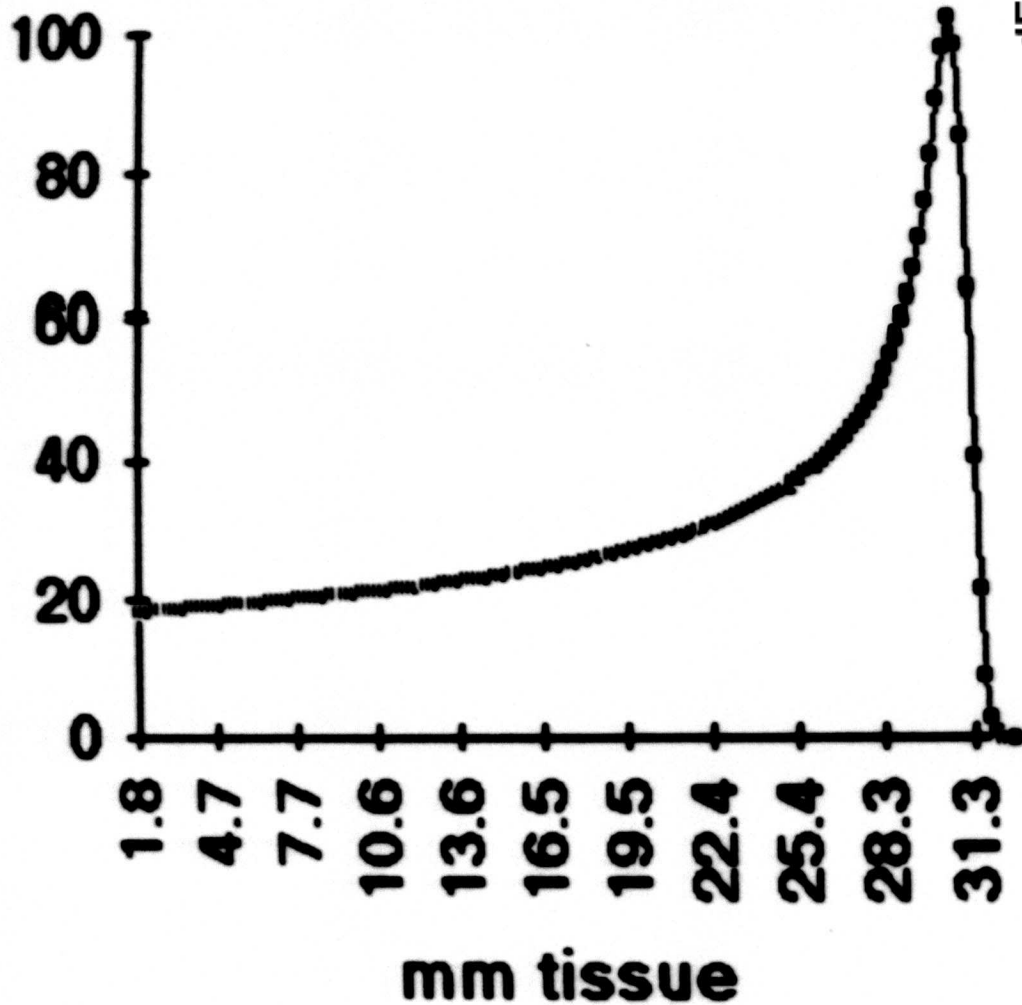


Quality of dose distribution →

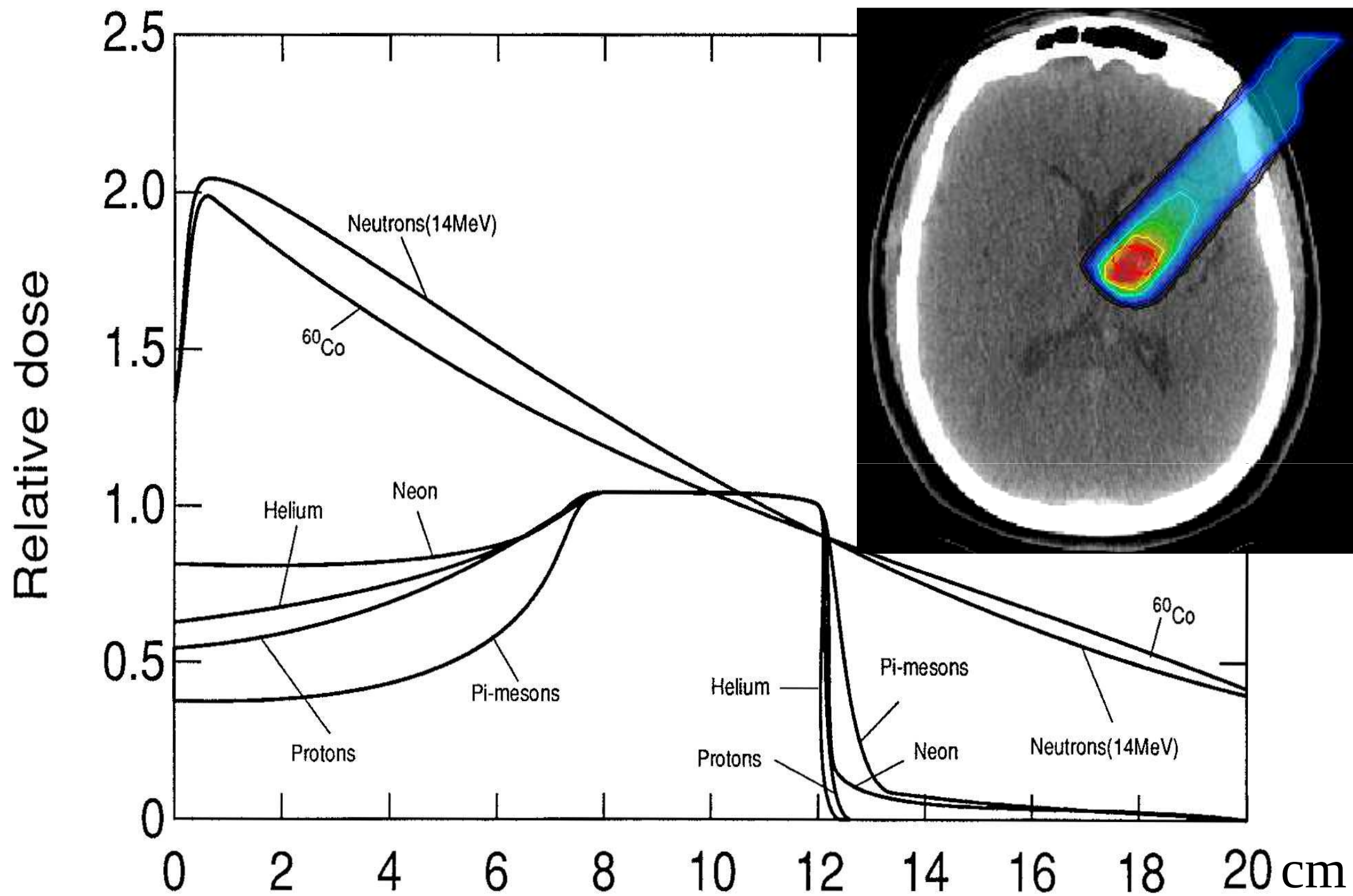


Essen	5,8MeV	salivary gl.,G1-2 sc.
Orleans	14 MeV	MM.,GBM
Nizza	40 MeV	-
Seattle	50 MeV	prostate.
Washington (Fermi)		sinus.,ut. sc.,lung
Faure	60 MeV	-“-

Töltött részecskék



Bragg Peak



A proton terápia története



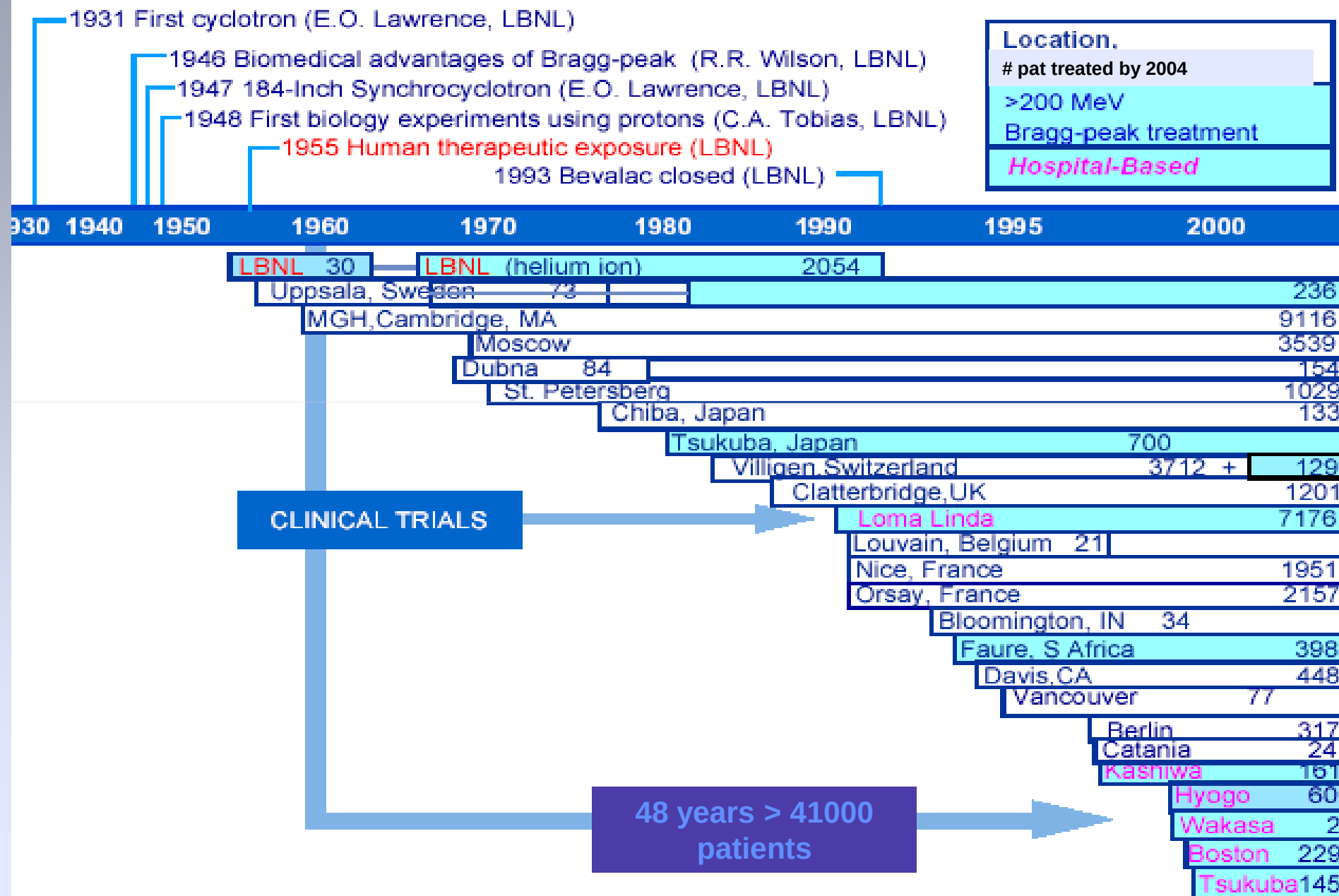
- 1946 Robert Wilson
- 1948 Tobias, Lawrence (Berkeley)(hypophysectomy)
- 1954-56 Boerje Larsson (Uppsala)
- 1960 Graffman 60 beteg.(Stereotactic neurosurgery)
- Early '60 Sweet, Koehler, (Kjellberg, Harvard)- AV. malform.
- 1969 Ganz (retinoblastoma), Constable (eye melanoma)
- 1970 Suit, Goitein (agyalapi daganatok), Oroszo, Japán (Tokio, Chiba)
- 1983 Tsukuba 250 MeV (tüdő, mediast, GI, Gyn,...)
- 1967 Első nagymezős proton besugárzás Svédországban
- 1974 Nagymezős frakcionált proton kezelési program /HCL, Cambridge
- 1990 Első hospital-based proton kezelési kp. - Loma Linda

Heidelberg Ion Therapy

HIT



Proton Therapy Scientific Milestones



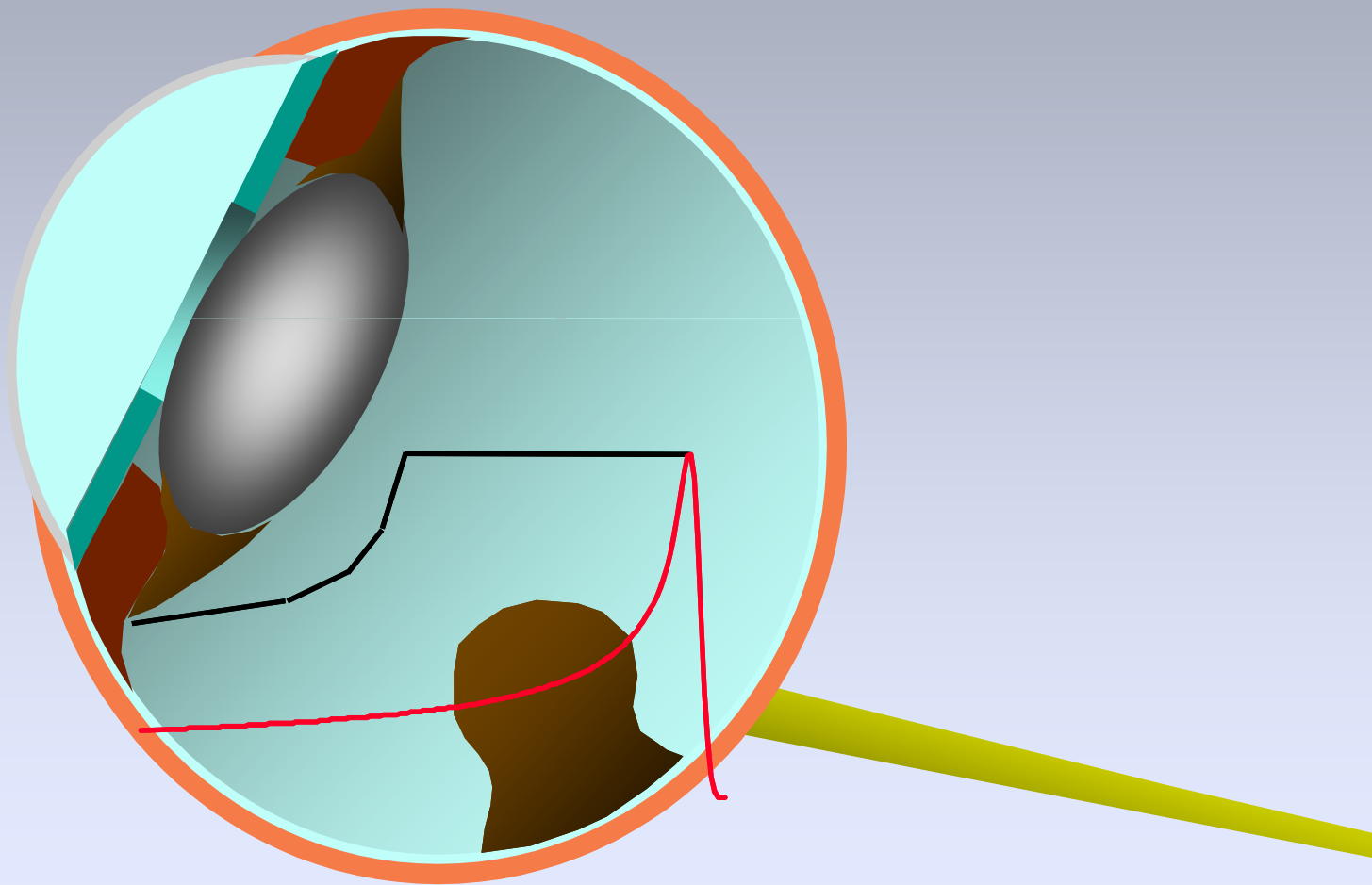
Patient Statistics (2011.május)

Canada Vancouver (TRIUMF)	p 1995	152	Dec-10	ocular tumors only
China Wanjie (WPTC)	<u>p 2004</u>	1078	Dec-10	
China Lanzhou	<u>C ion 2006</u>	126	Dec-10	
England Clatterbridge	p 1989	2021	Dec-10	ocular tumors only
France Nice (CAL)	p 1991	4209	Dec-10	ocular tumors only
France Orsay (CPO)	p 1991	5216	Dec-10	4245 ocular tumors
Germany Berlin (HMI)	p 1998	1660	Dec-10	ocular tumors only
Germany Munich (RPTC)	<u>p 2009</u>	446	Dec-10	
Germany HIT, Heidelberg	<u>C ion 2010</u>	400	Dec-10	estimate; has to be confirmed
Germany HIT, Heidelberg	<u>p 2010</u>	40	Dec-10	estimate; has to be confirmed
Italy Catania (INFN-LNS)	<u>p 2002</u>	174	Mar-09	ocular tumors only
Japan Chiba (HIMAC)	<u>C ion 1994</u>	5497	Aug-10	
Japan Kashiwa (NCC)	p 1998	772	Dec-10	
Japan Hyogo (HIBMC)	p 2001	2382	Nov-09	
Japan Hyogo (HIBMC)	<u>C ion 2002</u>	638	Nov-09	
Japan Tsukuba (PMRC, 2)	p 2001	1849	Dec-10	
Japan Shizuoka	p 2003	986	Dec-10	
Korea Ilsan, Korea	<u>p 2007</u>	648	Dec-10	
Russia Moscow (ITEP)	p 1969	4246	Dec-10	
Russia St. Petersburg	p 1975	1362	Dec-10	
Russia Dubna (JINR, 2)	p 1999	720	Dec-10	
South Africa iThemba LABS p 1993		511	Dec-09	
Sweden Uppsala (2)	p 1989	1000	Dec-10	
Switzerland Villigen PSI, incl OPTIS2	p 1996	772	Dec-10	47 ocular tumors
CA., USA UCSF - CNL	p 1994	1285	Dec-10	ocular tumors only
CA., USA Loma Linda (LLUMC)	p 1990	15000	Jan-11	
IN., USA Bloomington (MPRI, 2)	<u>p 2004</u>	1145	Dec-10	
MA., USA Boston (NPTC)	p 2001	4967	Dec-10	
TX, USA Houston	<u>p 2006</u>	2700	Dec-10	about 500 with scanning
FL, USA UFPTI Jacksonville	<u>p 2006</u>	2679	Dec-10	
OK, USA Oklahoma City (ProCure PTC)	<u>p 2009</u>	21	Dec-09	
IL, USA CDH Warrenville	<u>p 2010</u>		Oct-10	

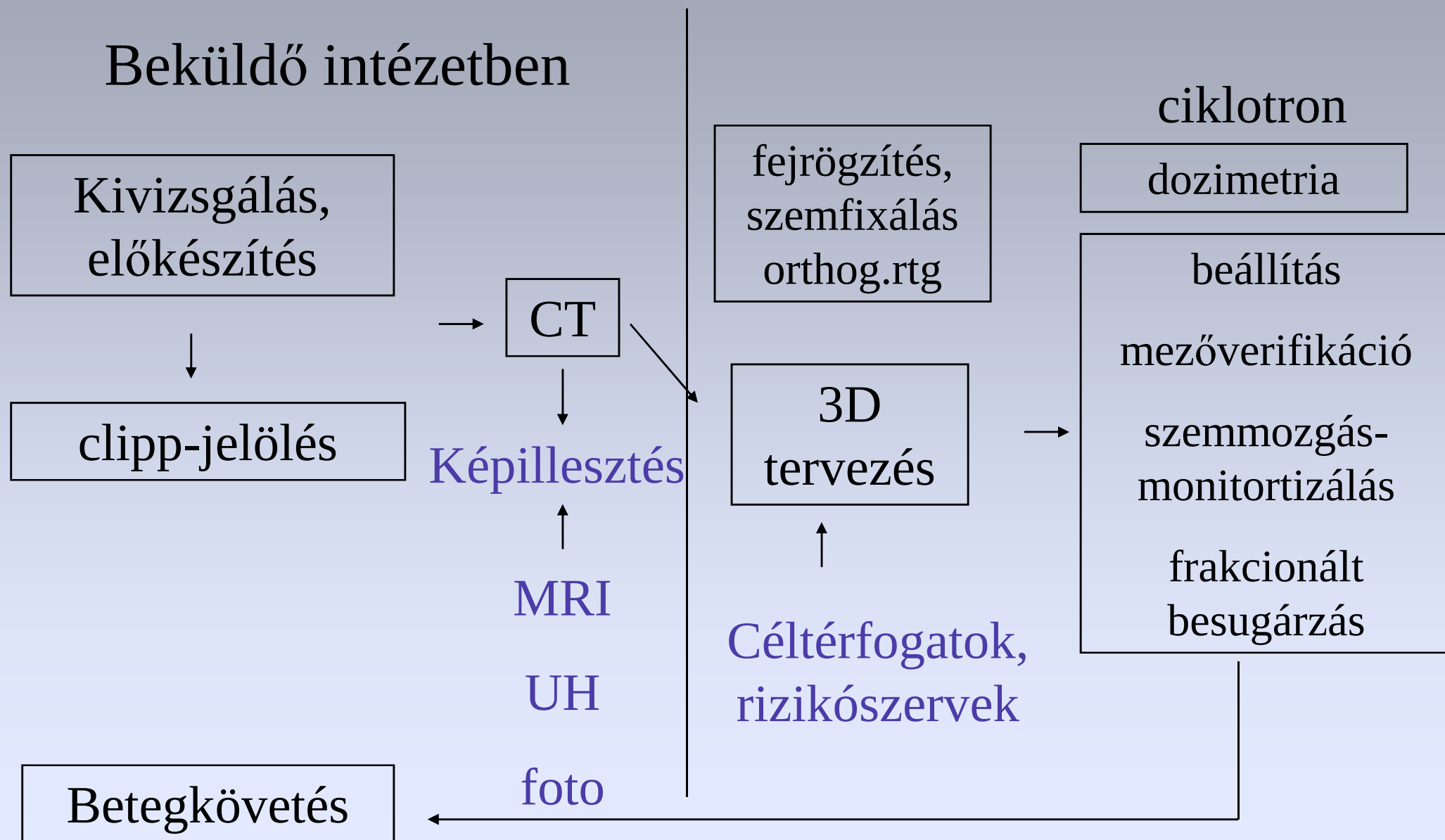
84492 Grand Total

64702 Total = 6661 C-ions + 58041 protons

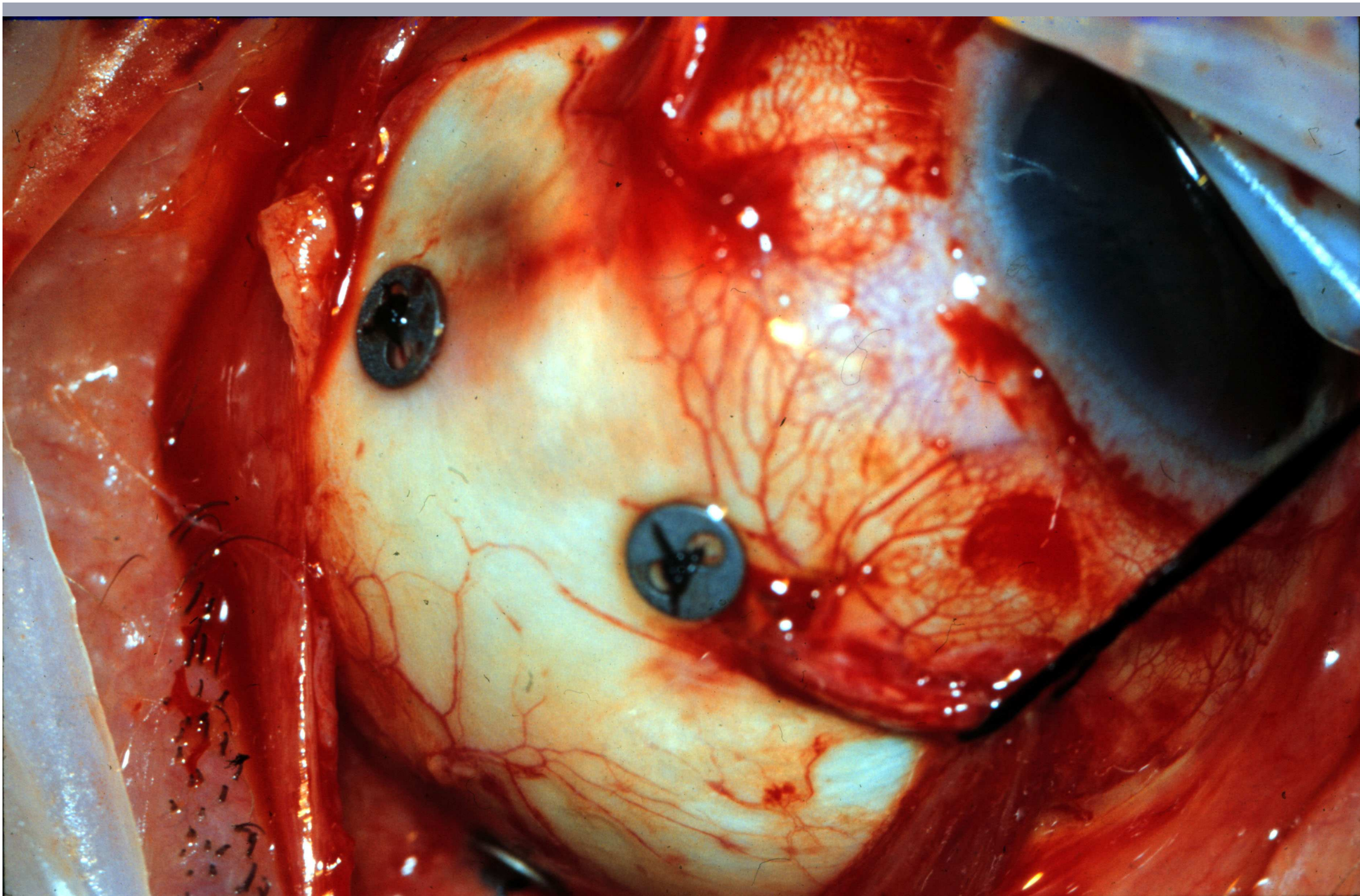
Szem melanoma - proton terápia



A protonterápia folyamatai





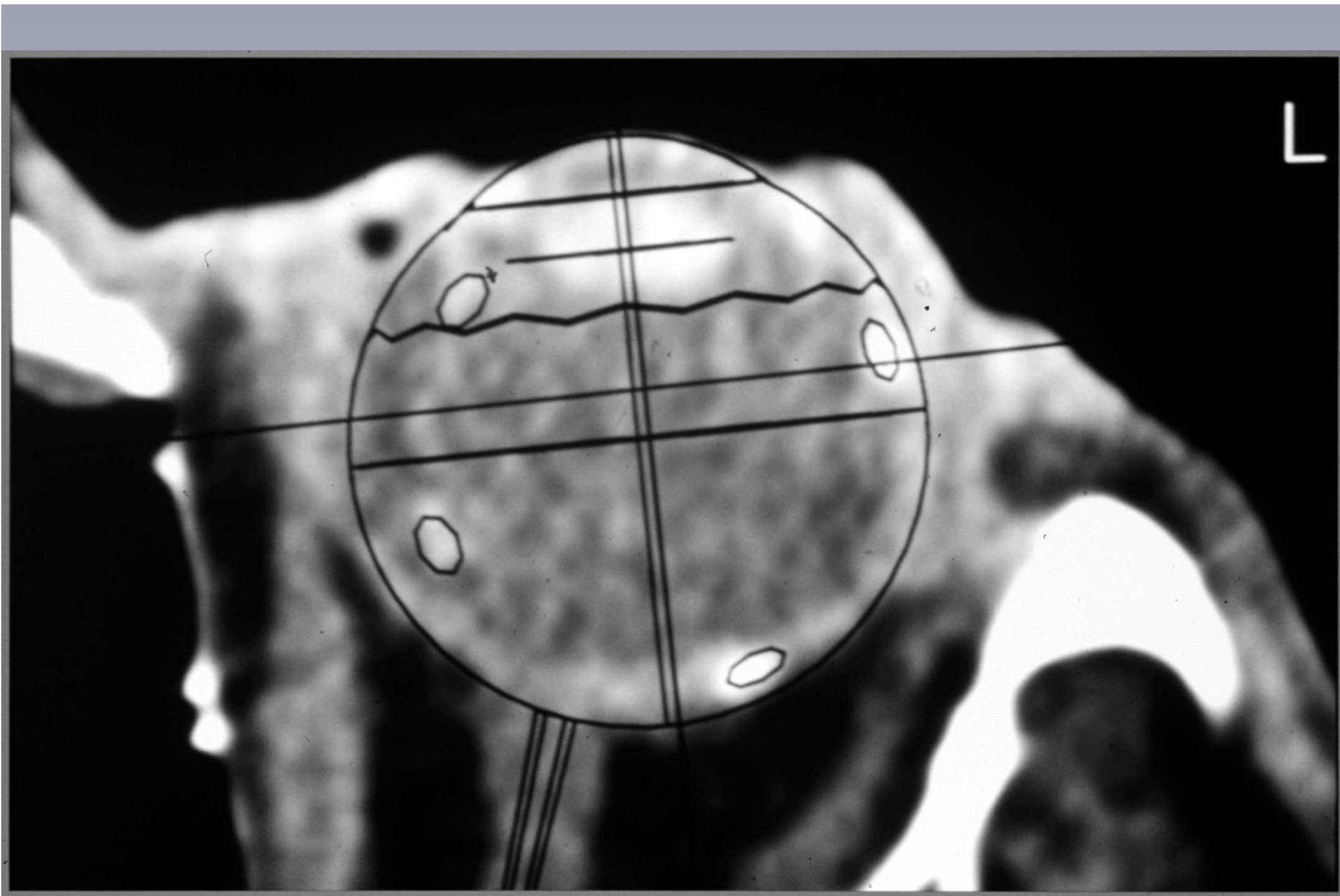


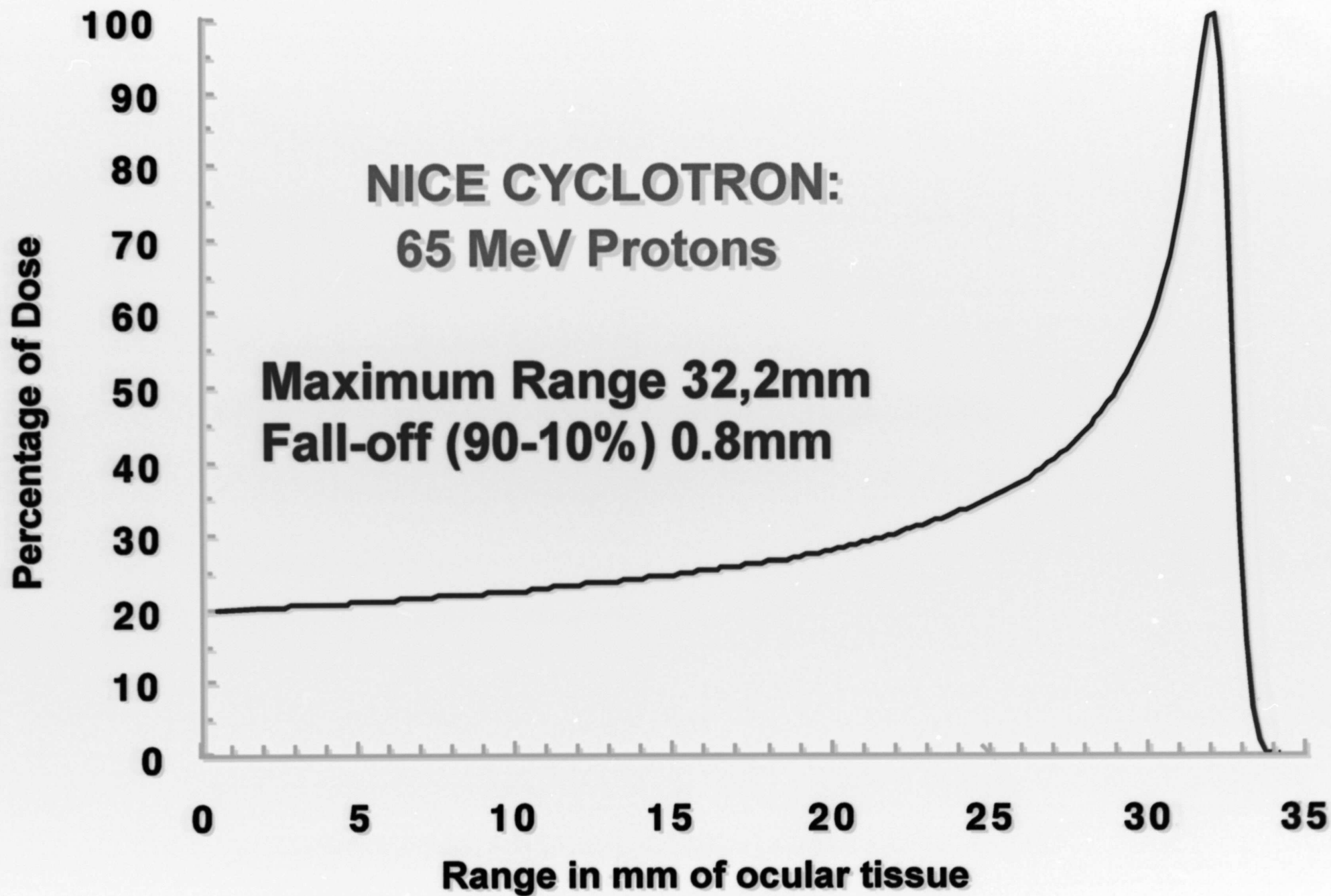
TI 2*2
mA 125
kV 120
SL 1
GT 0
ZO 4.0
CE -32
-129
AH 7572
21-OCT-97

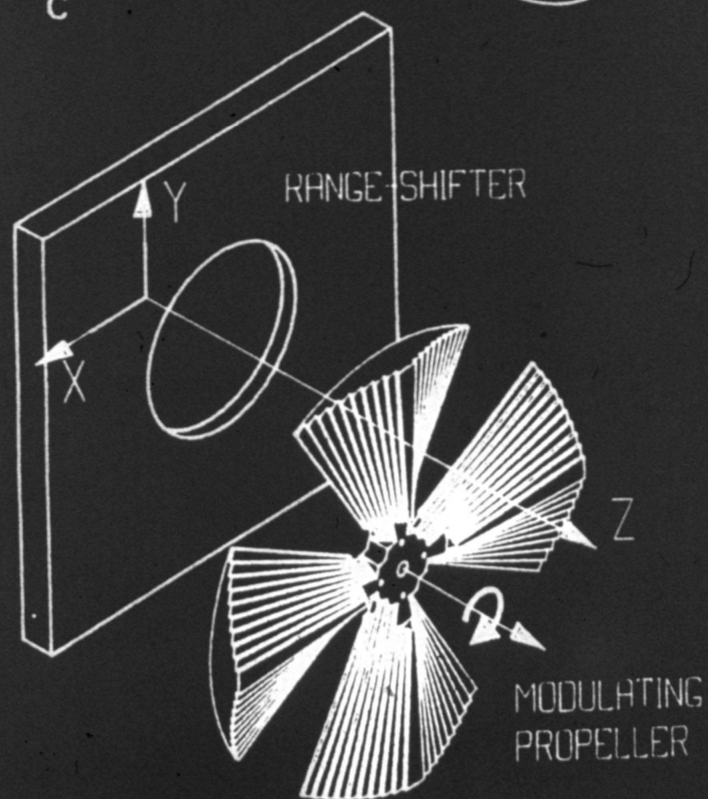
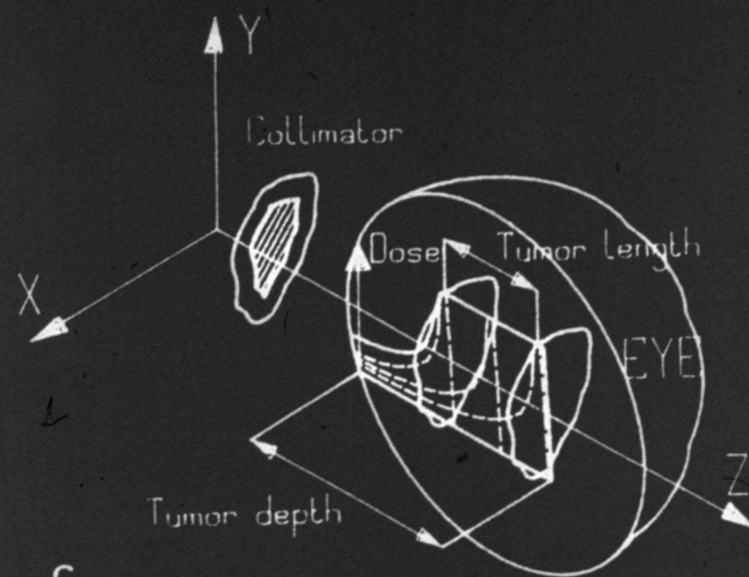
Ahmm
post op

W 260
C 51







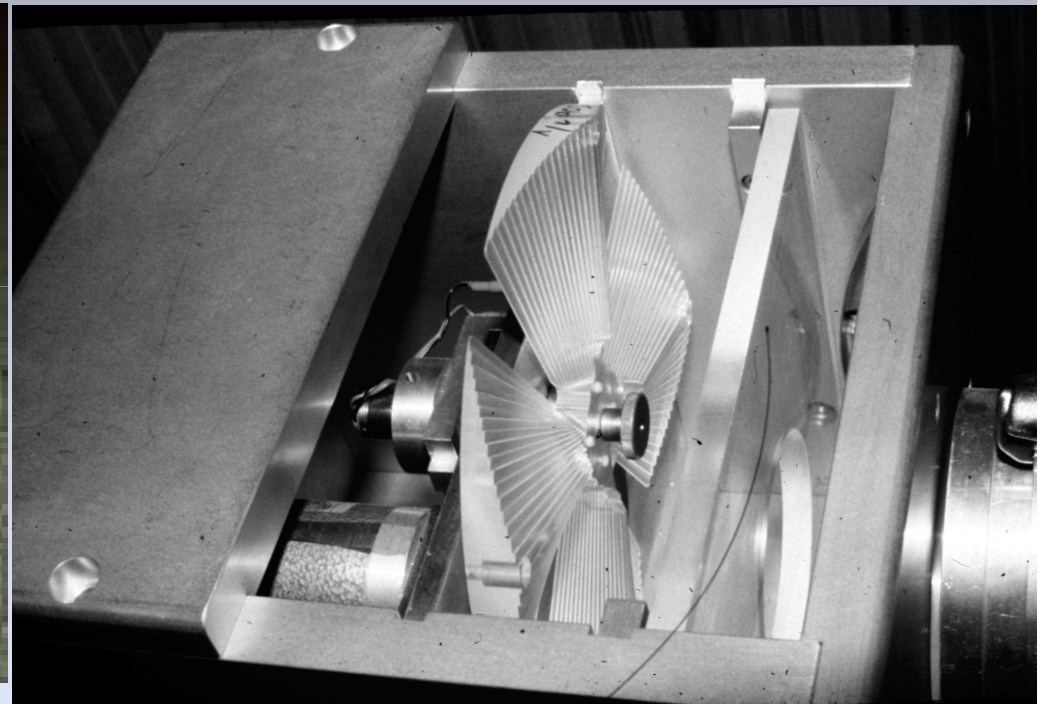


Proton Beam Shaping Devices



Wax bolus

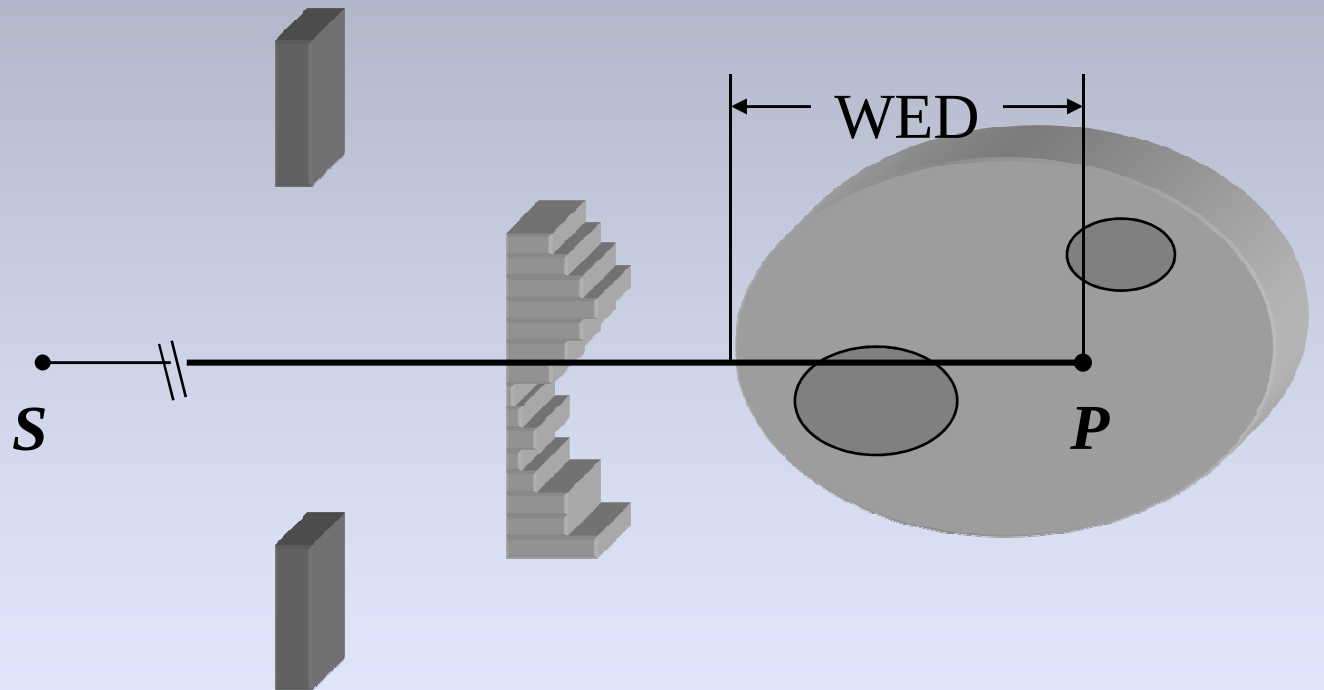
Cerrobend aperture



Modulating wheels

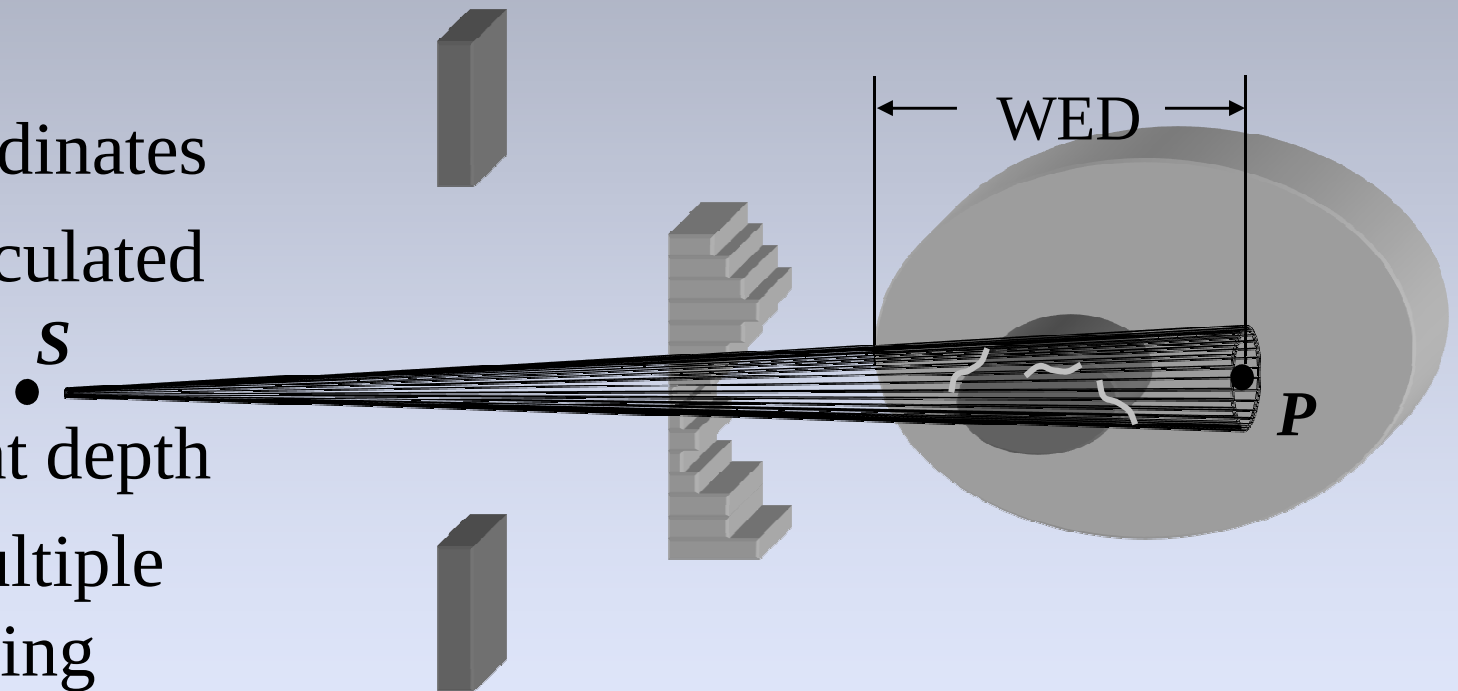
Ray-Tracing Dose Algorithm

- One-dimensional dose calculation
- Water-equivalent depth (WED) along single ray SP
- Look-up table
- Reasonably accurate for simple heterogeneities
- Simple and fast



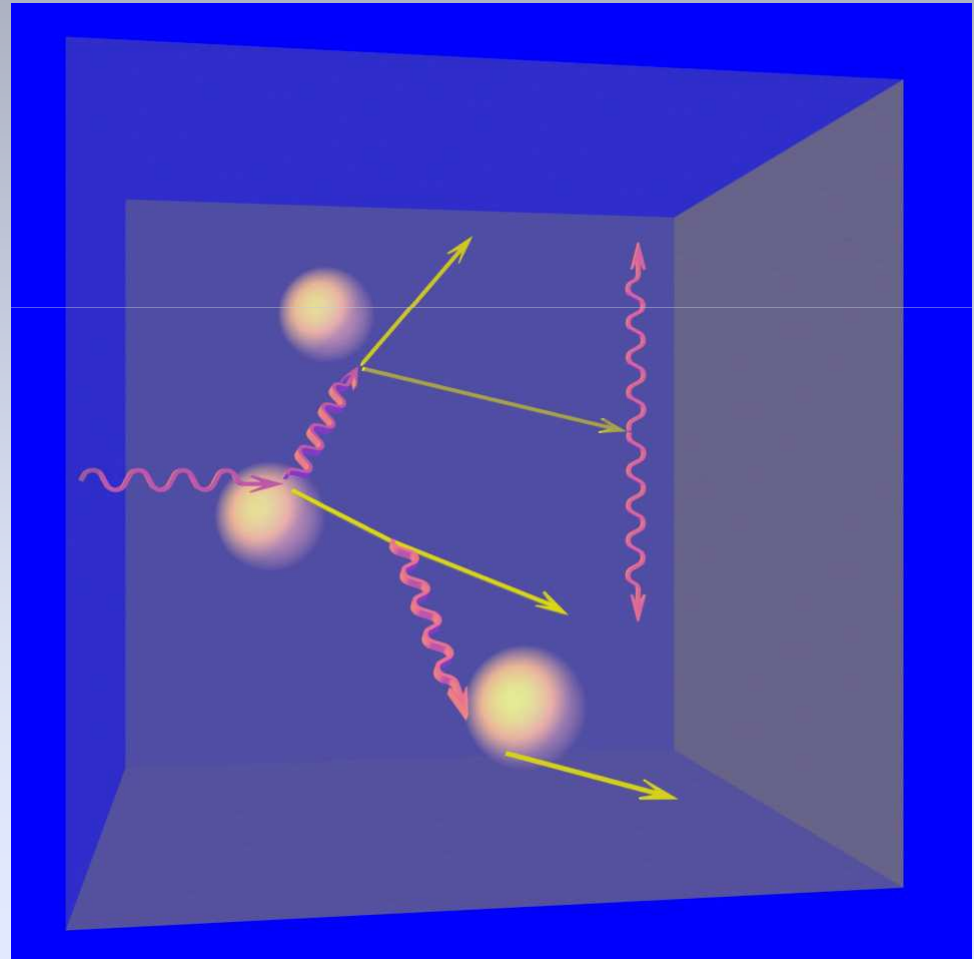
Pencil Beam Dose Algorithm

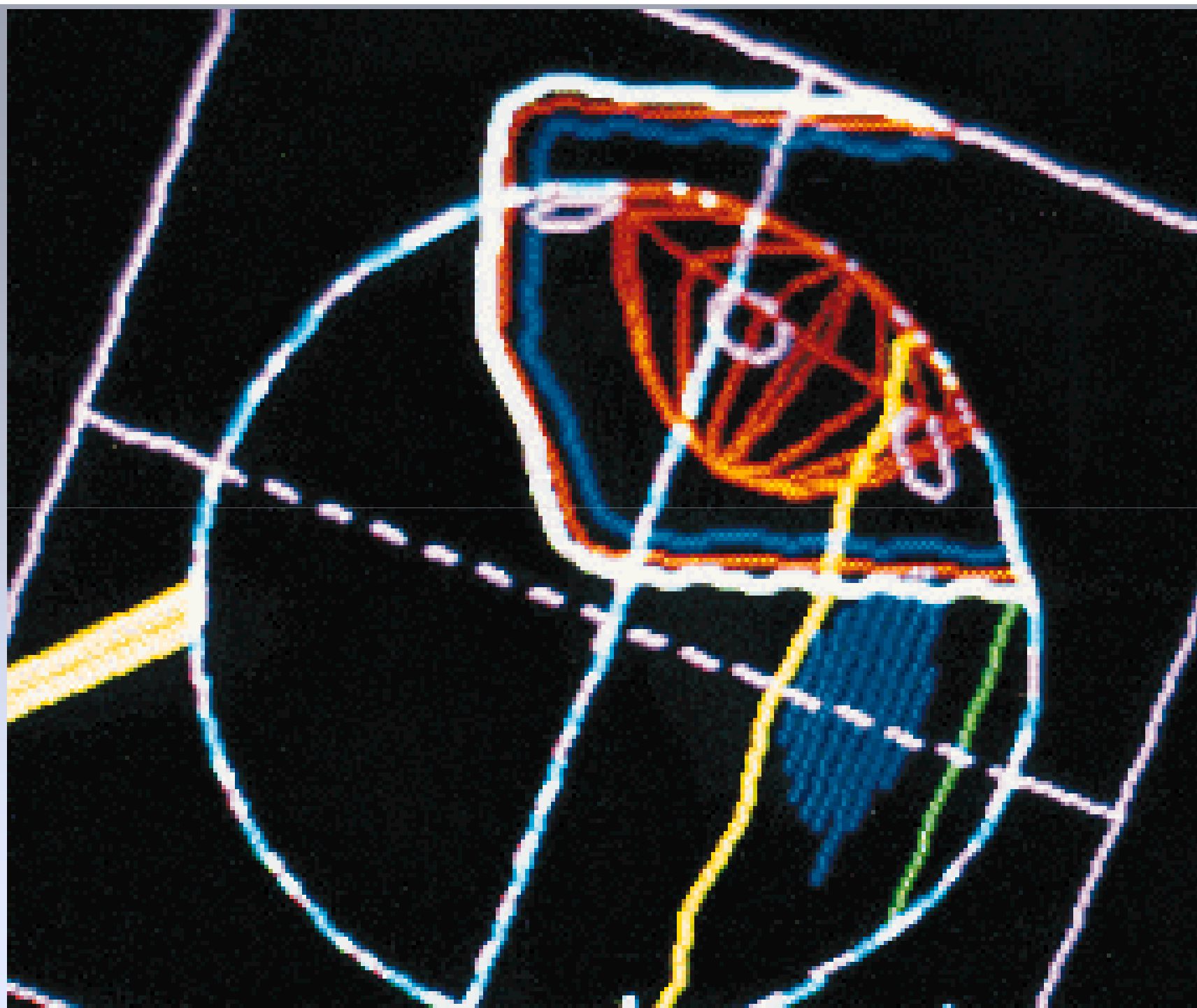
- Cylindrical coordinates
- Measured or calculated pencil kernel
- Water-equivalent depth
- Accounts for multiple Coulomb scattering
- more time consuming



Monte Carlo Dose Algorithm

- Considered as “gold standard”
- Accounts for all relevant physical interactions
- Follows secondary particles
- Requires accurate cross section data bases
- Includes source geometry
- Very time consuming



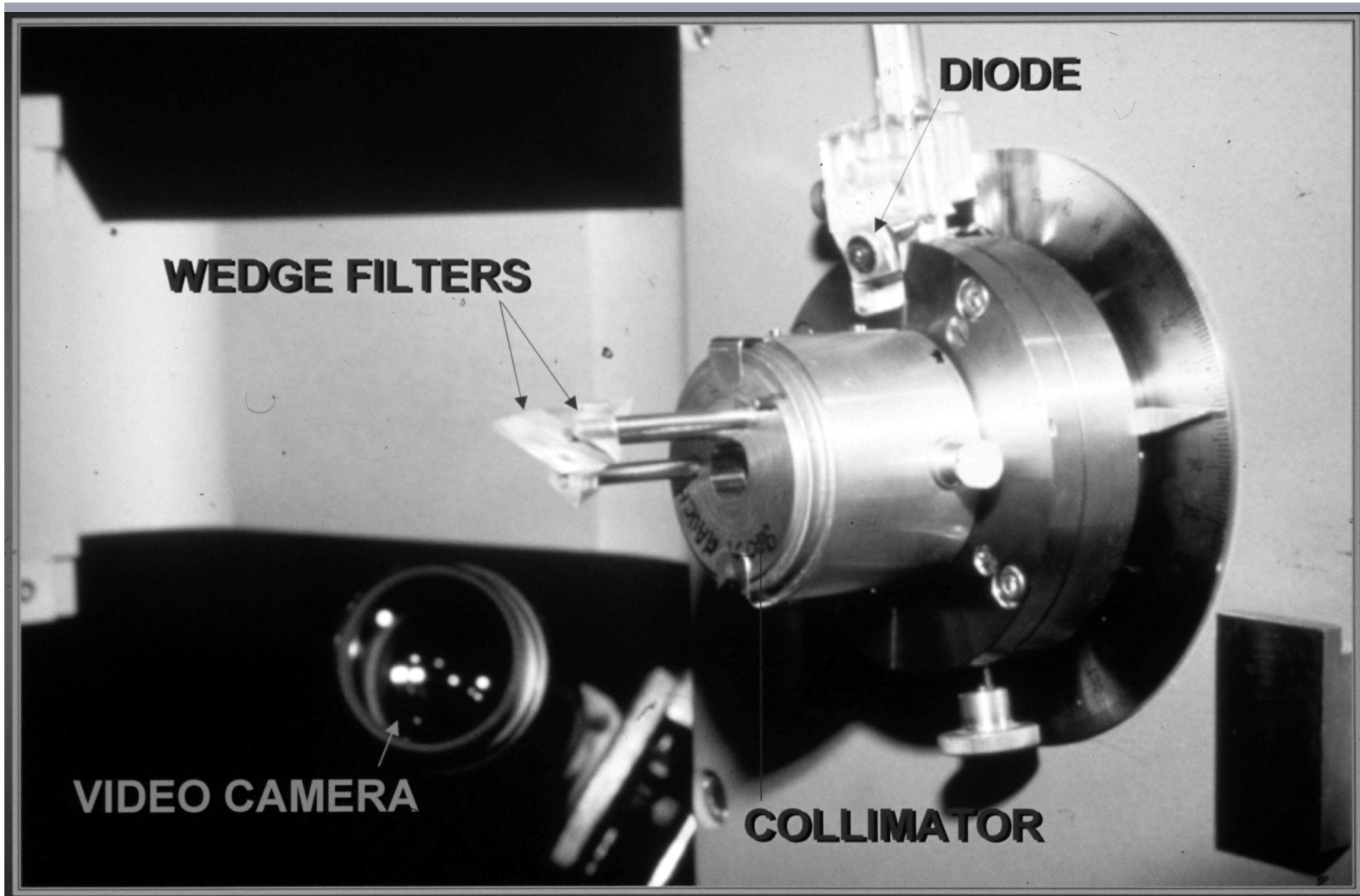


WEDGE FILTERS

DIODE

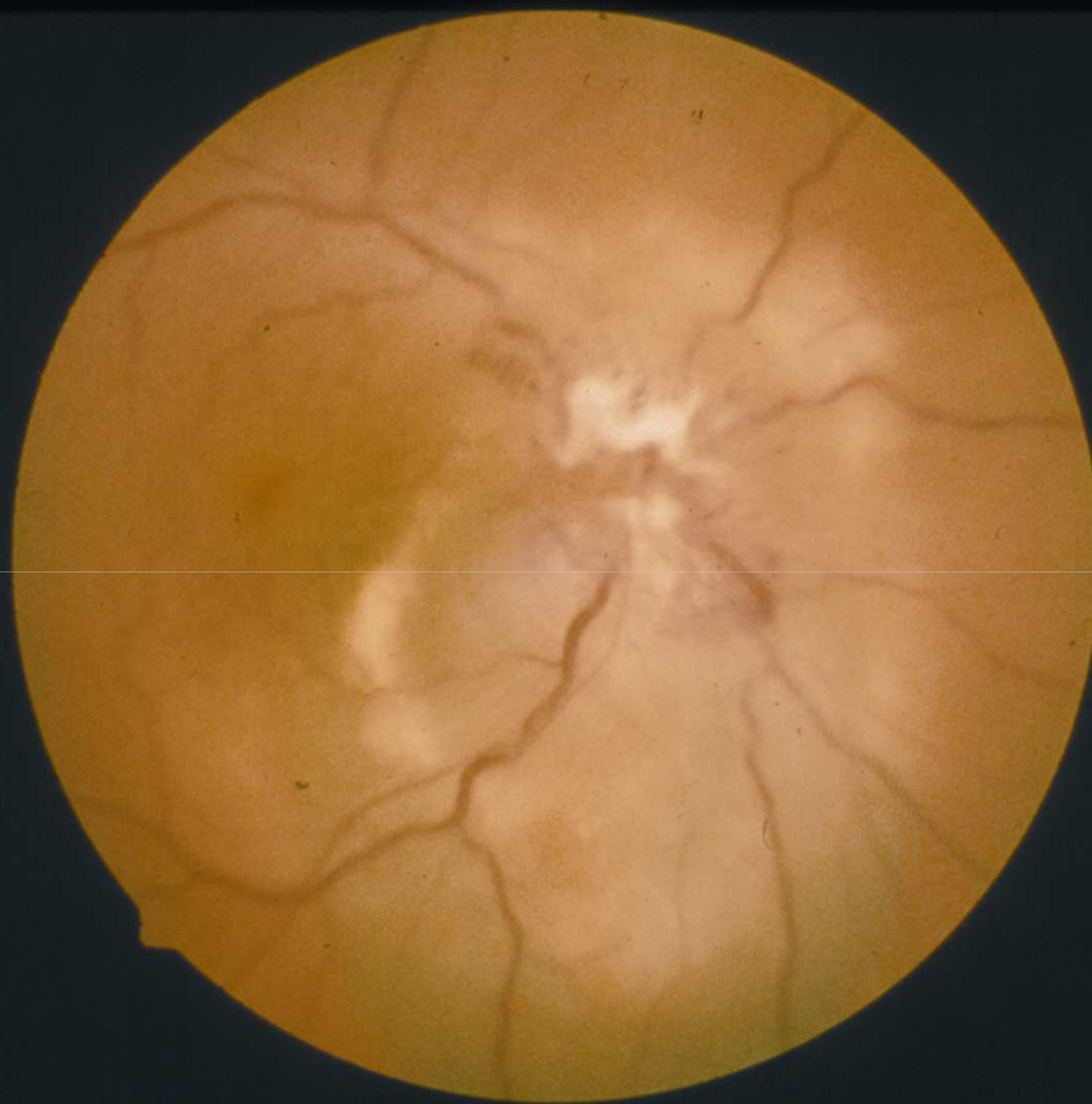
VIDEO CAMERA

COLLIMATOR

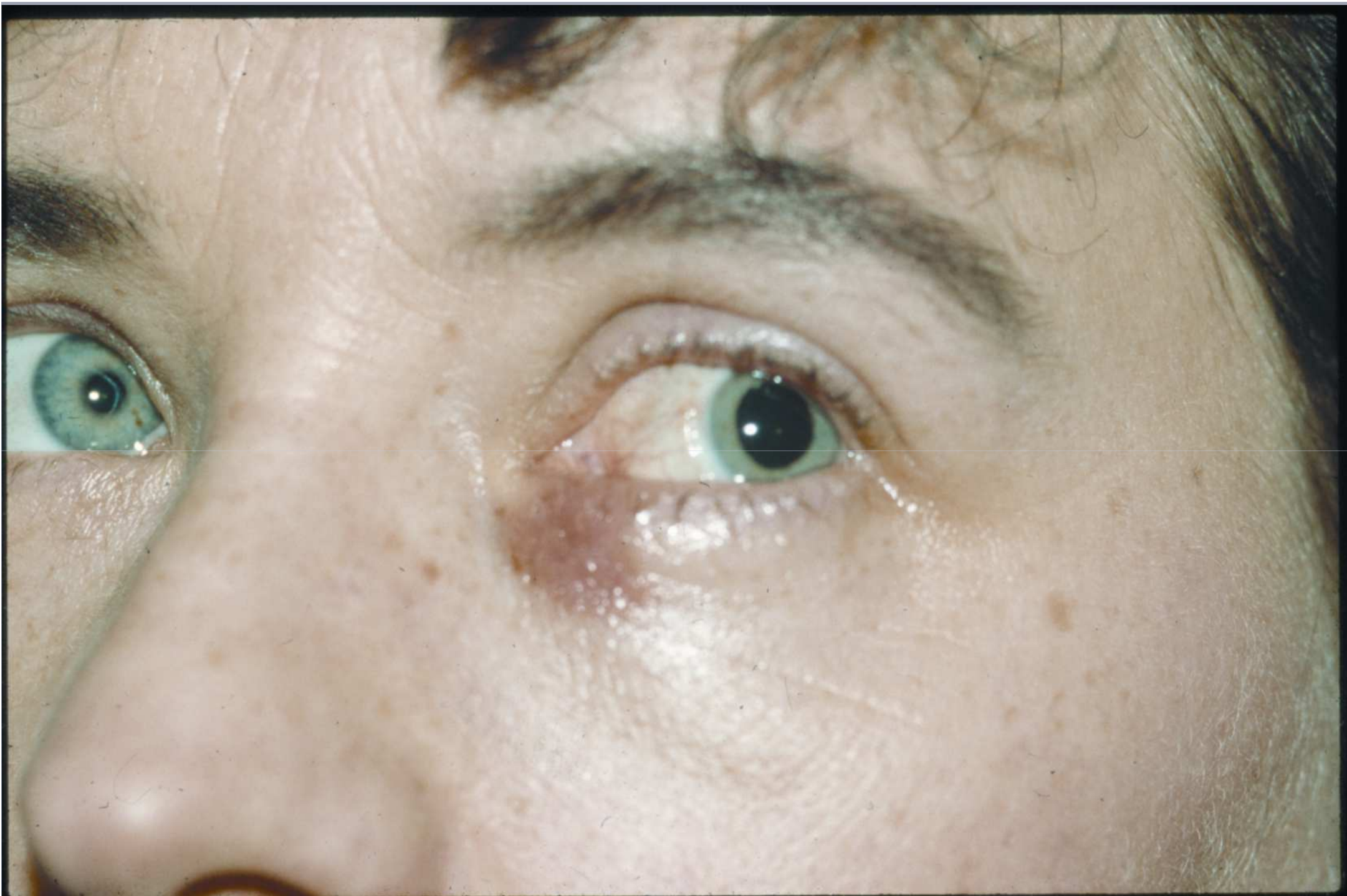


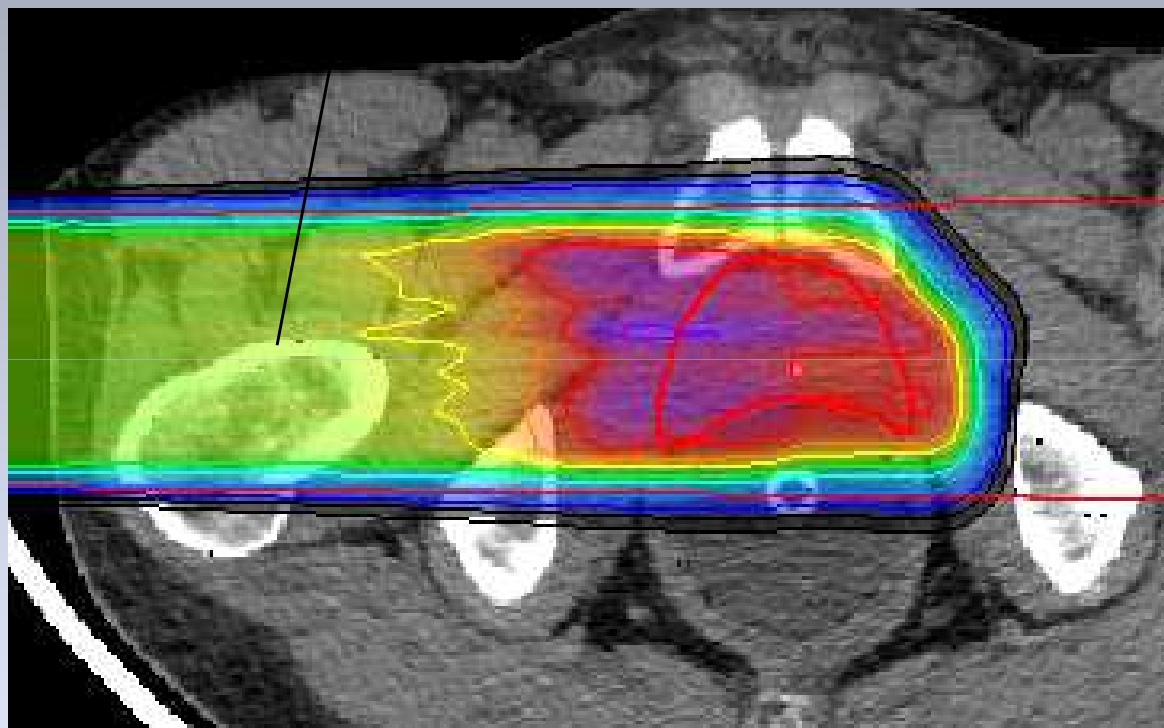
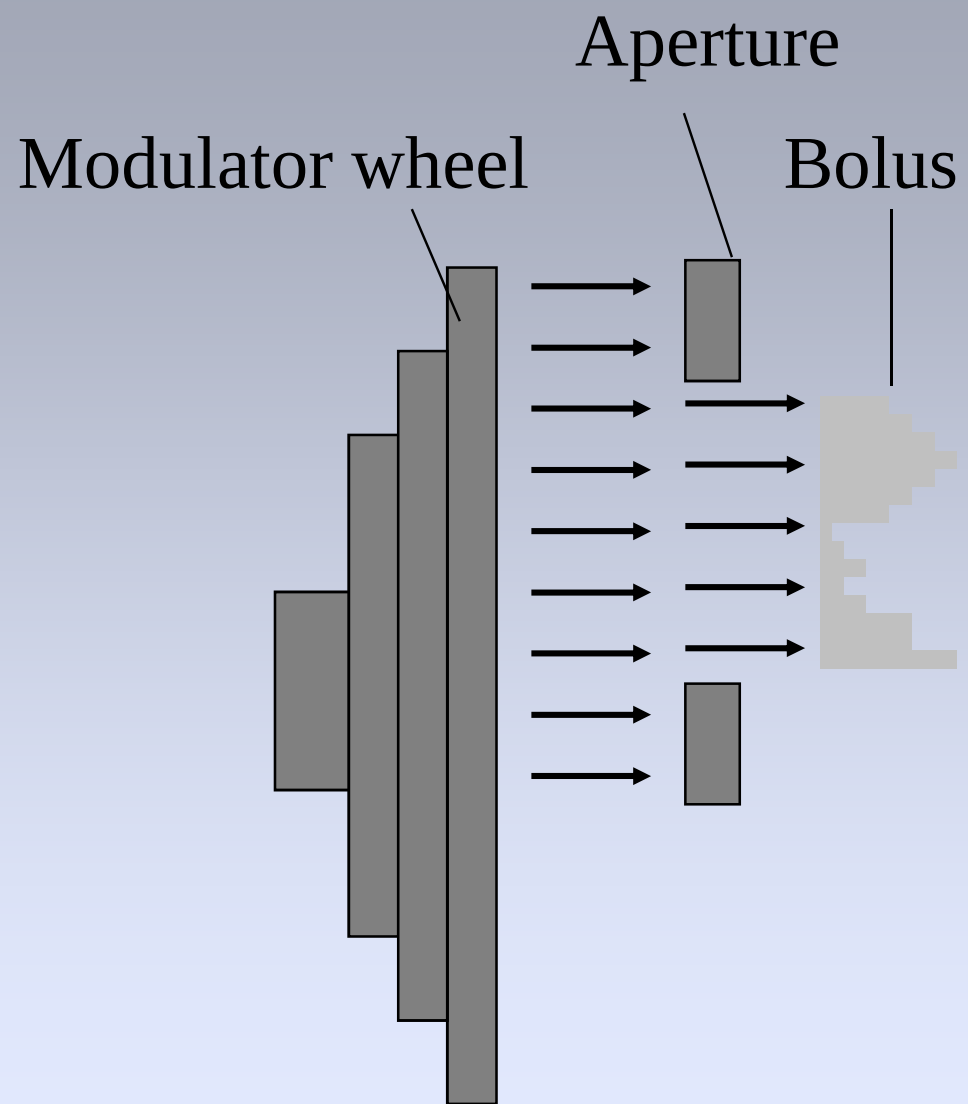












Hug E.B., Sweeney R.A., Nurre P.M., Holloway K.C., Slater J.D., Munzenrider J.E.

Proton radiotherapy in management of pediatric base of skull tumors

Int J Radiat Oncol Biol Phys. 2002 Vol. 52, No.4, pp 1017-1024

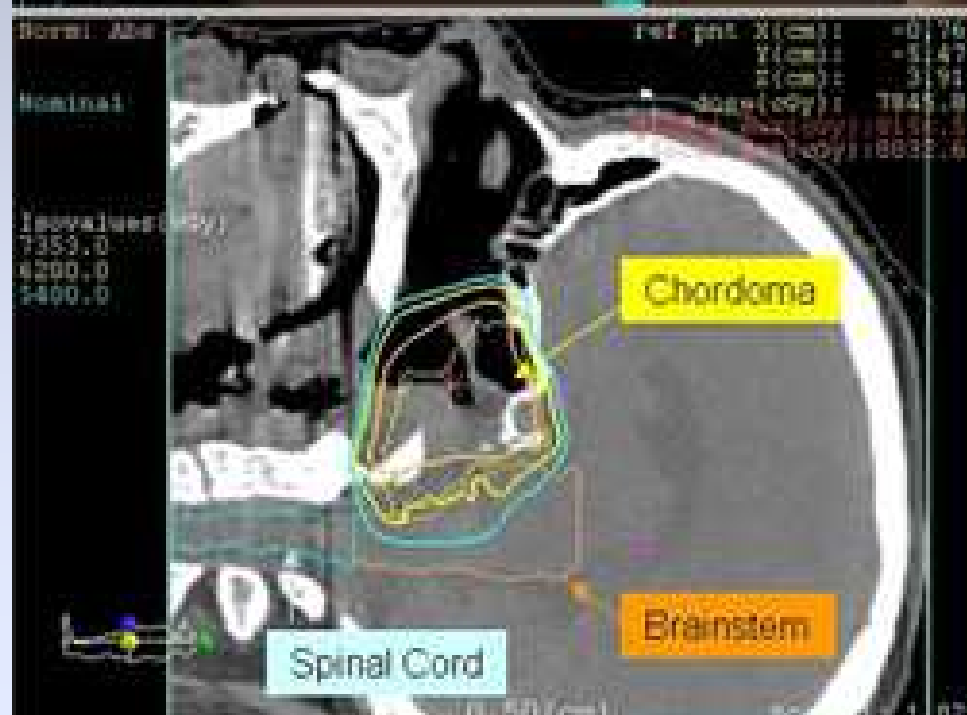
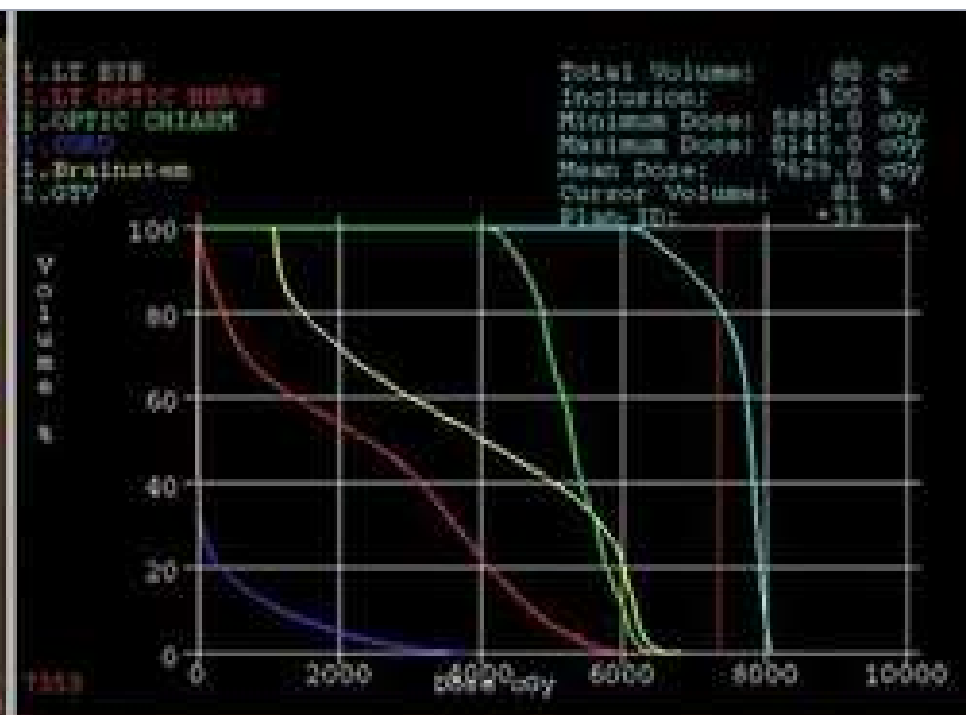
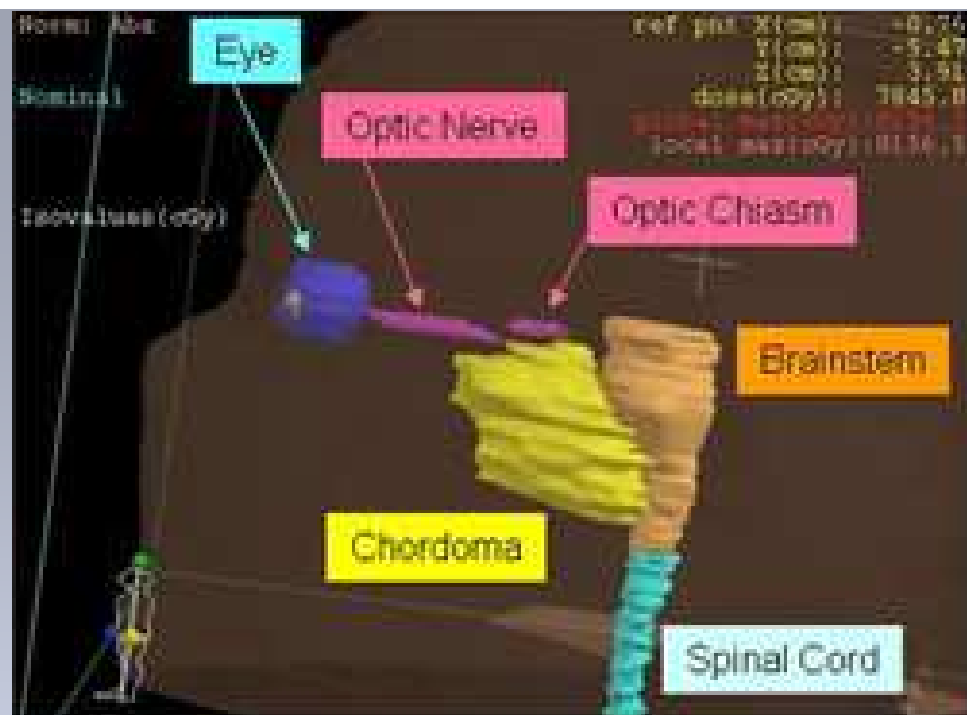
Locally advanced disease

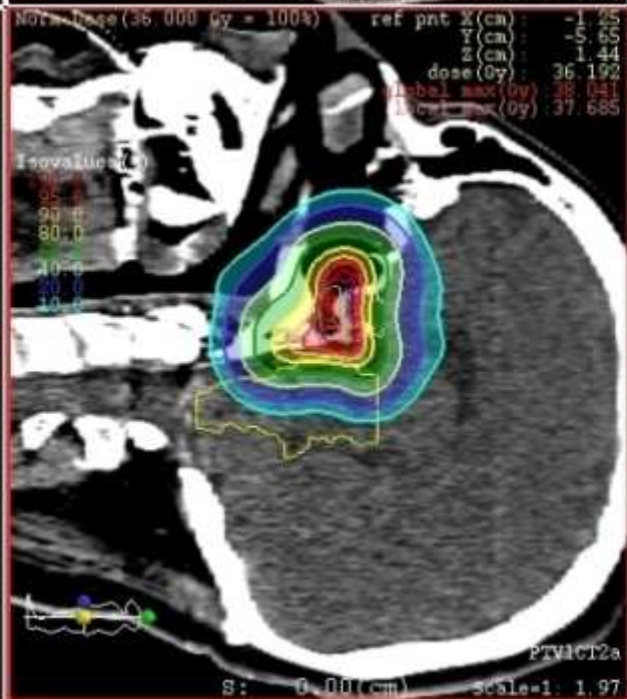
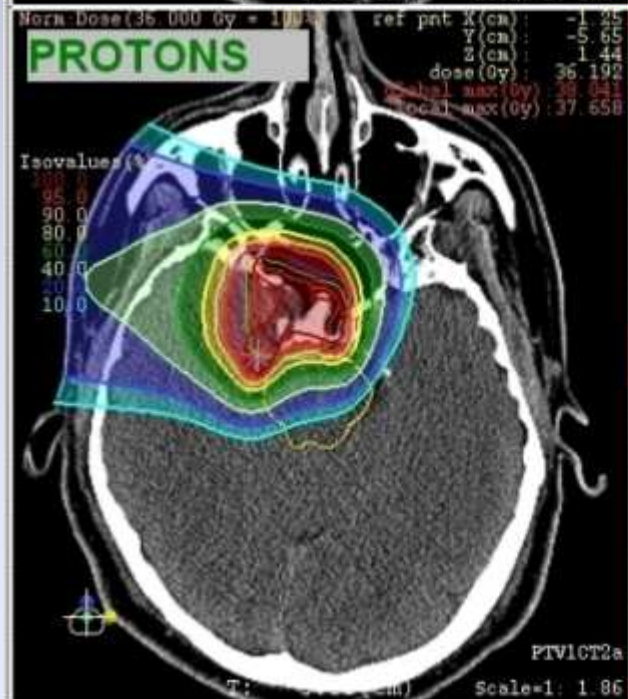
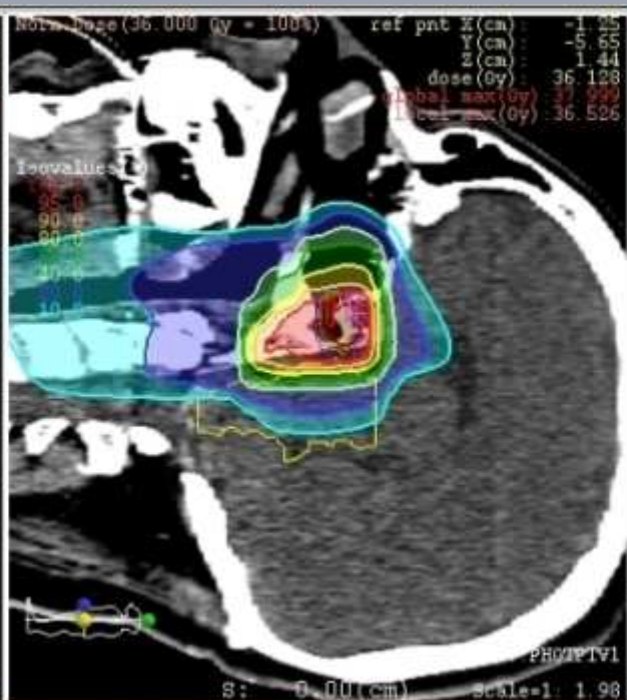
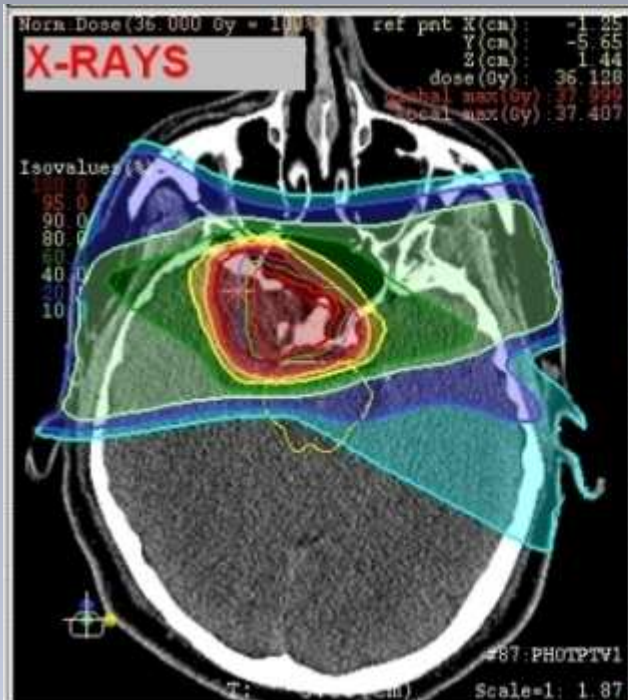
16 chordoma, 9 chondrosc., 8 rhabdomyosc. 5 other sc

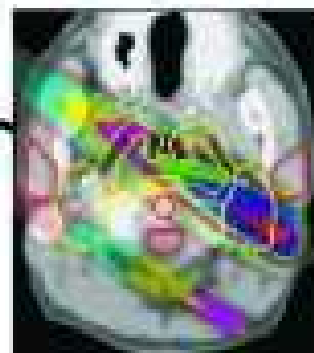
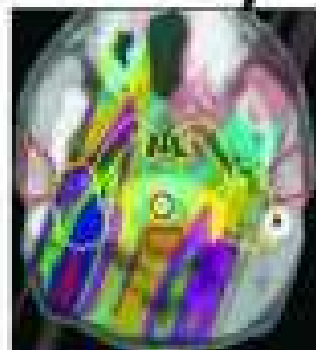
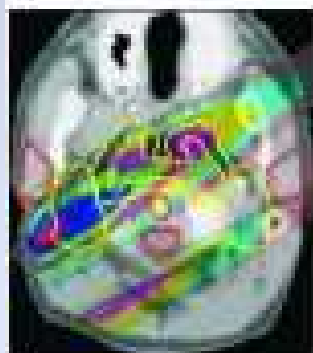
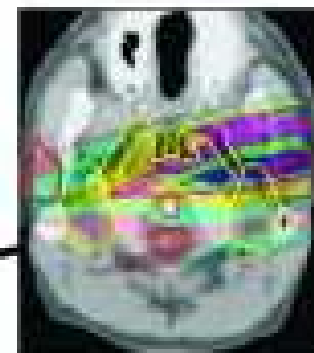
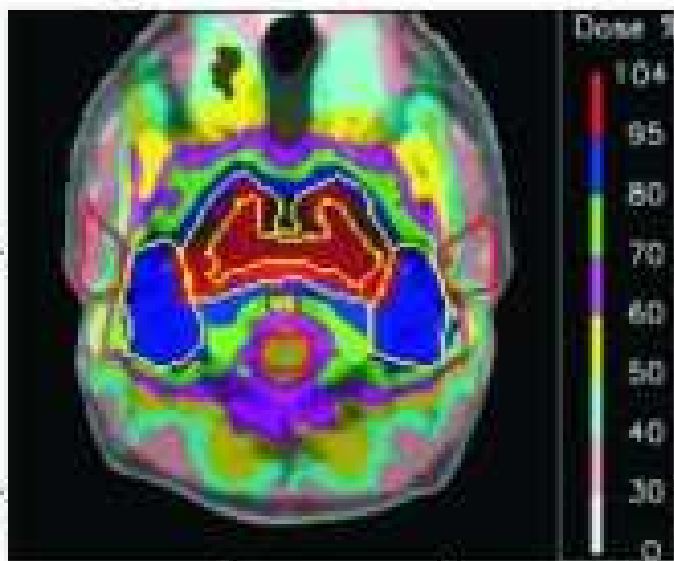
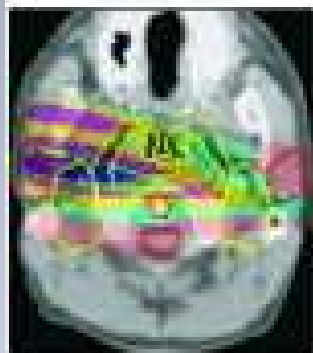
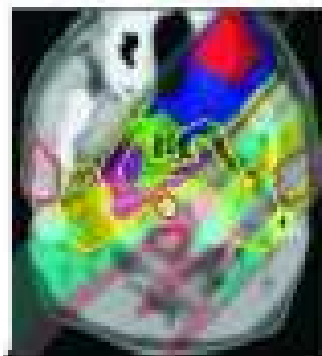
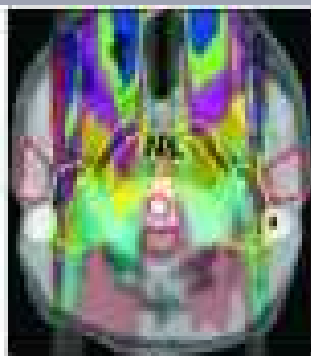
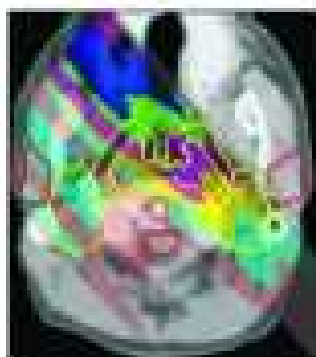
5 years local tumor control 72%:

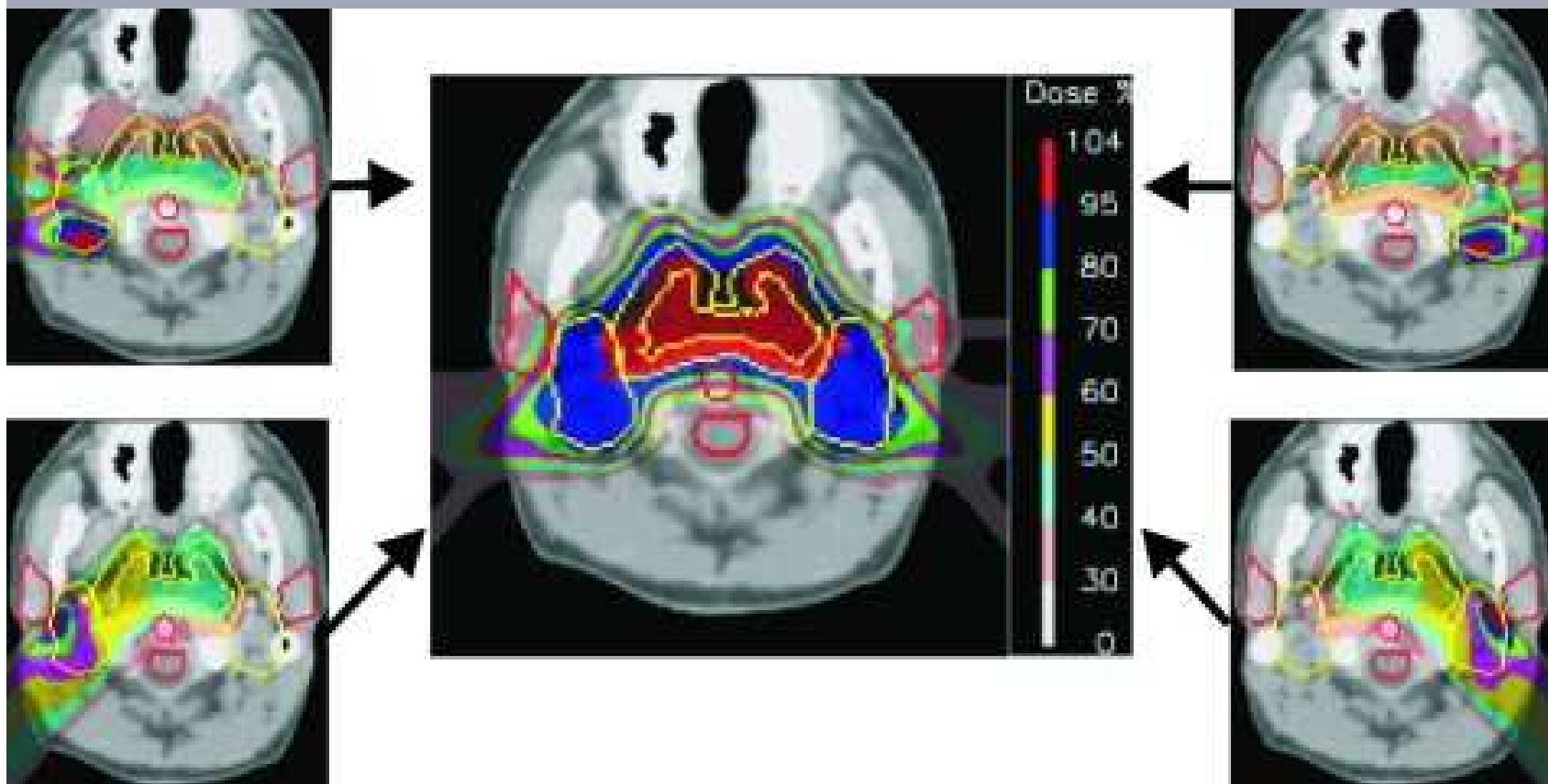
5 years overall survival 56%

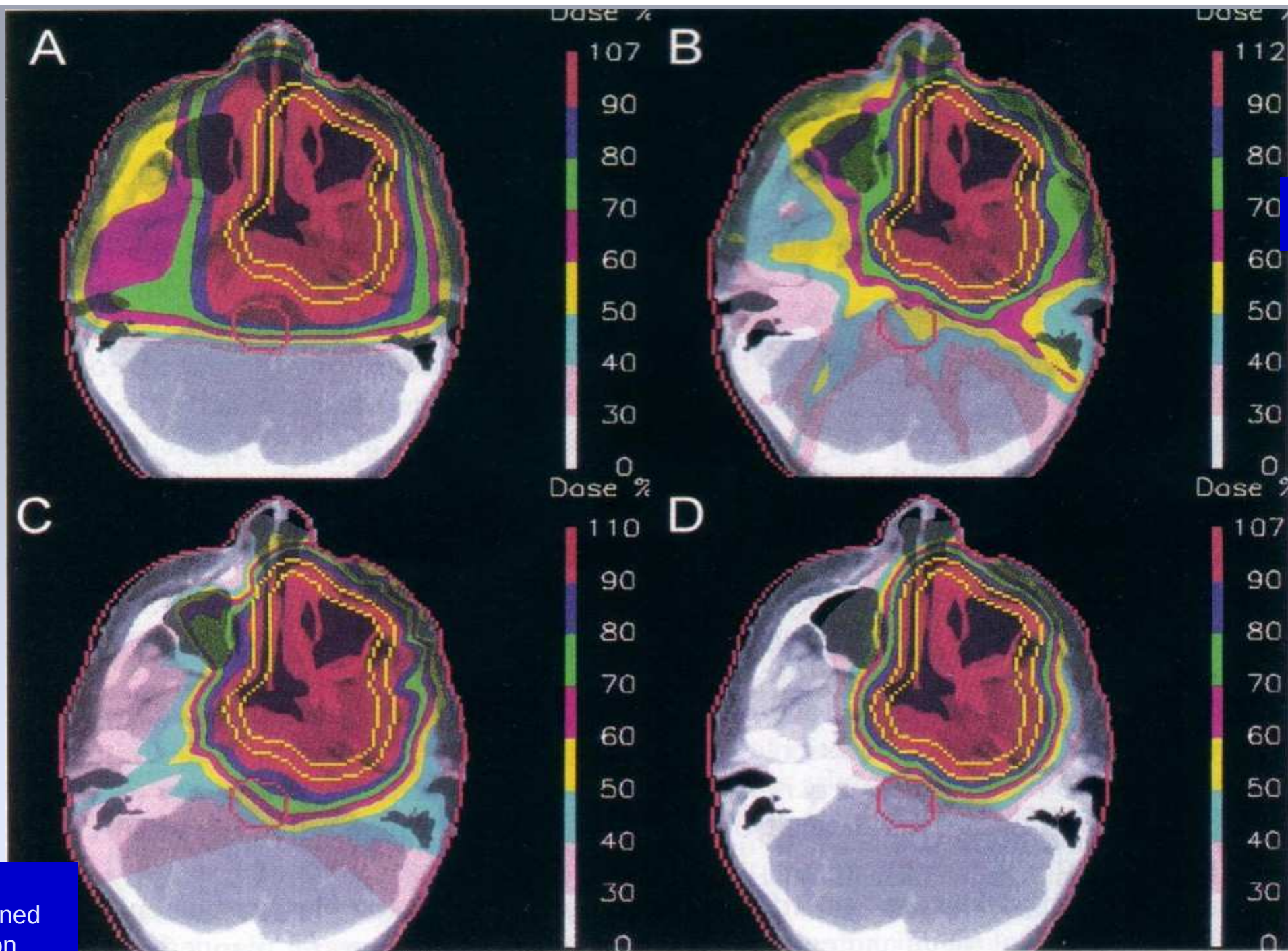
Serious neurological complication 7 %
(motor/sensor function deterioration)





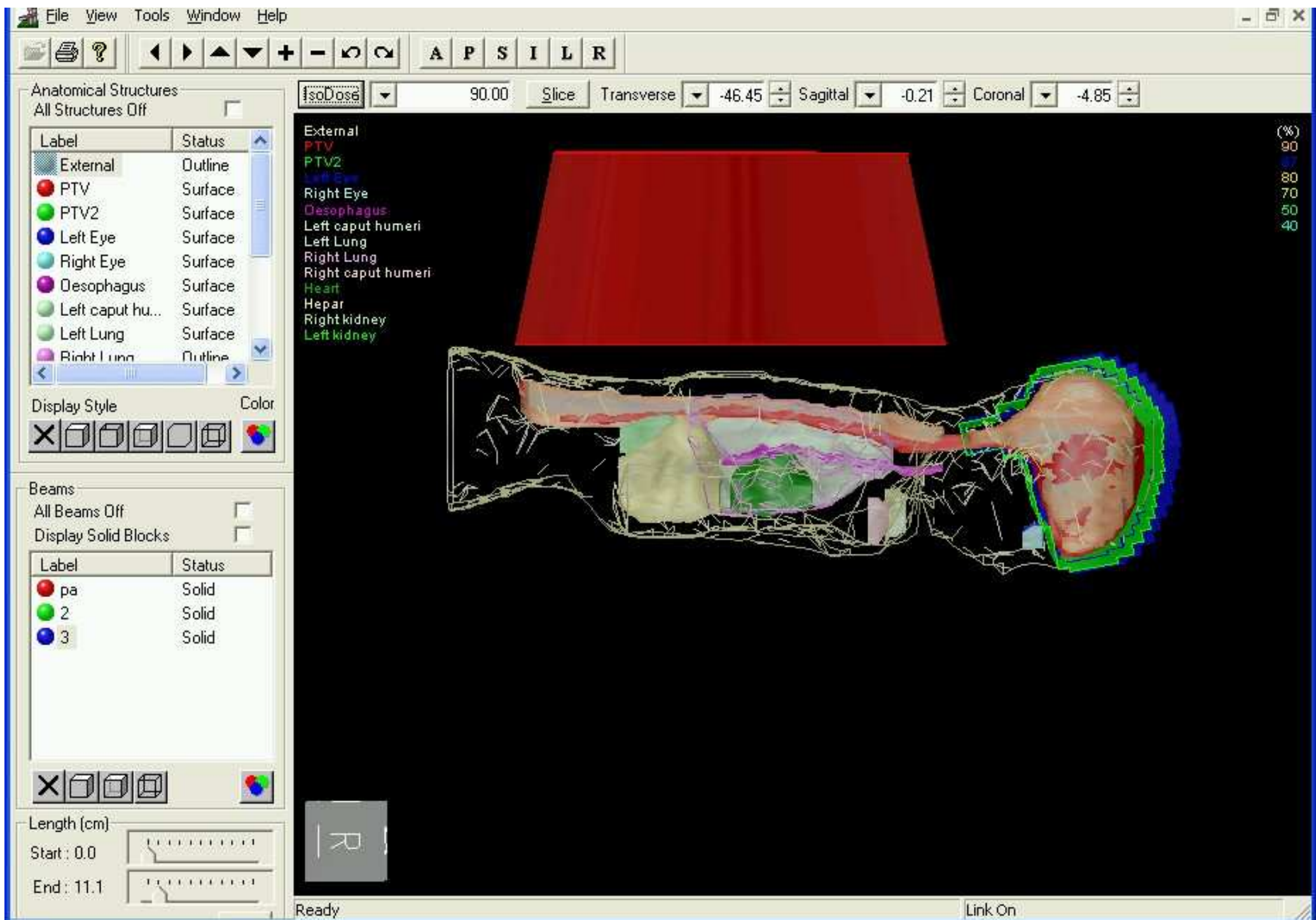


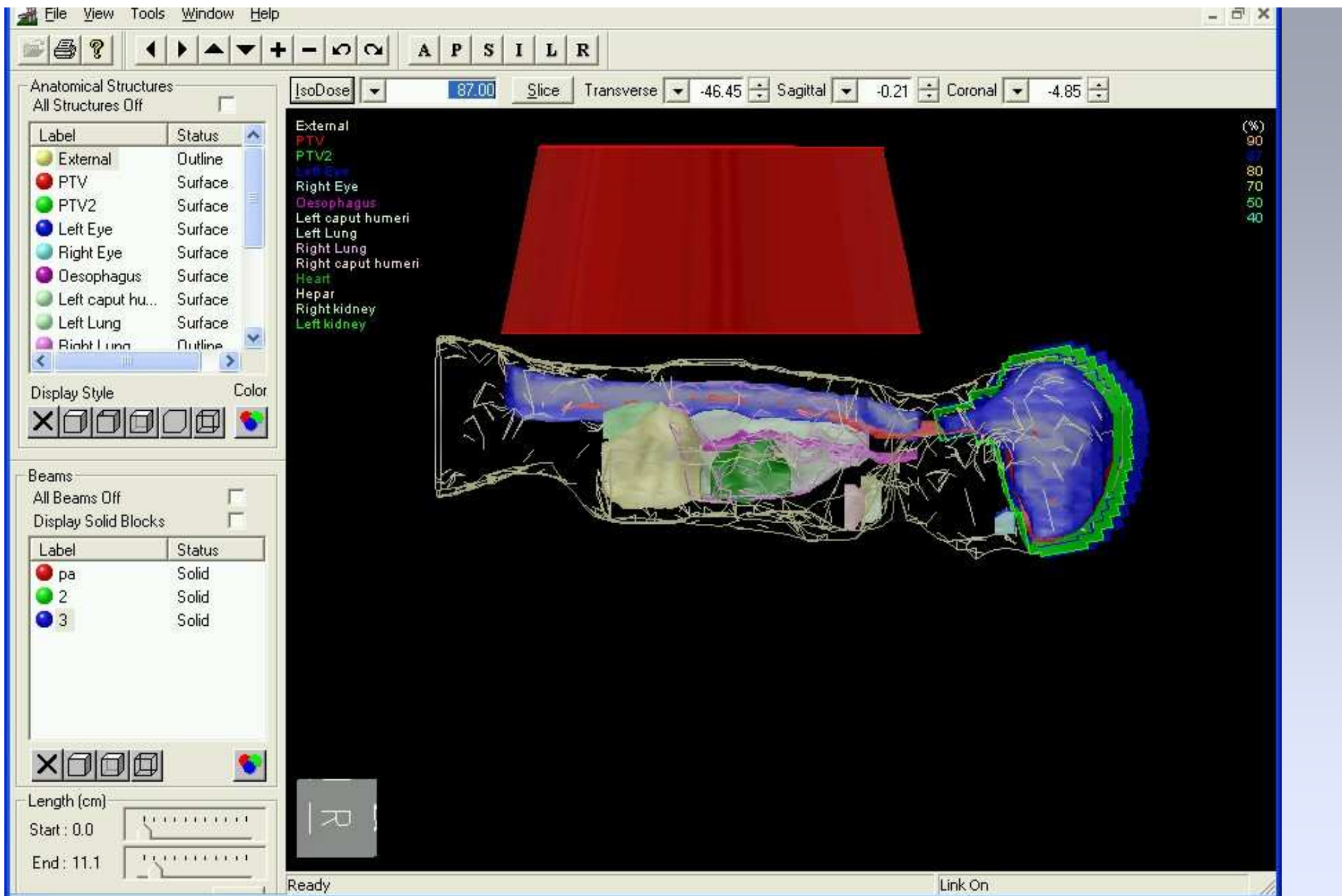


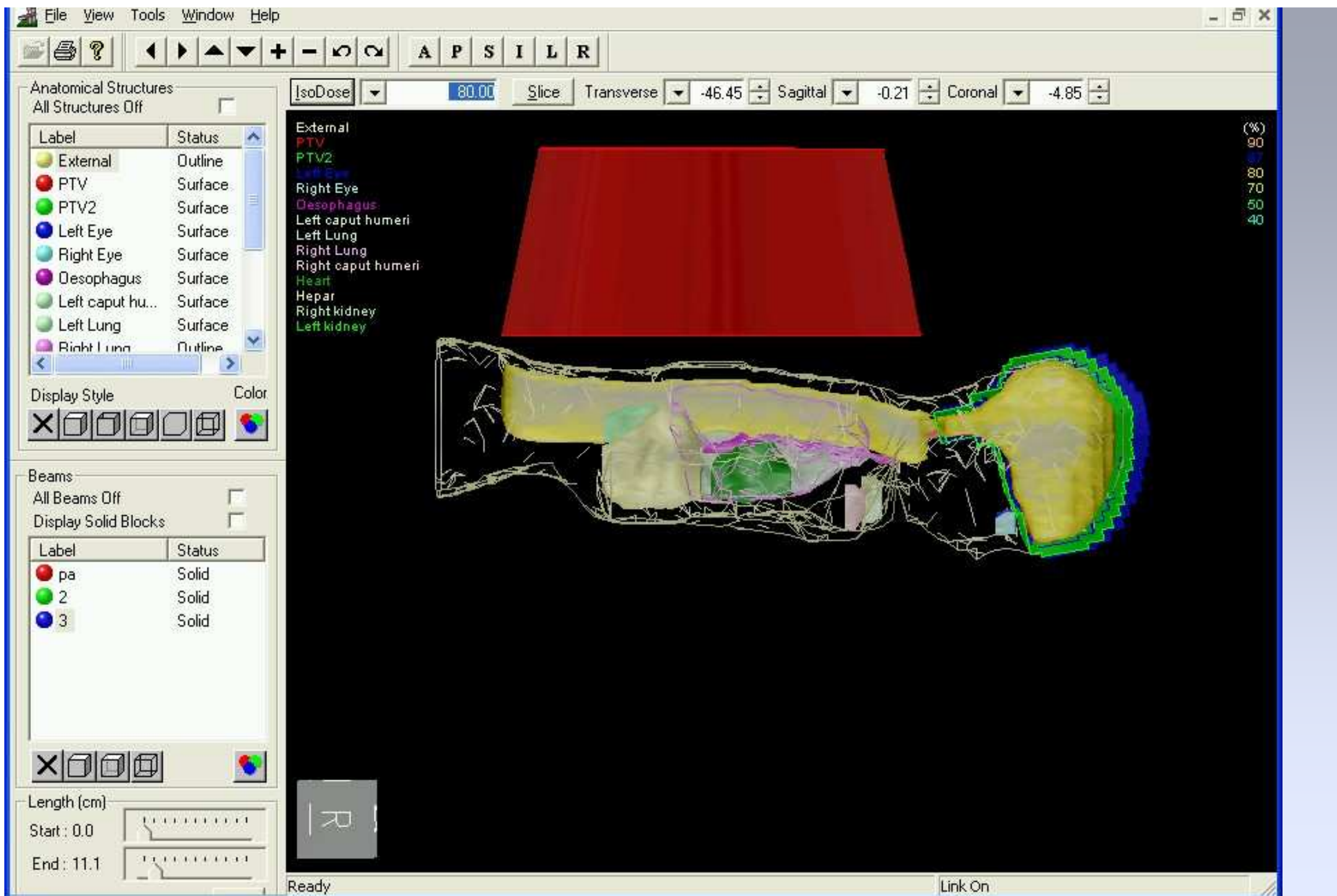


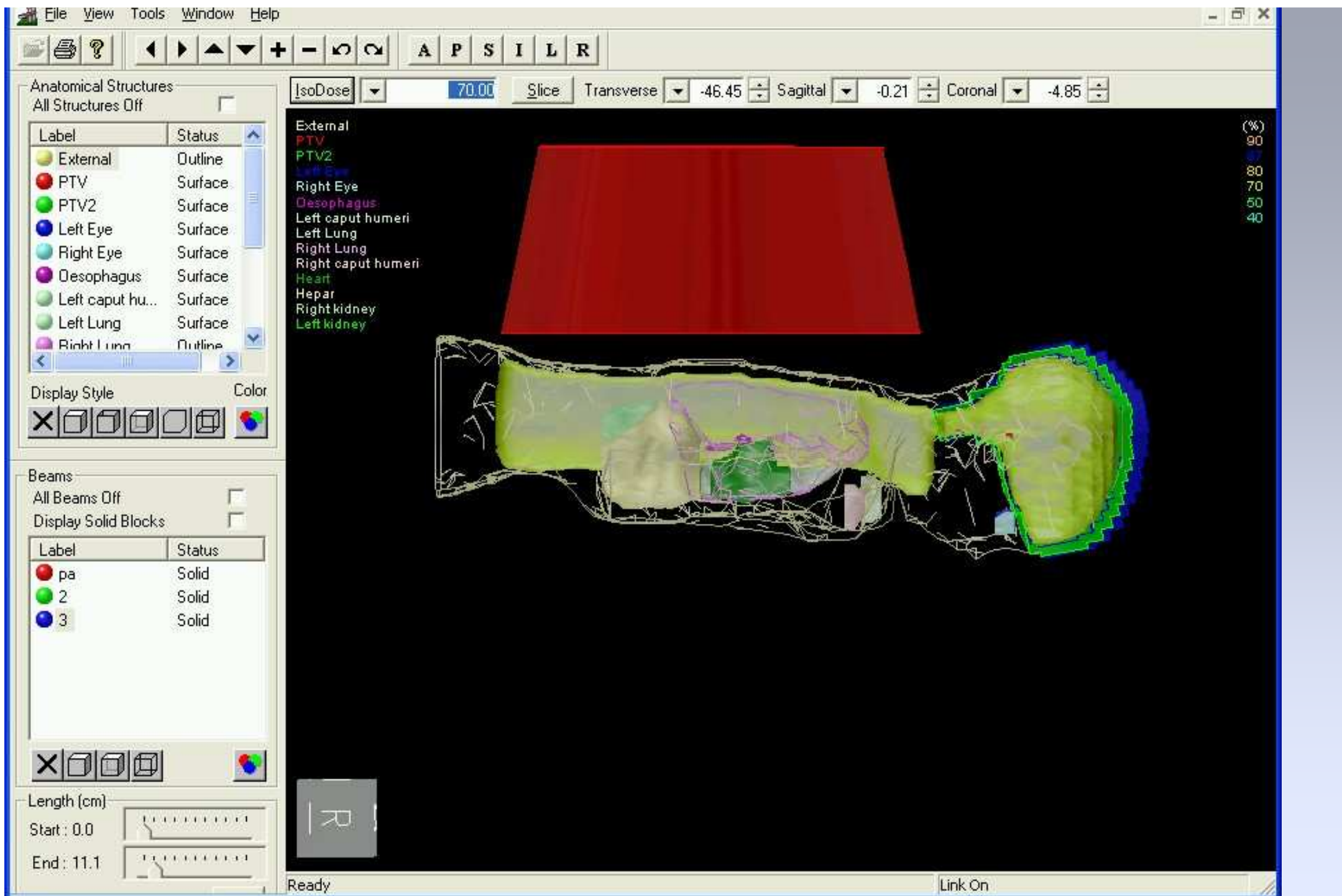
IM-
photon

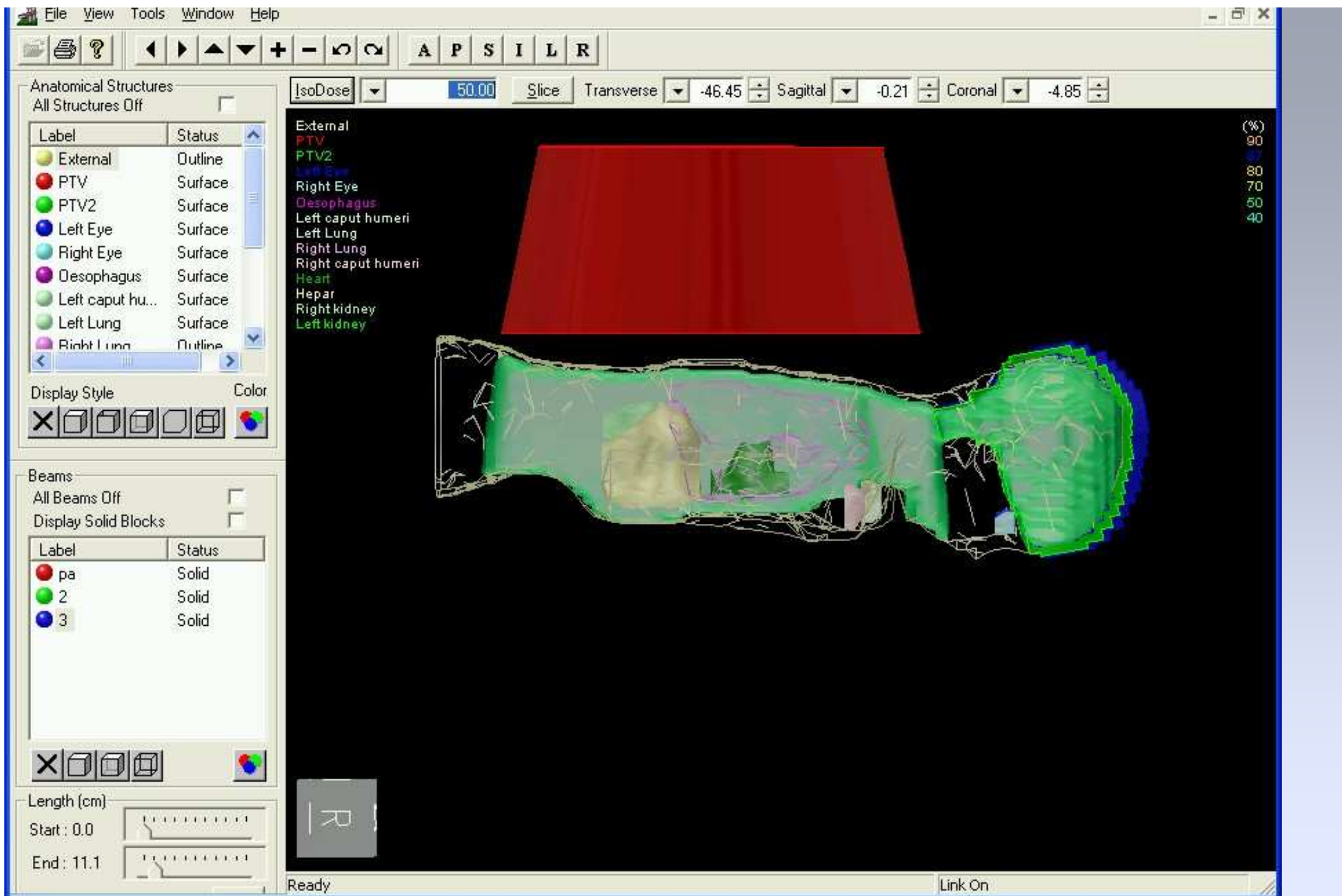
Spot
scanned
proton

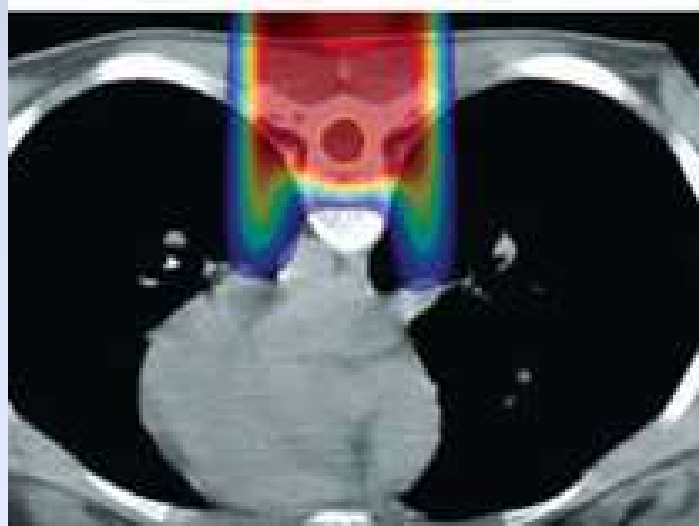
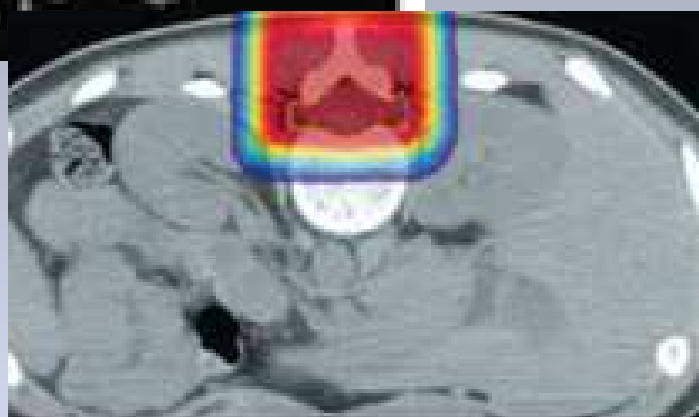
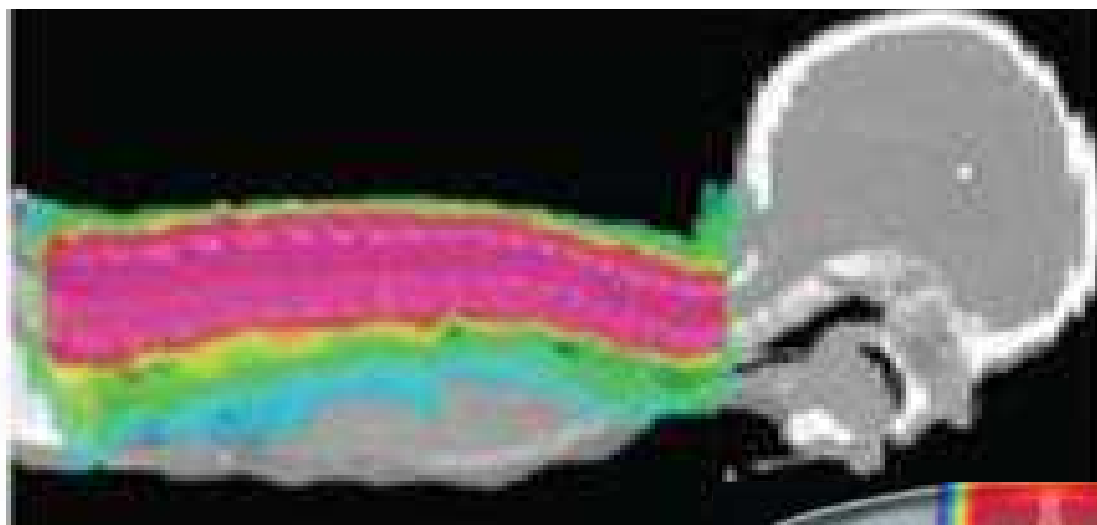












Dose (cGy)



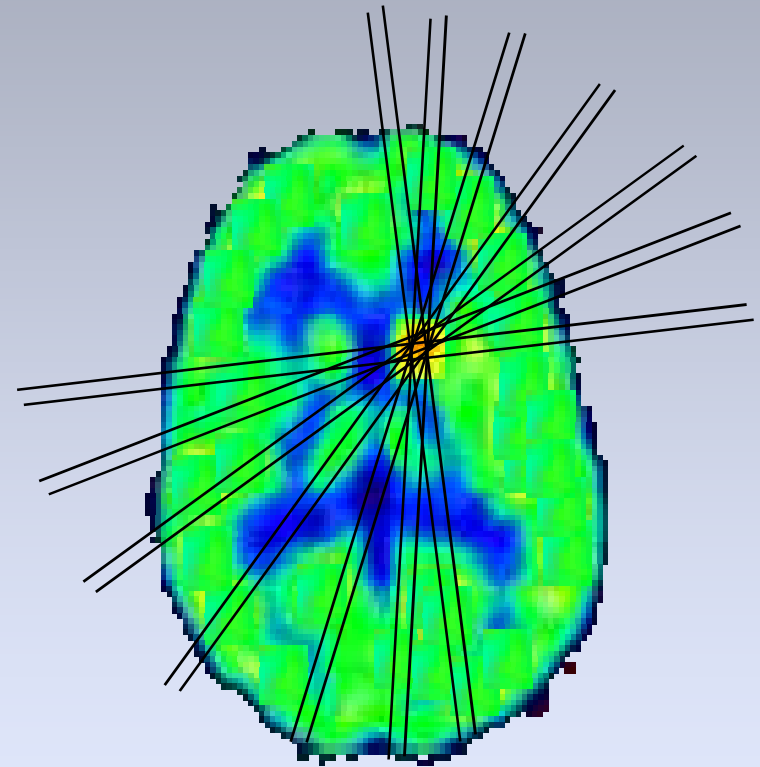
Protonterápia indikációja

Sugárérzékeny struktúrákkal övezett lokálisan növekvő tumorok:

- Szem tumorok (melanoma, retinobl.)
- Agyalapra terjedő tumorok (chordomák, chondrosarcomák, meningiomák, orrmelléküreg tu.)
- Kp.-i idegrsz : agydaganatok, gerincvelő ill. paraspinalis tumorok, AV malform.
- Gyermekkori daganatok
- Prostata karcinóma
- Emlő, fejnyak, nyelőcső, tüdő

PET Localization for Functional Proton Radiosurgery

- Treatment of Parkinson's disease
- Multiple narrow p beams of high energy (250 MeV)
- Focused shoot-through technique
- Very high local dose (> 100 Gy)
- PET verification possible after test dose

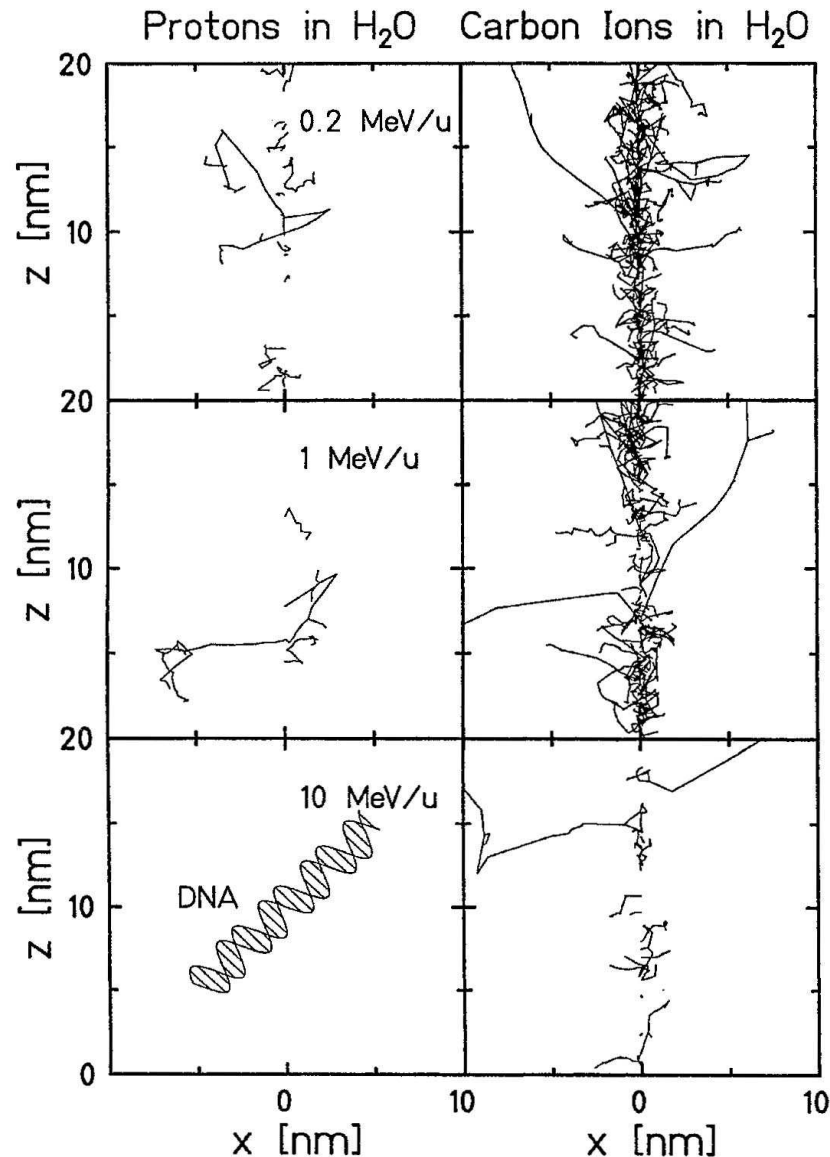


Positron Emission Tomography (PET) of Proton Beams

Reaction	Half-life	Threshold Energy (MeV)	<u>e</u>
$^{16}\text{O}(\text{p},\text{pn})^{15}\text{O}$	2.0 min	16.6	
$^{16}\text{O}(\text{p},2\text{p}2\text{n})^{13}\text{N}$	10.0 min	5.5	
$^{16}\text{O}(\text{p},3\text{p}3\text{n})^{13}\text{C}$	20.3 min	14.3	
$^{14}\text{N}(\text{p},\text{pn})^{13}\text{N}$	10.0 min	11.3	
$^{14}\text{N}(\text{p},2\text{p}2\text{n})^{11}\text{C}$	20.3 min	3.1	
$^{12}\text{C}(\text{p},\text{pn})^{17}\text{N}$	20.3 min	20.3	



Carbon ion terápia



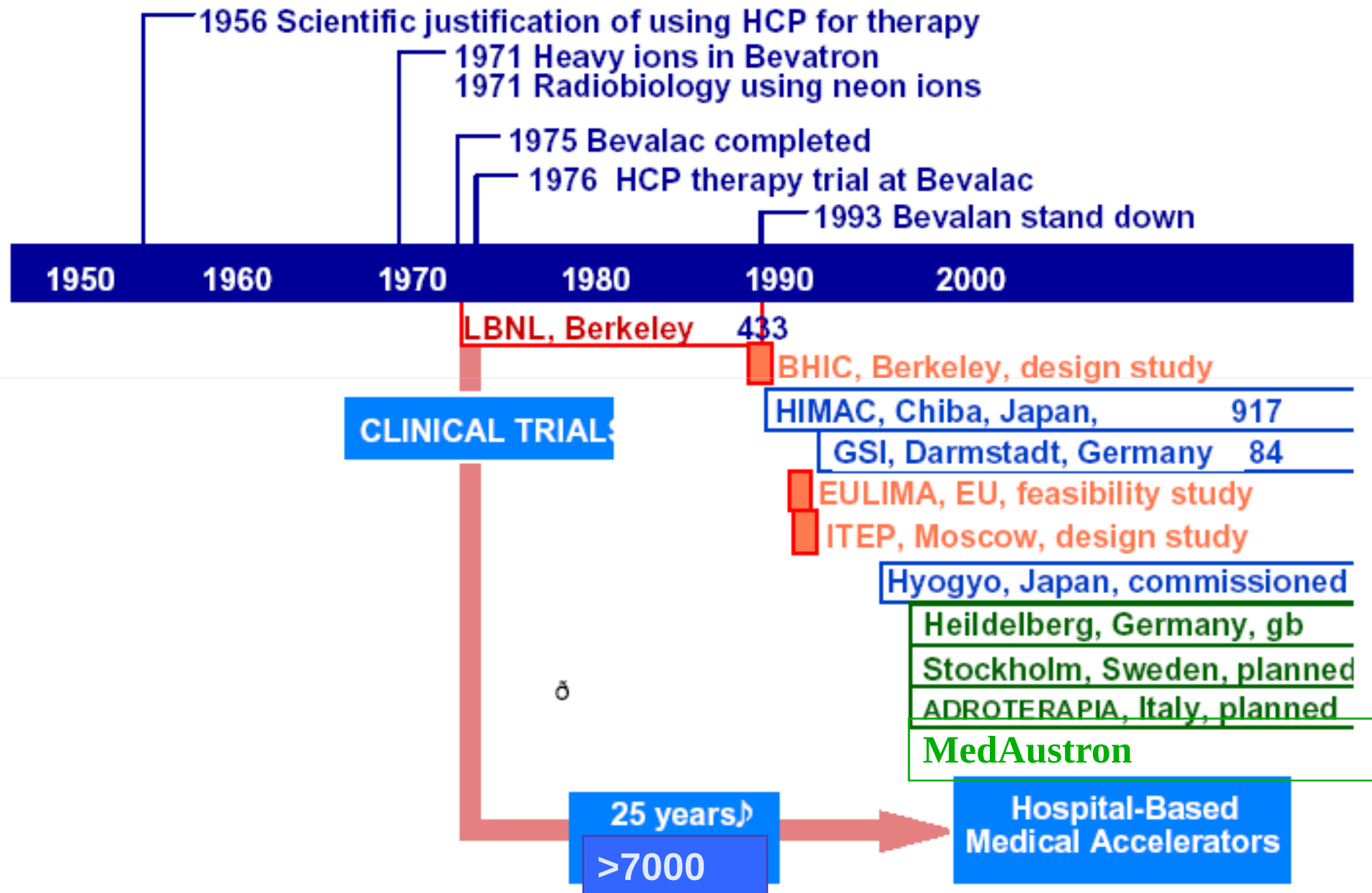
^{10}C és ^{11}C pozitron kibocsájtók - kezelés monitorizálás PET-el.

Nagy fizikai specificitás + nagy LET

Hátrányai

- drága
- korlátozottságok (fixált gantry)
- Tervezési, kivitelezési precizitás

High-LET Particle Therapy– Milestones



Neutron befogás terápia

Alapja egyes atomok relative nagy valószínűségű termikus neutron-befogása

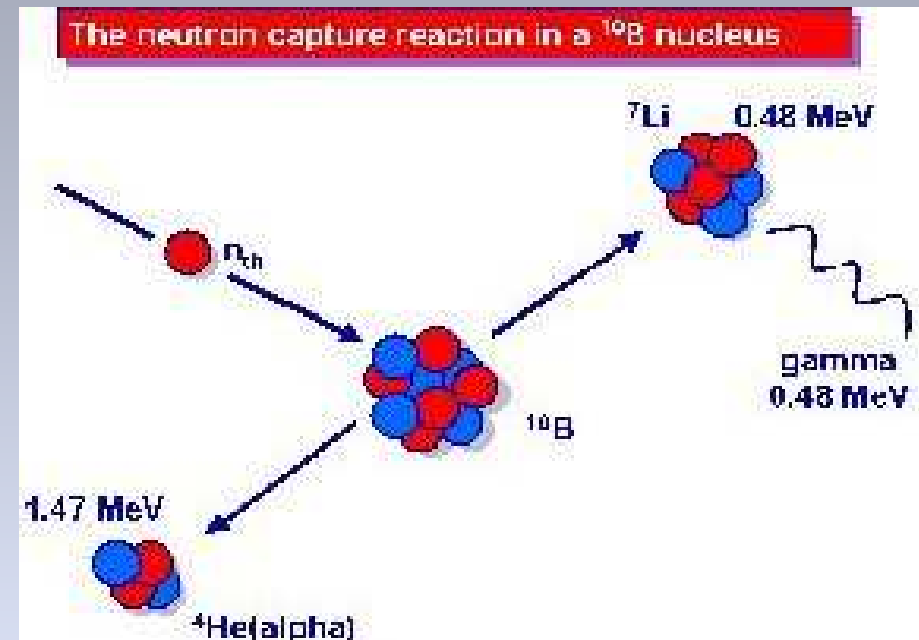
- Bór neutron befogás
- Gadolinium neutron befogás



Nuclearis reakció

Bór Neutron Befogás Terápia BNCT

- Bináris rendszer
- High LET
- High RBE
- Cell-targeted RT



Boron carrier

BPA (borophenylalanin)

BSH $\text{Na}_2\text{B}_{12}\text{H}_{11}\text{SH}$

Dose components

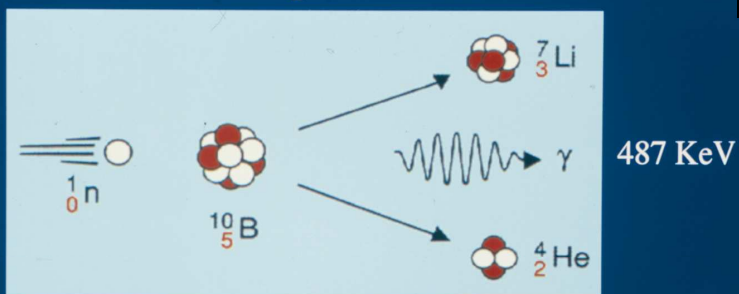
D_{Boron}

D_{Nitrogen}

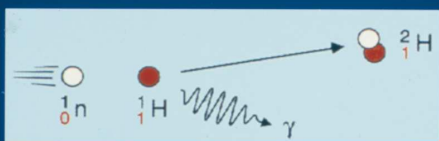
D_{Photon}

D_{neutron}

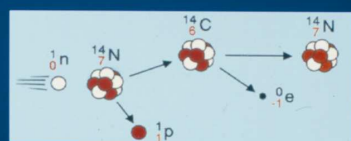
Neutron capture reactions



BNC: High LET radiation: range: 10-15 μm , energy: 2,3 MeV



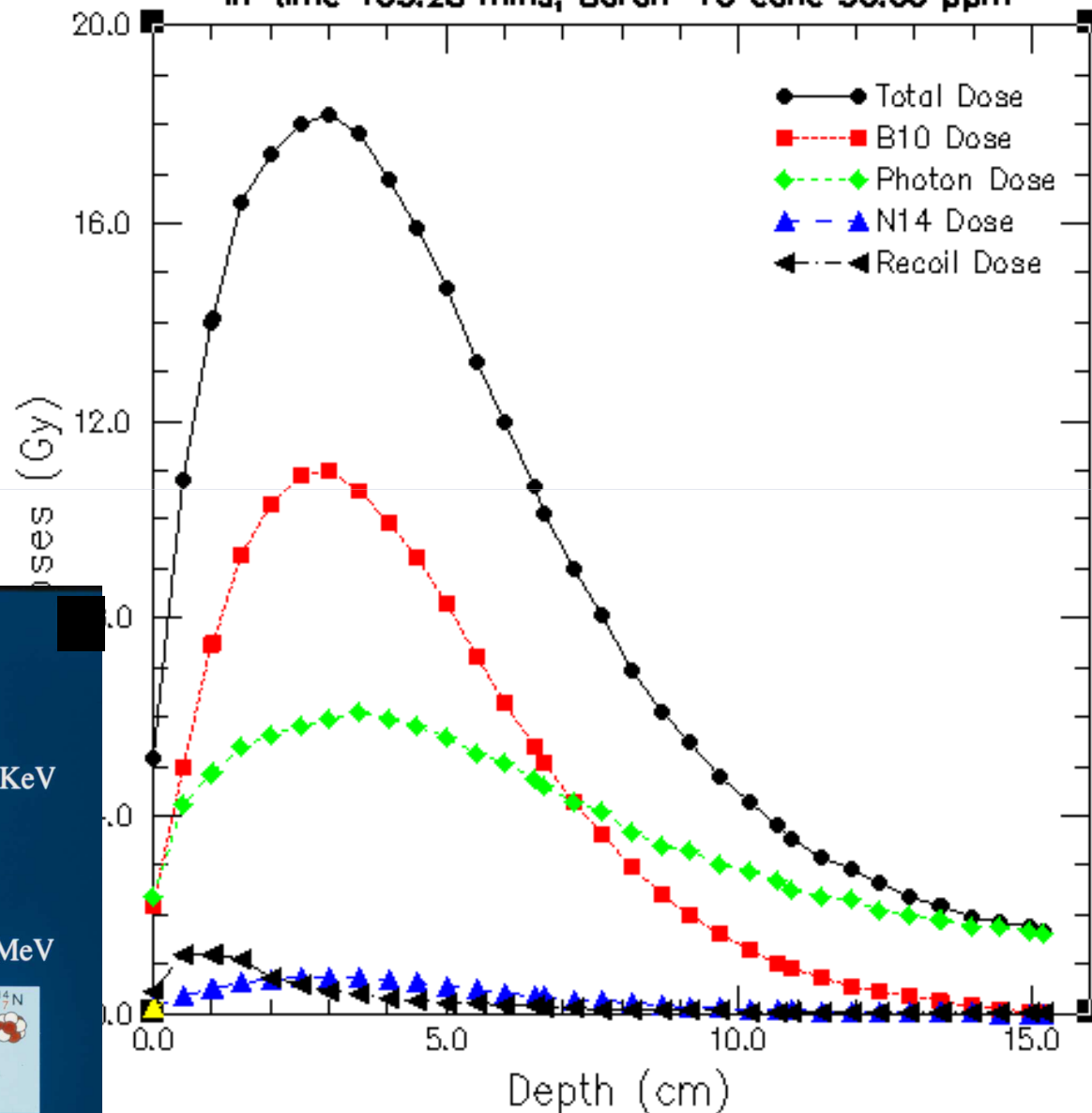
HNC: 2,2 MeV photons



NNC: back scattered protons

Dose Depth curve centre line of beam 110

Irr time 105.28 mins, Boron-10 conc 30.00 ppm



Miért nem alkalmazzák széleskörűbben a hadronterápiát?

The main limitation to use widely the CPT is the enormous cost of cyclotron based proton/heavy ion accelerator (around 100 million £) and the high maintenance-operation costs. According to recent estimation the cost of a Laser-driven CPT facility can be 10 folds lower (cc. 10 million £).

Tsukuba



250-MeV Synchrotron (gated
with respiratory motion)
with 1 fixed-beam research
and 2 gantry treatment rooms

Injector (RFQ/DTL Linac): Max.
energy: 7 MeV

Proton synchrotron:

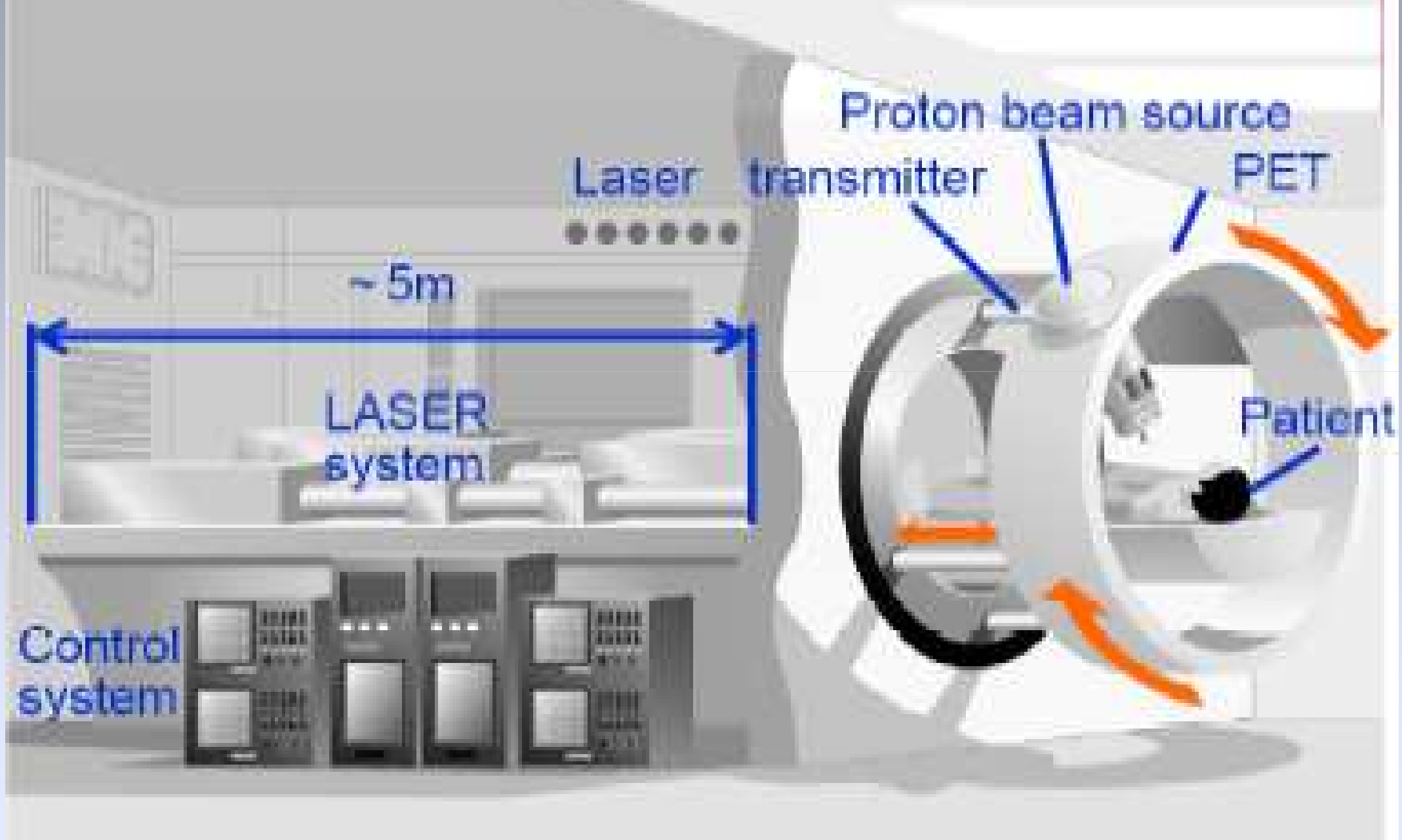
Energy: 70 . 270 MeV

Repetition rate: 0.15 . 0.5 Hz

Extracted beam intensity: 1.0×10^{11} protons/pulse, (16 nC/pulse)



„Table top” hadron forrás



Orvosi hadron forrás

- Intenzív sugárbiológiai kutatás
- Klinikai vizsgálatok
- **BETEGKEZELÉS**
- Frakcionálás optimalizálása/sugársebészet
- Kombináció
 - Más sugárkezelésekkel
 - Kemoterápiával/ biol. válaszmódosítókkal
 - Sugárvédő anyagokkal

Célkitűzés

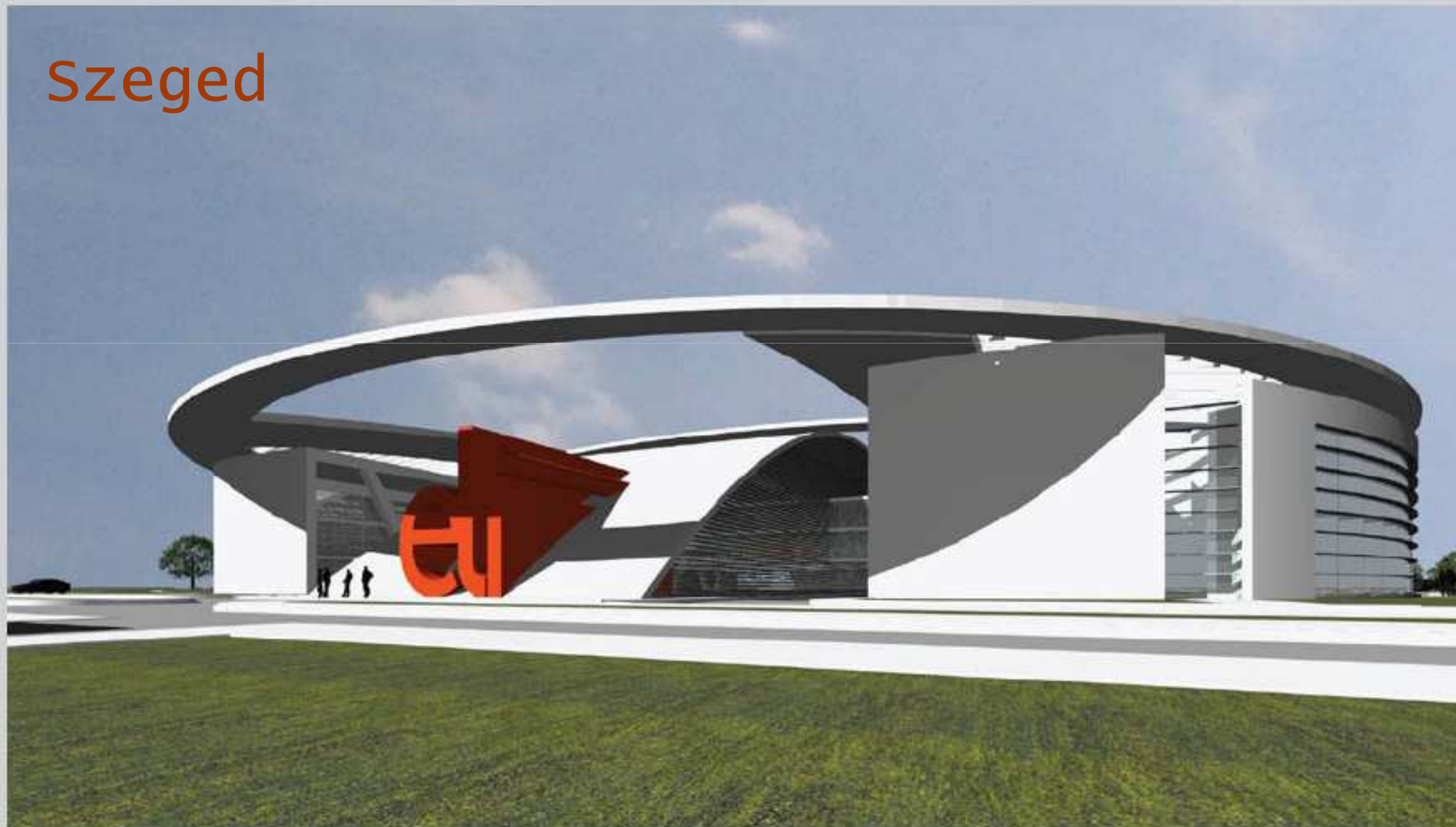
Kompakt, költség-hatékony Laser
indukált proton/ion berendezés,
amely betegek energia- és intenzitás-
modulált, töltött részecske kezelésére
(EIMCPT) alkalmas

Laser-hadron terápiás egység

- 1. Laser technology and target design for proton/ion acceleration
- 2. Technology and system development for the particle source operated as a treating facility- QA *
- 3. Dosimetric measurement and calculation on the laser accelerated charged particle for therapeutic application *
- 4. Preclinical research on the biological effect of laser driven CPT
- 5. Development of advanced patient positioning, individual immobilization for planning and CPT delivery.

- *
 - *radiation protection*
 - *particle /energy selection*
 - *particle intensity, direction, dose rate*
 - *beam collimation*
 - *complex facility design*
 - *proper room-building design*
 - *beam operation*
 - *treatment monitoring*
 - *quality assurance*

Szeged



Sugárbiol. munkacsoport feladatai

- I. Speciális pozícionáló és immobilizációs eszközfejlesztés hadronterápiához
- II. Lézer indukált sugárforrások hatásának vizsgálatára alkalmas biológiai modellek kidolgozása
 - konvencionális sugárforrásnál három fő biológiai rendszer beállítása
 - Sugárkezelés- biológiai hatás vizsgálata

